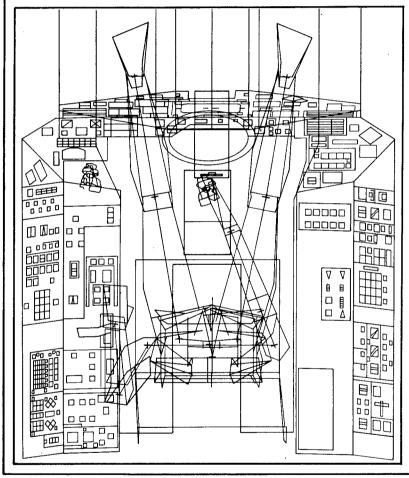
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JOINT ARMY-NAVY AIRCRAFT INSTRUMENTATION RESEARCH

JANAIR REPORT 690102 **ONR Contract** N00014-68-C-0289 NR 213-065





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COCKPIT GEOMETRY EVALUATION

PHASE I FINAL REPORT **VOLUME II-HUMAN DATA**

JANUARY 1969

D162-10126-1

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VOLUME	DOCUMENT Number	TITLE
1	D162-10125-1	PROGRAM DESCRIPTION AND SUMMARY
11	D162-10126-1	HUMAN DATA
111	D162-10127-1	COMPUTER PROGRAM
IV	D162-10128-1	MATHEMATICAL MODEL
v	D162-10129-1	VALIDATION

COCKPIT GEOMETRY EVALUATION PHASE I

FINAL REPORT

VOLUME II-HUMAN DATA

Prepared for Joint Army-Navy Aircraft Instrumentation Research Program

Office of Naval Research, Department of The Navy under Contract N00014-68-C-0289 NR 213-065

Research Engineer, Personnel Subsystem .

P.W. Ryan

Project Director _____

W.E. Springer



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FOREWORD

This report presents work which was performed under the Joint Army Navy
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Electronics Command, the Naval Air Systems Command, and the Office of Naval
Research through an organization known as the JANAIR Working Group. The
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- U. S. Navy, Office of Naval Research Aeronautics, Code 461, Washington, D. C.
 - Aircraft Instrumentation and Control Program Area
- U. S. Navy, Naval Air Systems Command Washington, D. C.
 - Avionics Division; Navigation Instrumentation and Display Branch (NAVAIR 5337)
 - Crew Systems Division; Cockpit/Cabin Requirements and Standards Branch (NAVAIR 5313)
- U. S. Army, Army Electronics Command Avionics Laboratory, Fort Monmouth, New Jersey - Instrumentation Technical Area (AMSEL-VL-I)

The Joint Army Navy Aircraft Instrumentation Research Program objective is: To conduct applied research using analytical and experimental investigations for identifying, defining and validating advanced concepts which may be applied to future, improved Naval and Army aircraft instrumentation systems. This includes sensing elements, data processors, displays, controls and man/machine interfaces for fixed and rotary wing aircraft for all flight regimes.

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1.0 INTRODUCTION AND SUMMARY

A computerized dynamic man-model is being developed as part of a contract administered by the Office of Naval Research (ONR) through the auspices of the Joint Army Navy Aircraft Instrumentation Research (JANAIR) Program Working Group (Committee). The baseline man-model to be developed in the first year of the proposed six-year program is a 23-joint articulated link "stick-man" as shown in Fig. 1. The man-model specifications are given in Appendix A.

The anthropometric, joint angular, mass, and visual characteristics used for the initial man-model (BOEMAN-I) are listed in this document. Present literature has been used whenever possible to provide the dimensional, mass, angular or visual information. Whenever these data proved insufficient, assumptions were made, as stipulated herein, to derive the necessary additional information.

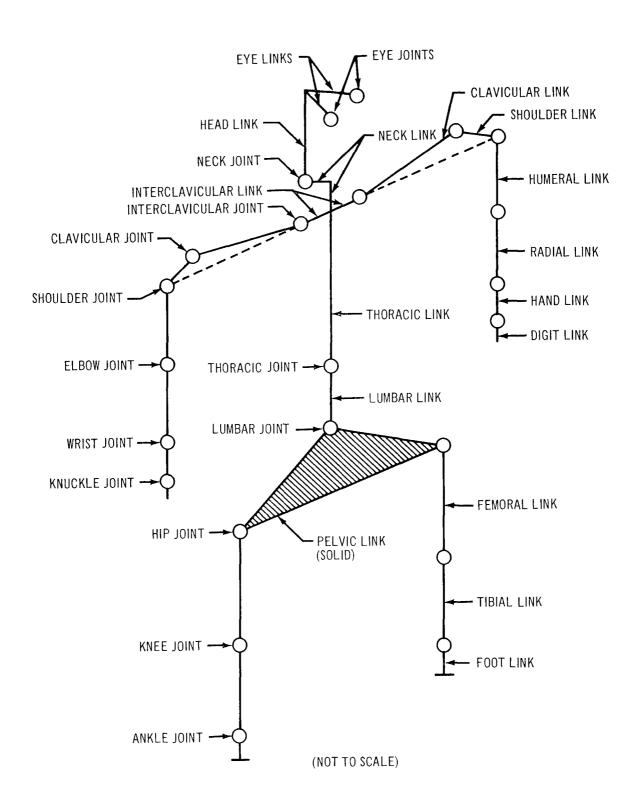


Figure 1. BOEMAN 1

2.0 GLOSSARY OF TERMS USED IN BODY MEASUREMENTS AND THE BASELINE MAN-MODEL

ACROMIAL Pertaining to the acromion.

ACROMION The highest point on the lateral edge of the shoulder

bone.

ANKLE JOINT Level of a line between the tip of the lateral

malleolus of the fibula and a point 5 mm distal to

the tibial malleolus.

ANTERIOR The front part of the body, or segment thereof, or

pertaining to the front part of the body.

AXILLARY Referring to the armpit region.

BICEPS The large muscle in the anterior aspect of the upper

arm.

BODY INDEX A descriptor of somatotype; the term C in $C = HW^{-1/3}$.

BROW RIDGE The bony elevation covered by the eyebrows.

CANTHUS A corner or angle formed by the meeting of the

eyelids.

CERVICALE The largest bony bump on the spinal column in the

region of the base of the neck.

CLAVICLE A bone joined to the breastbone and the scapula -

the "collarbone".

CLAVICULAR JOINT Midpoint of a line between the coracoid tuberosity

of the clavicle (at the posterior border of the bone) and the acromicclavicular articulation (or the tubercle) at the lateral end of the clavicle; the point, however, would be visualized as on the underside of

the clavicle.

CLAVICULAR LINK The direct distance between the two joint centers

listed above.

CRINION The point in the midplane where the hairline meets

the forehead.

DELTOID MUSCLE The large muscle on the outer side of the upper

arm in the shoulder region.

DIGIT LINK The distance between the third metacarpophalangeal

joint and the end of the third digit.

DISTAL END

The end of a limb farthest from the trunk,

opposed to proximal.

ECTOTYPE

An ectomorphic somatotype.

ELBOW JOINT

Midpoint of a line between (1) the lowest palpable point of the medial epicondyle of the humerus, and (2) a point 8 mm above the radiale (radiohumeral junction).

ENDOTYPE

An endomorphic somatotype.

EXTERNAL

Away from the central long axis of the body; the outer portion of a body segment.

EYE JOINT

The ball and socket joint in which the eyeball

moves.

EYE LINK

The distance between an eyeball and the head

link (See Fig. 1).

FEMIR

The bone of the thigh.

FEMORAL LINK

The distance between the hip joint and the knee

joint centers.

FOOT LINK

The distance between the ankle joint center and the sole of the foot.

FOREARM LINK

Same as the radial link.

FRANKFORT PLANE

The standard plane of orientation of the head, determined by locating the lower edges of the eye sockets and a single tragion in the same horizontal plane. This can be closely approximated when the subject looks directly forward.

GLABELLA

The most forward point in the midline of the forehead between the brow ridges.

GLUTEAL FURROW

The furrow formed by the overhang of the buttock on the back of the upper leg.

GONTAL ANGLE

The angle at the back of the lower jaw formed by the intersection of the vertical portion with the lower edge of the horizontal portion of the jaw.

HAND LINK

The distance between the wrist and the third metacarpophalangeal joint center.

HEAD LINK

Vertical distance from the neck joint center to the proximal end of the eye links. HELIX

The rolled outer part of the ear.

HUMERAL LINK

The distance between the shoulder and elbow

joint.

HUMERUS

The bone of the upper arm.

HIP JOINT CENTER

(Lateral aspect of the hip). A point at the tip of the femoral trochanter 0.4 inch anterior to the most laterally projecting part of the

femoral trochanter.

INION

A small bony bump often found at the rearmost part of the head.

INTERCLAVICULAR JOINT

The joint center between the sternum and a clavicular link.

INTERCLAVICULAR LINK

The distance between the left and right interclavicular joint centers.

INTERNAL

Near the central long axis of the body; the inner portion of a body segment.

KNEE JOINT

Midpoint of a line between the centers of the posterior convexities of the femoral condyles.

KNUCKLE JOINT

The joint formed by the meeting of a finger bone (phalanx) with a palm bone (metacarpal).

LARYNX

The cartilaginous box in the throat which houses the voice mechanism. The "Adam's Apple" is the most noticeable part of the larynx.

LATERAL

Lying to the right or left side of the midsagittal plane of the body; opposed to medial.

LATERAL VASTUS MUSCLE

The large muscle on the outside or the upper leg running from just above the kneecap to the hip.

LEG LINK

Same as tibial link.

LINK

Ordinarily a connector between adjacent joint centers; otherwise the segment beyond a terminal joint; a member of an immovable pair (neck and thoracic links); the distance between eyeball centers and the head link.

LUMBAR JOINT

The joint postulated to be at the junction of

the spine and hip.

LUMBAR LINK

Link between the lumbar and thoracic joint centers.

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MALLEOLAR

Referring to the malleolus.

MALLEOLUS

A rounded bony projection in the ankle region. There is one on both the lateral and medial

sides of the leg.

MANDIBLE

The lower jaw.

MASS MOMENT OF INERTIA

With respect to a given axis, it is the limit of the sum of the products of the masses of each of the elementary particles into which the entity can be conceived to be divided and the square of their distance from the given axis.

MASTOID PROCESS

The bony protrusion directly behind the ear.

MEDIAL

Lying near the midsagittal plane of the body; opposed to lateral.

MEDIAL VASTUS MUSCLE

The large muscle on the inside of the front of the upper leg running from knee cap to the hip.

MEMBRANOUS LIP

The lip of everyday language; the reddish

portion of the lip.

MENTON

The lower surface of the tip of the chin in the

midsagittal plane.

METACARPAL BONE

A bone of the palm of the hand.

METACARPALE

The point of juncture on the back of the hand of the palm bone (metacarpal) with the first bone of the finger (phalanx).

METATARSAL

A bone of the instep of the foot.

MIDPLANE

Same as midsagittal plane.

MIDSAGITTAL PLANE

The plane which divides the body into symmetrical right and left sections.

NASAL ROOT

The area of greatest indentation where the nose meets the forehead.

NASAL SEPTUM

The cartilaginous wall separating the right

nostril from the left.

NATURAL WAIST LINE

The level of greatest lateral indentation in the abdomen region. If no Natural Waist Line is visible, the level at which the belt is worn is used instead.

NAVICULAR BONE

The small bone of the hand just distal to the bend of the wrist on the thumb side.

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NECK JOINT

The joint center postulated to be between the

head and neck links.

NECK LINK

Consisting of both a vertical and a horizontal component connecting the neck joint and the point where the interclavicular link crosses

the thoracic link.

OCCIPITAL REGION

The back of the head.

OLECRANON

The bony tip of the elbow.

ORTHOSIS

The straightening of a deformity as by a brace.

PATELLA

The kneecap.

PELVIC LINK

The distance between hip joints (horizontal), or the distance between a line connecting the hip joints and the lumbar joint (vertical).

PHALANGEAL

Referring to a phalanx or to the phalanges.

PHALANX

(Plural, Phalanges) - A bone of the fingers or

toes.

PHILIRUM

The vertical groove running from the upper membranous lip to the base of the nasal septum.

POPLITEAL AREA

The area of the back of the leg directly behind

the knee.

POSTERIOR

The back of the body or referring to the back of the body.

PROSTHESIS

An artificial substitute for a missing part as

a hand, arm, leg, etc.

PROXIMAL END

The end of a limb nearest the trunk; opposed

to distal.

RADIAL LINK

The distance between the wrist and elbow joint

centers.

RADIUS

One of the two forearm bones. This bone runs from the lateral side of the elbow region to the

wrist on the same side as the thumb.

RAMUS

(Plural, Rami) - The vertical portion of the

lower jaw bone (mandible).

SAGITTAL PLANE

Median vertical longitudinal plane dividing the human into right and left halves.

SCYE

The girth of the upper arm around the shoulder (acromion).

SHOULDER JOINT

A joint center between the scapula or shoulder

link and the humeral link.

SHOULDER LINK

The distance between the clavicular and shoulder joint centers - an unsatisfactory measurement - approximately 3.5 cm.

SITS ERECT

Subject sits on a flat horizontal surface, his weight distributed equally, with his back held in and his shoulders held back, thighs horizontal and the knees at right angles.

SOMATOTYPE

A classification of body characteristics among endomorphy, mesomorphy, and ectomorphy.

STERNUM

The breastbone.

STYLION

The point at the center of the notch just distal to the styloid process of the radius.

SUBMANDIBULAR

Under the mandible or lower jaw.

SUBNASALE

The point where the base of the nasal septum meets the philtrum.

SUBSTERNALE

The point located at the middle of the lower edge of the breastbone.

SUPRASTERNALE

The lowest point of the notch in the upper edge of the breastbone.

TEMPLE REGION

The area on the side of the head between eye and ear.

TEMPORAL CREST

A narrow, bony ridge running along the side of the head, curving up from the upper lateral margin of the eye socket, above and past the ear, and downward, ending behind the ear. This serves as the area of attachment for the temporal muscles.

TEMPORAL MUSCLES

The muscles of the temple region.

THORACIC LINK

Link above lumbar link, in thoracic region, from the thoracic joint to the neck link.

THORACIC JOINT

A joint postulated to be located at the waist; the joint center between the lumbar and thoracic links.

TIBLAL LINK

The distance between the ankle and knee joint centers.

TRAGION

The point located at the notch just above the tragus of the ear. This point corresponds approximately to the upper edge of the ear hole.

TRAGUS

The small cartilaginous flap in front of the ear hole.

TRAPEZIUS MUSCLE

The large muscle at the back of the neck and shoulder.

ULNA

One of the two forearm bones; this bone runs from the tip of the elbow to the wrist on the same side as the little finger.

ULNAR

Referring to the ulna.

VASTUS

See lateral vastus muscle and medial vastus muscle.

WRIST JOINT

On the palmar side of the hand, the distal wrist crease at the palmaris longus tendon, or the midpoint of a line between the radial styloid and the center of the pisiform bone; on the dorsal side of the hand, the palpable groove between the lunate and capitate bones, on a line with metacarpal bone III.

ZYGOMATIC ARCH

The bony arch running along the side of the cheek almost to the ear.

3.0 DISCUSSION

3.1 GENERAL

The data necessary to describe the articulated link baseline man-model (BOFMAN-I) include: (1) link lengths, (2) joint angular limits, (3) link mass quantities and location, (4) visual capabilities, and (5) the relationships between standard anthropometric measurements and quantities required for BOFMAN-I.

The following sections include applicable data from present literature and information derived by the authors to supplement these as required.

3.1.1 Anthropometric Characteristics

Present anthropometric surveys (Refs. 1, 2, 4, 6, 25, 47, 48) serve as an initial source of dimensional data. In addition, anthropometric surveys of foreign military personnel are available (Refs. 49, 50, 51). The data of Hertzberg, et al. (Ref. 1) are used initially to synthesize reach capabilities and to determine link lengths. These reach capabilities have been determined for subjects categorized by stature and arm length.

Once the man-model is validated and a method of relating anthropometric measurements to link dimensions is developed, the use of other anthropometric surveys will be possible. This will entail the inputing of the dimensional characteristics of the new survey so that link dimensions (joint-center to joint-center distances) may be calculated.

Dempster, et al. (Ref. 54) have discussed the estimation of the radial and tibial links by measuring the corresponding bone lengths of live humans. These link dimensions can be obtained because the ends of these bones are readily palpable. The error inherent in this method is less than 2 percent. Unfortunately, the other links do not have palpable ends; hence, direct measurement using radiography is the only present technique available. The measurement techniques, the relationship between bone lengths and link lengths, and the relationship between radial and humeral links, and tibial and femoral links are also given.

Appendix B contains tables of anthropometric bivariant data. The surveys included are Hertzberg (Ref. 1), the 1967 USAF pilot population (in press), combined NATO data, and Naval Aviator data (Ref. 47). These data were furnished through the courtesy of the Anthropology Branch of AMRI, Wright-Patterson Air Force Base, Ohio, and the Air Crew Equipment Laboratory of NADC, Warminster, Pa.

3.1.1.1 Current Anthropometric Measurements

The surveys of conventional anthropometric measurements are adequately research and referenced in <u>The Human Body in Equipment Design</u> (Ref. 25). A reiteration of this excellent work would seem unnecessary. Selected measurements and dimensions are included in Table 1, however, to provide an immediate source of dimensional data. The corresponding pictorial descriptions are provided by Figs. 2 through 7.

3.1.2 Link Dimensions

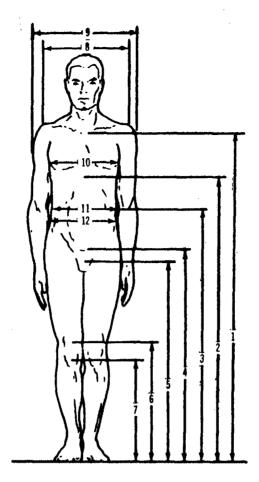
The links of BOFMAN-I, shown in Fig. 1, are named after the bones of the human skeleton which they most closely simulate. However, a bone is a

Table 1. Measurements of Girth

	<pre>Circumferences (in inches)</pre>	Source	Mean	Standard Deviation	5th Percentile	95th Percentile
	Head (euryon)	7	22.h7	0.62	21.0	24.3
HEAD (ELINY'OR)	Head (gonion)	11	18.62			
NEDA COMPUTATIONS NECK CHYRODIO CARTILAGE)	Neck (thyroid cartilage)	Н	% गा	0.7և	13.3	16.8
CWEST (AMILA)	Shoulder (sternal angle)	11	41.73			
OHEST OTHNISTERREN	Shoulder (axilla)	1	45.25	2.43	10.2	51.5
FI	Chest (nipple level)	1	38.80	2.45	33.7	14.8
PUBLIC BUTTOCK	Chest (xiphistermum)	11	35.94			
MODELLA		1	32.04	3.02	26.5	40.1
THE CALF MAX	Iliac Crest	11	33.03			
(may 3 Thomas ————————————————————————————————————	Buttock	7	37.78	2.29	33.0	43.5
NOTE OF THE PARTY	Thigh	1	22.39	1.74	18.3	26.14
MOMENTERED	Thigh (crotch)	11	22. LB			
AND AND A MENTAL FLAND		Н	17.33	1.41	14.2	20.9
POREMA BELOW	Mid-Patella	17	14.76			
OF SORKAN	Tibial Tuberosity	ן נו	13.39			
WHET (STYLOGG)	Calf (max.)	Н	14.40	0.96	12.2	16.7
	Ankle (min.)	F	8.93	0.57	7.8	10.5
	Foot, at. Floor		91, 1.9			

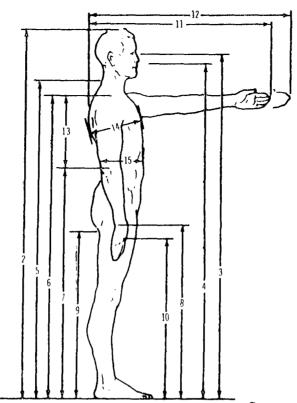
Table 1. Measurements of Girth (Cont)

Circumferences (in inches)	Source	Mean	Standard Deviation	5th Percentile	95th Percentile
Arm at Axilla	1	12.54	1.10	10.2	15.2
Mid-arm Flexed	1	12.79	1.07	10.5	15.4
Arm Above Med. Epicondyle Flexed	1	11.50	0.73	9.9	13.3
Forearm Below Med. Epicondyle	11	11.15			
Upper Third of Forearm	11	10.63			
Wrist (styloids)	1	6.85	o.lio	6.0	7.8



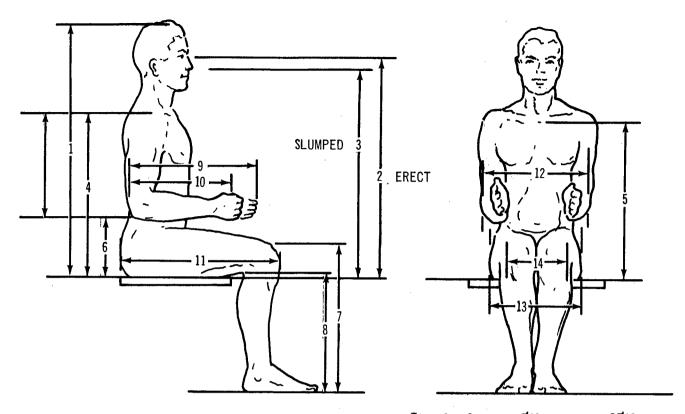
No.	Dimensions (in.)	Source	Mean	Standard Deviation	5th Percentile	95th Percentile
1	Top of Breastbone (Supra- sternale) Height	1	56 .2 8	2.19	52.7	59.9
2	Bottom of Breastbone (Substernale) Height	1	48.71	2.02	45.6	52.1
3	Waist Height	11	42.02	1.81	39.1	45.0
4	Upper Junction of Penis and Abdomen	1	34.52	1.75	31.6	37.4
5	Crotch (In-seam) Height	1	32.83	1.73	30.l ₄	35.7
6	Top Edge of Kneecap Height	ı	20.22	1.03	18.4	21.9
7	Knee Joint Height (Lower Leg Length)	2	17.94	1.12	16.1	19.8
8	Shoulder bone Breadth (Bi-acromion)	1	15.75	.74	14.6	16.9
9	Maximum Shoulder Breadth (Bi-Deltoid)	1	17.88	.91	16.5	19.4
10	Chest Breadth	1	12.03	.80	10.8	13.4
11	Waist Breadth	1	10.66	.94	9.4	12.3
12	Pelwis Width (Bi-iliac)	Ħ	11.40	.62	10.4	12.4

Figure 2. STANDARD NUDE STANDING DIMENSIONS



No.	Dimensions (in.)	Source	Mean	Standard Deviation	5th Percentile	95th Percentile
1	Weight (Nude) in Lbs.	1	163.66	20.86	132.5	200.8
2	Stature	1	69.11	2.44	65.2	73.1
3	Eye Height at Attention	1	64.69	2.3 8	60.8	68.6
4	Eye Height Relaxed (Based upon 1.2" normal slump)	3	63.48	?	?	?
5	Base of Neck (Cervicale) Height	1	59.08	2.31	55.3	62.9
6	Top of Shoulder (Acromion) Height	1	56 .5 0	2.28	52. 8	60.2
_7	Elbow (Radiale) Height	1	43. 50	1.77	40.6	46.4
8	Wrist (Stylion) Height	1	33.52	1.52	31.0	<u> 36.1</u>
9	Buttock Crease (Gluteal Furrow) Height	1	31.57	1.62	29. 0	34.3
10	Knuckle (Metacarpal III) Height	1	30.04	1.45	27.7	32.4
וו	Fingertip to Back (Shoulders Back)	1	34.59	1.65	31.9	37.3
12	Fingertip to Back (Shoulders Forward)	1	3 8.59	1.90	35.4	41.7
13	Top of Shoulder to Elbow	2	14.28	.81	12.9	15.6
1	Chest Depth	1	9.06	.75	8.0	10.կ
15	Waist Depth	1 1	7.94	.88	6.7	9.5

Figure 2. STANDARD NUDE STANDING DIMENSIONS (Cont)



No.	Dimension (in.)	Source	Mean	Standard Deviation	5th Percentile	95th Percentile
0	Elbow to Shoulder	1	14.32	0.69	13.2	15.4
1	Sitting Height	1	35.94	1.29	33.8	38.0
2	Eye Height, Erect	1	31.47	1.27	29.4	33.5
3	Eye Height, Relaxed Slump	3*	29.47	arramanaga magnasar - magnasaga arapmanaga ay ay inggan		eranga sakangga sakanggan da saka aya saka saka a
4	Top of Shoulder (Acromion) Height	1	23.26	1.14	21.3	25.1
5	Top of Sternum Height (Trunk Height)	2	23.01	1.17	21.1	24.9
6	Elbow Height	1	9.12	1.04	7.4	10.8
7	Top of Knee	1	21.67	.99	20.1	23.3
8	Back of Knee (Popliteus) Height	1	16.97	.77	15.7	18.2
9	Elbow to Finger Tips	1	18.86	.81	17.6	20.2
10	Elbow to Center of Grip	4	14.2	.79	13.0	15.5
11	Buttocks to Front of Knee	1 1	23.62	1.06	21.9	25.4
12	Outside of Elbows Breadth	1	17.28	1.42	15.2	19.8
13	Hip Breadth	1	13.97	.87	12.7	15.4
114	Outside of Knees Breadth	1	7.93	.52	7.2	8.8

^{*}Based on an average slump of 2.0" estimated by Ely et.al. (3).

Figure 3. STANDARD NUDE SITTING DIMENSIONS

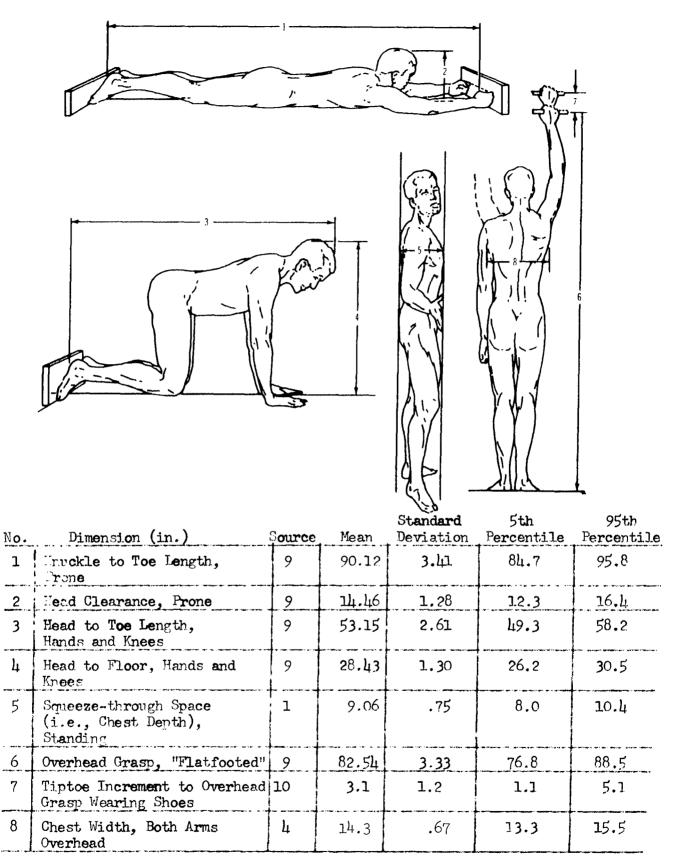
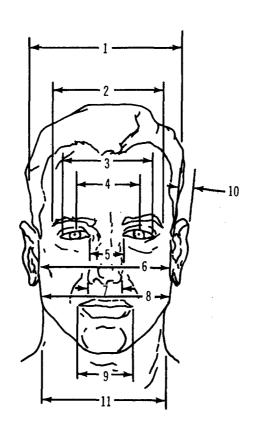
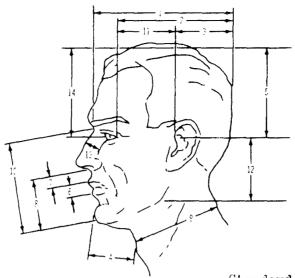


Figure 4. NUDE DIMENSIONS FOR SIMULATED WORKING POSTURES



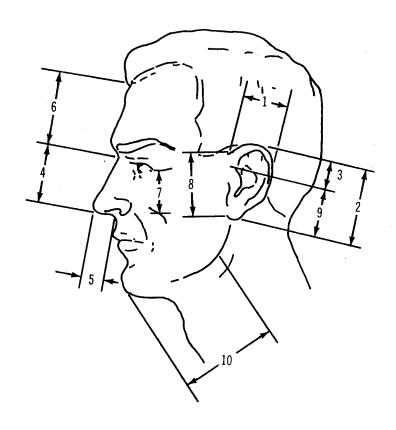
No.	Dimension (In.)	Source	Mean	Deviation	Percentile	Percentile
1	Head Breadth	1.	6.07	.20	5.74	6.40
2	Maximum Brow (Frontal) Diameter	1	4.71	.20	4.39	5.05
3	Outside Eye Corners (Biocular) Diameter	1	3.78	.17	3.48	14.06
4	Interpupillary Distance	1	2.49	.14	2.27	2.74
5	Inside Eye Corner (inter- ocular) Diameter	1	1.25	.1.0	1.09	1.42
6	Earhole-Earhole (Bitragion) Djameter	1	5.60	•21	5.3	5.9
7	Nose Breadth	1	1.31	.11	1.1 6	1.49
8	Maximum Jaw Width (Bigonial Diameter)	1 .	4.27	.22	3.9	4.6
9	Lip Length	1	2.03	. 7.14	1.81	2.27
10	Ear Protrusion	1	.84	.14	.63	1.10
ננ	N ec k Width	5	4.83	.27	4.38	5.27

Figure 5. STANDARD HEAD AND NECK DIMENSIONS



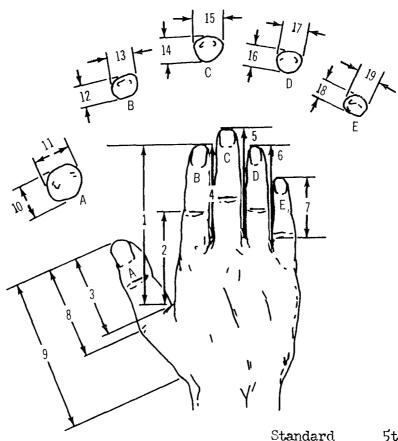
No.	Dimension (in.)	ource	Mea n	Standard Deviation	5th P erc ent ile	95th Percentile
1	Nasel Root to Back of Head (With Back of Head Against a Wall)	1	7.75	. 34	7.2	8.3
2	Outside Eye Corner (Exter- nal Canthus) to Back of Head (With Head Against a Wall)	1	6.78	.32	6.2	7.3
3	Ear Hole (Tragion) to Back of Pead (With Head Against a Wall)	1	4.03	.30	3.5	4.5
4	Chin (Menton) Projection	1	1.88	.26	1.5	2.3
5	Earhole to Top of Head (Tragion to Vertex: Head Height)	1	5.11	.30	4.6	5.6
6	Lip Margin to Lip Margin	1	.64	.12	.44.	.83
7	Upper Lip (Philtrum) Length	1	.77	.14	.54	.98
8	Bottom of Nose (Subnasale) to Chin (Menton)	1	2.63	.27	2.19	3.07
9	Neck Depth	<u> 5</u>	4.87	.34	l: . 31	5.h3
10	Top of Mose (Masion) to Point of Chin (Menton)	5	14.88	.26	4.45	5.31
11	Earhole (~ Tragion) to Outside Corner (Enternal Canthus) of Eye	5	3.25	.25	3.00	3.50
12	Earhole (Tragion) to Jaw Angle (Gonion)	5	2.89	.23	2.51	3.27
13	Top of Mose (Masion) to Incide Corner of Eye	5	.93	.08	.80	1.06
14	Eye Pupil to Top of Head	1.1	4.4	.30	3.9	5.1

Figure 5. STANDARD HEAD AND NECK DIMENSIONS (Cont)



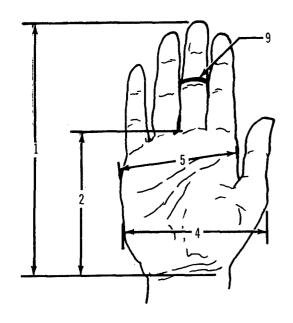
Mo.	Dimensi o n (in.) S	ource	Mean	Standard Deviation	5th Percentile	95th Percentile
1	Ear Breadth	1	بلا.1	.11	1.27	1.67
2	Ear Length	1	2.147	.16	2.21	2.73
3	Ear Length Above Ear Hole (Tragion)	1	1.17	.11	.99	1.35
4	Nose Length	1	2.01	.14	1.79	2.23
5	Nose Protrusion	1	.89	.11	.72	1.08
6	Hairline(Crinion) to Top of Nose (Nasion)	5	2.49	. 3 0	2.00	2.98
7	Outside Corner of Eye to Bottom Edge of Front of Cheek Bone	5	1.53	.13	1.32	1.74
8	Upper Ear-Cheek Junction to Lower Ear-Cheek Junction	5	1.97	.16	1.71	2.23
9	Ear Hole (≈ Tragion) to Lower Ear-Cheek Junction	5	1.25	.13	1.04	1.46
10	Jaw Angle (Gonion) to Point of Chin (Menton)	5	3.84	.23	3. lı6	4.22

Figure 5. STANDARD HEAD AND NECK DIMENSIONS (Cont)

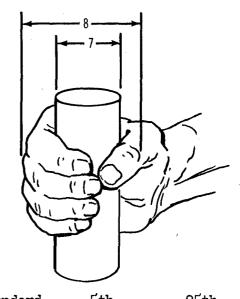


No.	Dimension (in.)	Source	Mean	Standard Deviation	5th Percentile	95th Percentile
	to an an analysis of the second secon	8			1	
1	Thumb Web to Index Fingertip		4.50	.30	4.00	5.00
2	Thumb Web to Second Knuckle, Index Finger	8	2.64	.26	2.22	3.06
3	Web to Tip of Thumb	8	2.32	.17	2. 03	2.61
14	Web to Tip of Index Finger	8	2.85	.20	2.52	3.18
5	Web to Tip of Middle Finger	8	3.32	.21	2.98	3.66
6	Web to Tip of Ring Finger	8	2.89	.17	2.61	3.17
7.	Web to Tip of Little Finger	8	2.20	.19	1.89	2.51
8	First Knuckle to Tip of Thumb	8	2.44	.13	2.23	2.65
9	Thumb Length	8	4.69	. 24	4.29	5.09
10	Thumb Thickness	8	.76	.04	.69	.83
11	Thumb Breadth	8	.94	.06	.84	1.04
12	Index Finger Thickness	8	.74	.04	.67	.81
13	Index Finger Breadth	8	.89	.04	.79	.93
14	Middle Finger Thickness	8	.77	.05	.69	.85
15	Middle Finger Breadth	8	.89	.04	.82	.96
16	Ring Finger Thickness	8	.72	.04	.65	.79
17	Ring Finger Breadth	8	.83	.04	.76	•90
18	Little Finger Thickness	8	.63	.04	.56	.70
191	Little Finger Breadth	8	.73	.04	.66	.80

Figure 6. STANDARD HAND DIMENSIONS



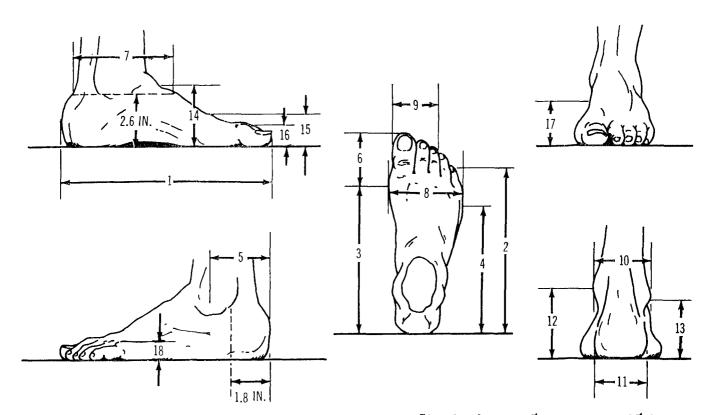






		Standard	5th	95th		
No.	Dimension (in.)	Source	Mean	Deviation	Percentile	Percentile
1	Hand Length	1	7.49	.34	6.9	8.0
_2	Palm Length	1	4.24	.21	3.89	4.60
3	First Joint Knuckle to Second Joint Knuckle Length, Middle Finger	1	2.67	.12	2.49	2. 85
4	Maximum Hand Breadth at Thumb	1	4.07	.21	3.73	4.42
5	Maximum Hand Breadth Across First Joint Kmuckles	1	3.48	.16	3.22	3.74
6	Minimum Thickness of First Knuckle, Middle Finger	1	1.17	.07	1.05	1.28
7	Thumb-Middle Finger-Touch Grip Diameter	1	1.90	.14	1.62	2.05
8	First Knuckle Middle Finger to Second Knuckle Thumb Grip Clearance for Thumb Middle Finger Touch Around 1.90" Cylinder	1	4.09	.2]	3.72	4.144
9	Middle Finger Hole Diameter	1	.86	.05	.79	•93

Figure 6. STANDARD HAND DIMENSIONS (Cont)



No.	Dimensions (Standing in.)	Source	Mean	Standard Deviation	5th Percentile	95th Percentile
1	Foot Length	1	10.50	.45	9.8	11.3
2	Heel to Tip of Small Toe Length	6	8.25	.41	7.6	8.9
3	Heel to Inside Ball of Foot Length	1	7.64	. 34	7.1	8.2
4	Heel to Outside Ball of Foot Length	6	6 .2 8	.37	5.7	6.9
5	Heel to Outside Ankle Bone (Lat. Malleolus)	7	3.32	.19	3.0	3.6
6	Inside Ball to Tip of Great Toe	6	2.78	.20	2.4	3.1
7	Ankle Length at 2.6" Above Sole	6	4.38	.2 6	3. 9	4. 8
8	Foot Breadth	1	3.80	.19	3. 5	4.1
9	Width of First Three Toes	6	2.75	.18	2.4	3.0
10	Width of Ankle Joint	1	2.95	.15	2.7	3.2
11	Heel Breadth, 1.8" from Back of Heel	6	2.75	.15	2.5	3.0
12	Inside Ankle Bone (Med. (Mall.) Height	1	3.45	.21	3.1	3.8
13	Outside Ankle Bone (Lat. (Mall.) Height	1	2.73	.22	2.4	3.1
14	Dorsal Arch Height	6	3.08	.21	2.7	3.4

Figure 7. STANDARD FOOT DIMENSIONS WHILE STANDING

No.	Dimensions (Standing in.)	Source	Mean	Standard Deviation	5th Percentile	95th Percentile
15	Inside Ball of Foot Height	6	1.53	.09	1.4	1.7
16	Great Toe Height	6	1.08	.10	.9	1.2
17	Sole of Foot (Plantar) Arch Height	6	1.12	.20	.8	1.4
18	Outside Ball of Foot Height	6	1.00	.08	•9	1.1

Figure 7. STANDARD FOOT DIMENSIONS WHILE STANDING (Cont)

complex biological material with many properties. In itself, it is not a link but its rigidity forms a functional dimension. The link in relation to the body system is a straight or core line which extends through a body segment and terminates at both ends in axes or hinge points. The adjacent members rotate about these axes.

From the standpoint of developing a stick-man or link-man model, the number of links is somewhat arbitrary. However, to reduce the complexity of the model, it may be desirable to ignore minor link movements and to group a chain of links into units (e.g., the 25 separate vertebral links above the sacrum into the lumbar link and the thoracic link). This was the approach taken by Dempster (Ref. 11) (See Figs. 8 and 9), based on the work of Harless (Ref. 13) and in the Boeing proposal to JANAIR. The link dimensions shown in Fig. 9 are for the 5th, 50th, and 95th percentile Air Force flying personnel.

As a first approach to a computerized man-model, the above concept appears quite reasonable. The differences between the link models of Dempster (Ref. 11) and Boeing are minor. BOFMAN-I includes joints on the spinal column and the eyes. The thoracic joint between the lumbar and thoracic links is located near the waist line, and only one joint is used at the shoulder in BOFMAN-I.

The shoulder joint arrangement of BOEMAN-I differs from that shown in the 1955 study of Dempster (Ref. 11) but agrees with the 1967 study, Dempster and Gaughran (Ref. 60). In Dempster (Ref. 11), the shoulder is simulated by two joints and a 3.5 cm connecting link called the scapular link. The subject report lists the scapular link as "an unsatisfactory

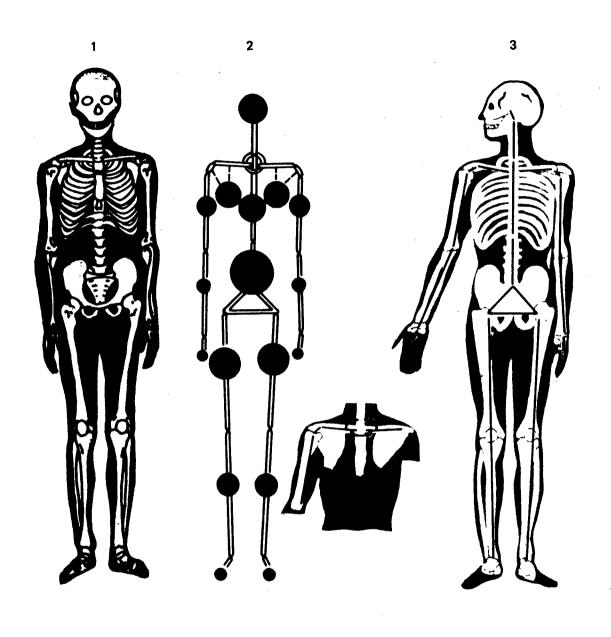


Figure 8. PLAN OF BODY LINKS AS DESCRIBED BY DEMPSTER

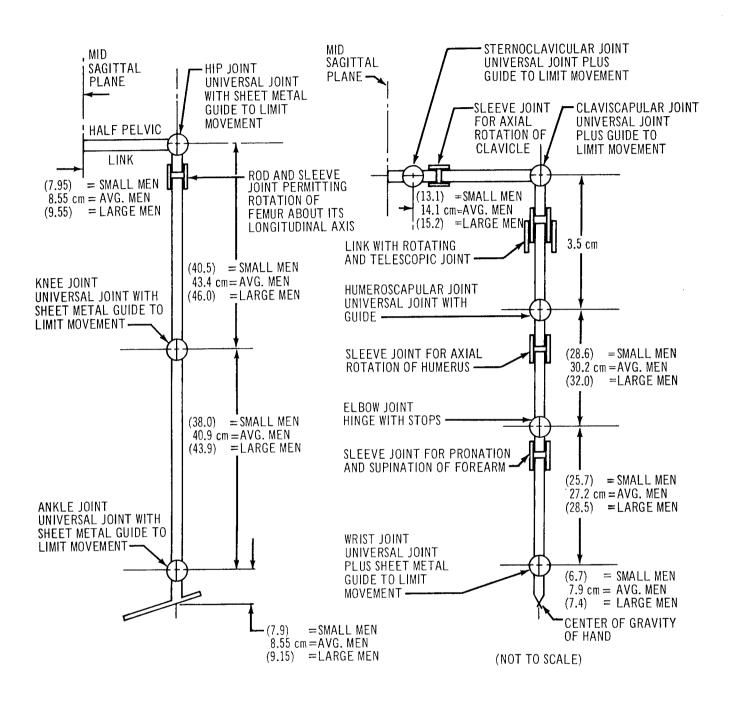


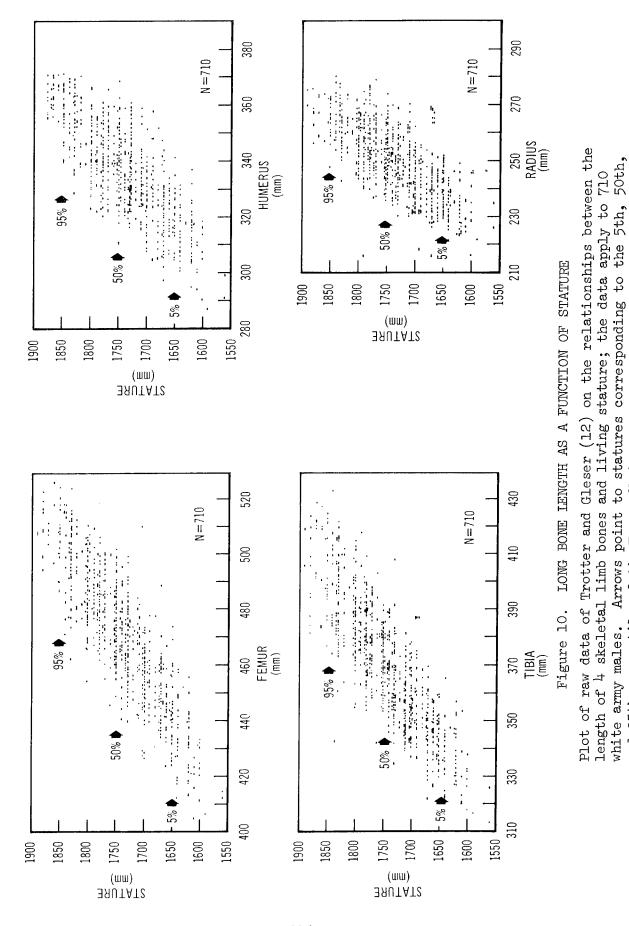
Figure 9. GENERAL LINK PLAN OF THE LOWER AND UPPER LINK SYSTEMS

From Dempster (Ref. 11)

measurement" of approximately 3.5 cm for all sized individuals. Preliminary evaluations of BOEMAN-I indicate the scapular link and a second
joint at the shoulder provide an unnecessary complication with no
increase in accuracy of joint location synthesis. The shoulder joint
for BOEMAN-I has been simplified by extending the clavicle 0.4 in to
mate with the humeral link in a single "shoulder joint"; i.e., the
clavicular joint now has zero degree of freedom. This makes the link
length compatible with external body dimensions and circumferences and
is represented by the dashed lines shown in Fig. 1.

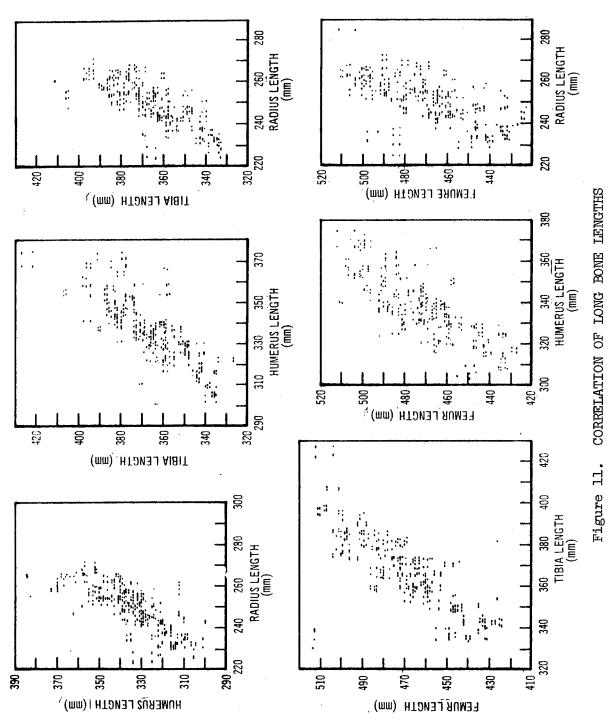
While the concept of a link man is reasonable, it must be realized that there are limitations to its applicability and that the dimensions of the links are somewhat variable. Dempster (Ref. 11) was most thorough in his analysis of the link dimensions of the limbs but there still remain some inherent limitations. The link dimensions for the limbs in Dempster (Ref. 11) are based, among other things, on the correlation between stature and four skeletal bones (humerus, femur, radius, and tibia) (See Fig. 10). Figures 10 and 11 help illustrate some of the variation inherent in the link dimensions.

In addition, Dempster (Ref. 11) discusses some of the limitations such as the variability in long bone length for any given stature of Army personnel, the variability of the centers of joint rotation, the variance in the joint radii as an inverse function of bone length, the use of only three pelves for the transpelvic link determination, etc. However, even with these limitations, the link dimensions appear reasonable and quite usable from an engineering standpoint.



and 95th percentile of Air Force flying personnel

D162-10126-1



(Comparable to 5th, 50th, and 95th percentiles of Air Force flying personnel) From raw data of Trotter and Glesser (12).

Dempster (Ref. 11) was primarily concerned with the seated operator and, hence, his limbs. Therefore, the link dimensions of the torso were not investigated. For BOFMAN-I, these torso dimensions were required and, hence, derived by Boeing research personnel from existing anthropometric data.

Table 2 gives the link dimensions for BOFMAN-I with values for the 1st, 50th, and 99th percentiles as well as standard deviations. Table 3 is from Dempster (Ref. 11) and gives some bone and link lengths for the 5th, 50th, and 95th percentiles as well as the relationships between the two measurements. Table 4 is from Dempster, et al. (Ref. 54) and gives regression equations relating upper and lower link lengths. The dimensions and standard deviations for link numbers 1 through 4 were taken from Hertzberg, et al. (Ref. 1). The dimensions for link numbers 11, 12, 13, 17, 18, 19, 20, and 21 were taken from Dempster (Ref. 11). The standard deviations for these links were calculated by averaging the differences between the dimensions reported for the 5th and 50th percentiles and the 50th and 95th percentiles and applying appropriate conversion factors.

Example:

Link #19 - Femoral Link:
$$\sigma = \frac{46.0 - 40.5}{2 \times 1.645} = 1.67 \text{ cm}$$

The dimension for link number 9 was assumed constant for all percentiles. The dimension for link number 18 (transpelvic) must be treated as a special case because the dimension is based on only three measurements, and does not have a normal distribution; hence, a standard deviation is not applicable. Its 1st and 99th percentile values were determined from

Table 2. Link Dimensions for BOEMAN-I

No.	Link	or CM	in	ls Percen		-	th ntile in		th ntile in
1	Stature	6.19	2.44	161.3	63.5	175.6	69.1	190.3	74.9
2	Eye Height, Standing	6.04	2.38	150.3	59.2	16և.և	64.7	178.5	70.3
3	Eye Height, Sitting	3.22	1.27	72 . lı	28.5	80.0	31.5	87.3	34.h
4	Interpupillary	0.36	0.14	5.5	2.2	6.3	2.5	7.2	2.8
5	Eyeball to Head	0.00	0.00	14.0	5.5	14.0	5.5	14.0	5.5
6	Head	0.23	0.09	14.7	5.8	15.2	6.0	15.7	6.2
7	Neck (Horizontal)	0.00	0.00	3.8	1.5	3.8	1.5	3.8	1.5
8	Neck (Vertical)	0.15	0.06	10.2	4.0	10.4	4.1	10.9	4.3
9	Inter-Clavicular	0.00	0.00	5.1	2.0	5.1	2.0	5.1	2.0
10	Clavicular*	0.64	0.25	13.7	5.4	15.2	6.0	16.5	6.5
11	Humeral	1.03	0.61	27.8	10.9	30•2	11.9	32.6	12.8
12	Radial	0.85	0.34	25.2	9.9	27.2	10.7	29.2	11.5
13	Hand (Wrist to Hand C.G.)	0.21	0.08	6.5	2.6	7.0	2.8	7.5	3.0
14	Hand (Extended)	0.86	0.34	17.0	6.7	19.0	7.5	21.0	8.3
15	Thoracic	0.94	0.37	29.7	11.7	31.8	12.5	34.0	13.4
16	Lumbar	0.32	0.13	4.0	1.6	4.6	1.8	5.3	2.1
17	Pelvic (Vertical)	0.62	0.25	7.9	3.1	9.3	3.7	10.7	4.2
18	Pelvic (Hori- zontal)	0.97	0.38	15.5	6.1	17.1	6.7	20.1	7.9
19	Femoral	1.67	0.66	39.5	15.6	43.4	17.1	47.3	18.6
20	Tibial	1.79	0.71	36.7	14.4	40.9	16.1	45.1	17.8
21 *Sho	Foot (Ankle to Floor) ulder link has zero					8.6 added to			3.7 h.

Table 3

Estimation of Some Link Dimensions of Air Force Flying Personnel Based on Ratios from Cadaver Measurements

	95th Percentile cm	50th Percentile . cm	5th Percentile cm
Clavicle length (40.7% of biacromial width)	17.6	16.3	15.1
Biacromial width Clavicle Link (86.4% of clavicle length)	43.1 15.2	40.1 14.1	37.0 13.1
	•	ternal end 26 m from midline	e)
Shoulder Link		<u>+</u> 3.5	
Humerus length Humerus Link (89.0% of humerus length)	35.9 32.0	33.9 30.2	32.1 28.6
Radius length Radius Link (107.0% of radius length)	26.6 28.5	25.4 27.2	24.0 25.7
Hand length Hand Link (wrist center to the hand center of gravity) (20.6% of humerus length)	20.4 7.4	19.0 7.0	17.6 6.7
Pelvic Link (horizontal component) (37.2% of femur length)		17.1	
Femur length Femur Link (91.4% of femur length)	50.3 46.0	47.5 43.4	44.3 40.5
Tibial length Tibial Link (110.0% of tibial length)	39.9 43.9	37.2 40.9	34.5 38.0
Foot length (heel to toe I) Foot Link (talus center point to center of gravity) (30.6% of foot length)	28.6	26.7	24.8
Vertical distance from midtalus to floor level		8.6	
Adapted from Dempster (Ref. 11)			

Table 4

Regression Equations Relating Link and Anthropometric Dimensions of the Upper and Lower Limbs

From Dempster, et al. (Ref. 54)

Prom Delighsoor, Co are (Mare 94)	Standard Error of	Correlation
Empirical Equation (mm)	Estimate	Coefficient
Ulna Length = 23.7922 + (0.9810 x Radius Length)	4.58	.94
Humerus Length = 64.4829 + (0.9683 x Radius Length)	9•97	.81
Radial Link Length = 1.0709 x Radius Length)		
Humeral Length = 58.0752 + (0.9646 x Radius Length)	8.92	.94
Radius Length = 7.9728 + (0.9002 x Ulna Length)	4.39	.94
Humerus Length = 74.0856 + (0.9688 x Ulna Length)	11.07	.76
Radial Link Length = 0.9870 x Ulna Length		
Humeral Link Length = 66.2621 + (0.8665 x Ulna Length)	9.90	.94
Femur Length = 125.6879 + (0.9067 x Tibia Length)	18.39	.73
Fibula Length = 31.3653 + (0.9252 x Tibia Length)	5.28	•97
Tibial Link Length = 1.0776 x Tibia Length	100 ton us.	
Femoral Link Length = 132.8253 + (0.8172 x Tibia Length)	16.57	•73
Femur Length = 101.8815 + (0.9629 x Fibula Length)	11.45	.87
Tibia Length = 8.6266 + (1.0119 x Fibula Length)	5.53	•97
Tibial Link Length = 8.2184 + (1.0904 x Fibula Length)	5.95	•97
Femoral Link Length - 92.0397 + (0.8699 x Fibula Length)	10.34	.87

Fig. 17. Fortunately, this dimension is not a critical part of the computerized man-model for cockpit geometry evaluation and the 50th or 99th percentile values can be used in the majority of applications when needed.

As previously reported, the thoracic joint was assumed to be located at the waist. The lumbar joint is located somewhere between the thoracic and hip joints. The vertical pelvic and lumbar link dimensions of BOEMAN-I were based on the assumption that the ratio of the lumbar link to the vertical pelvic link is 1:2 and that the total length of these two links is the difference between the standing waist height and the standing hip joint height. The standing waist height is reported in Hertzberg, et al. (Ref. 1), for the lst, 50th, and 99th percentiles. The standing hip height was determined by adding the dimensions of link numbers 19, 20, and 21 for the same three percentiles. The standard deviations for the two links were calculated from the lst and 99th percentiles.

The thoracic link is assumed to originate at the thoracic joint and terminate where it intersected the interclavicular joints. It should be noted that there is no joint at this intersection. The thoracic link was determined by taking the difference between the standing shoulder joint height, reported by Dreyfuss (Ref. 62) and the standing waist height of Hertzberg (Ref. 1). The standard deviation was calculated from the 1st and 99th percentile dimensions.

The neck joint was determined by finding a point from which an arc could be drawn which best approximated the arc movement of the eye from -67-1/2° to +90° (See Fig. 12). The horizontal distance from the eye to this point

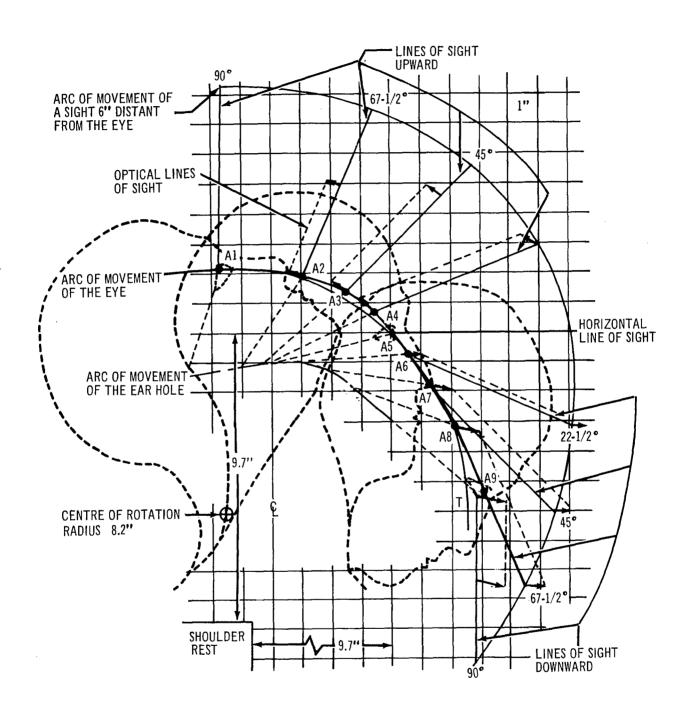


Figure 12. RANGE OF HEAD AND EYE MOVEMENTS IN THE VERTICAL PLANE (From Ref. 16)

is link number 5 and because of the lack of any statistical data, it is assumed constant for all percentiles. Dimension number 7 is based on the eye point being 4 inches ahead of the shoulder point as reported in MIL-STD-803A-3 (Ref. 15). Because link number 5 is constant for all percentiles, so is link number 7.

It was felt that seated and standing eye heights were critical as they provide an excellent reference point. Therefore, the difference between the standing eve height in Pertzberg (Pef. 1) and the computed shoulder height must be accounted for by vertical neck and head links (link numbers 6 and 8) for each percentile. From Fig. 12, the head link was available (vertical distance from the center of rotation to the horizontal line of sight) and, therefore, if this is assumed to be for the 50th percentile, a ratio of the head link to the neck link was available and this same ratio was applied to the 1st and 99th percentile dimensions needed to make the respective eye heights correct. Standard deviations were calculated from these values. It should be noted that Sutro, et al. (Ref. 52) have found that the horizontal and vertical centers of head rotation are not coincident and they suggest the use of a compromised center of rotation. At this time, it is felt that the critical movement in vision in an aircraft is the vertical movement; hence, for the present the neck joint will be retained as is. If future requirements indicate that separate centers of rotation would constitute a significant improvement, another joint can be inserted in the horizontal neck link to account for horizontal head movement. Based on the work of Sutro, et al. (Ref. 52), this joint would be located 2.06 inches inward from the present vertical center.

Figures 13 through 20 are of cumulative distributions on probability paper of some of the link dimensions based on the findings of Dempster (Ref. 11). A comparison of the 1st and 99th percentiles based on these figures is in reasonable agreement with those calculated and reported in Table 2.

3.1.3 Body Parameters

3.1.3.1 General

The BOEMAN-I program and the follow-on refinements require that certain body parameters be defined. These parameters are volume, density, mass, mass centers, and moments of inertia for the human body as a whole as well as for certain body segments.

These parameters, especially those for body segments of live humans, are difficult to obtain. There is a paucity of data available and the problem is further hindered by the fact that the majority of the investigations which have been conducted have used a small number of subjects, quite often cadavers whose body sizes were significantly smaller than the present population and the experimental methods are sometimes open to question. Dempster and Gaughran (Ref. 60) were quite critical of some of the older investigations. Only recently do we find the techniques and equipment developed which will permit reliable investigations on live humans with physical size comparable to that of today's flying personnel.

The relative proportions of the various body segments have been of interest since ancient times, particularly to those professions that had to select or classify subjects according to their body build. In the

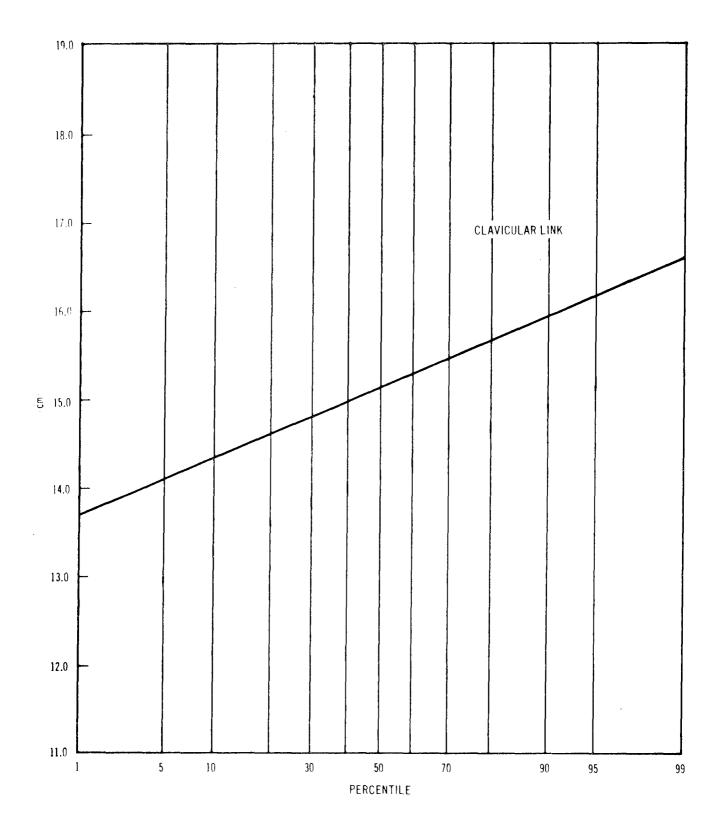


Figure 13. CUMULATIVE DISTRIBUTION OF CLAVICULAR LINK LENGTHS

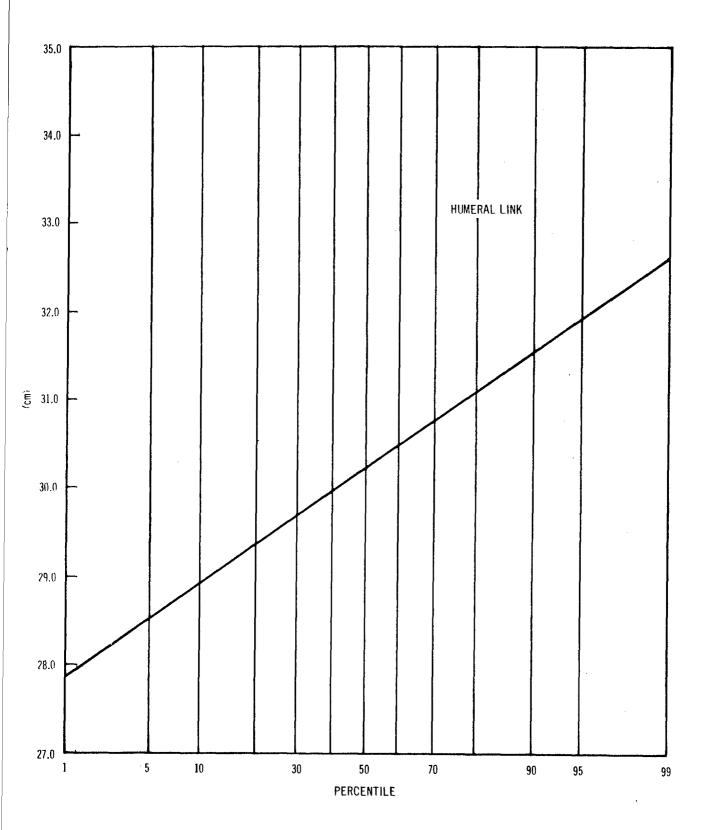


Figure 14. CUMULATIVE DISTRIBUTION OF HUMERAL LINK LENGTHS

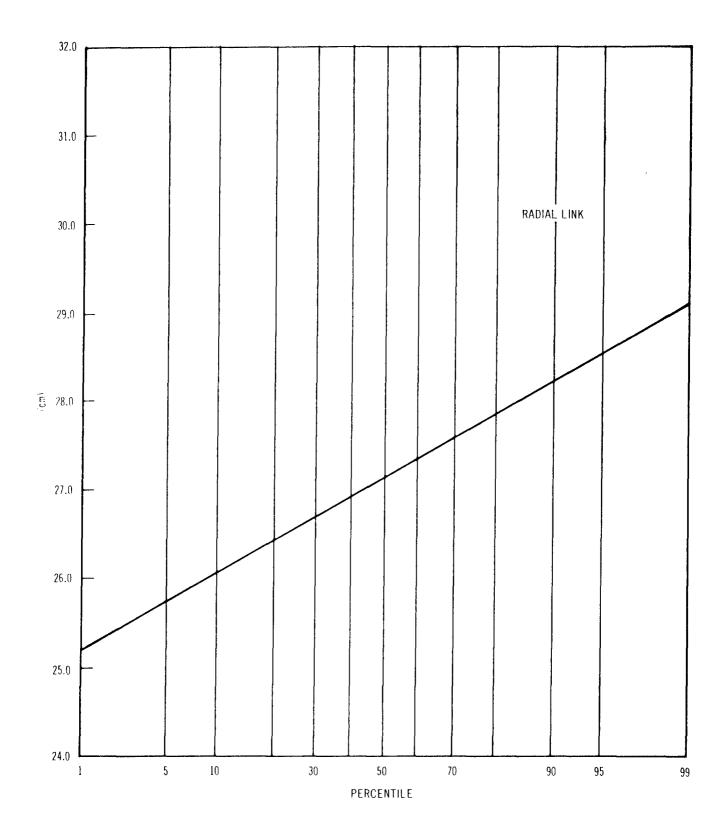


Figure 15. CUMULATIVE DISTRIBUTION OF RADIAL LINK LENGTHS

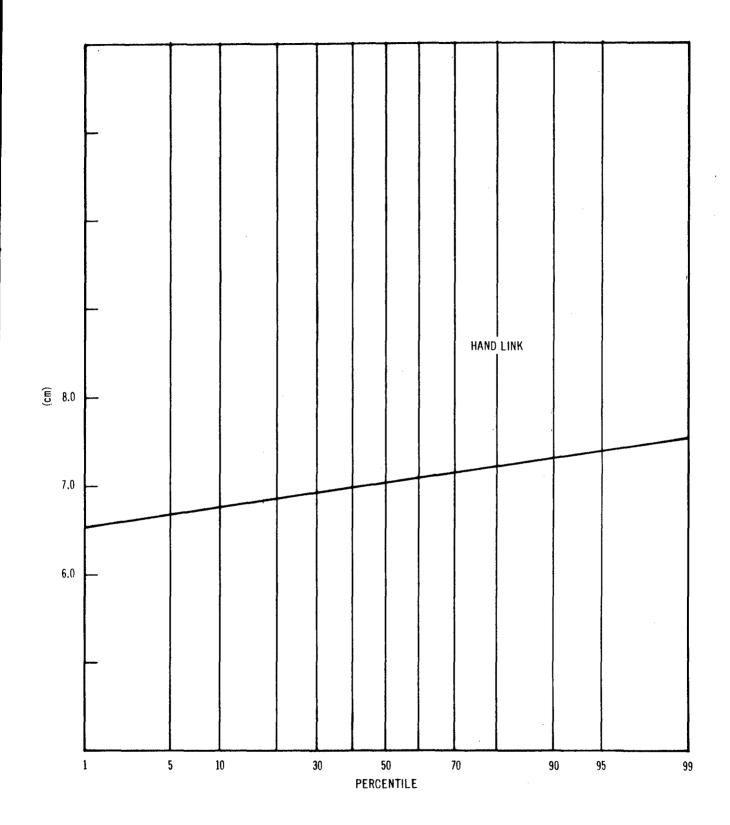


Figure 16. CUMULATIVE DISTRIBUTION OF HAND LINK LENGTHS

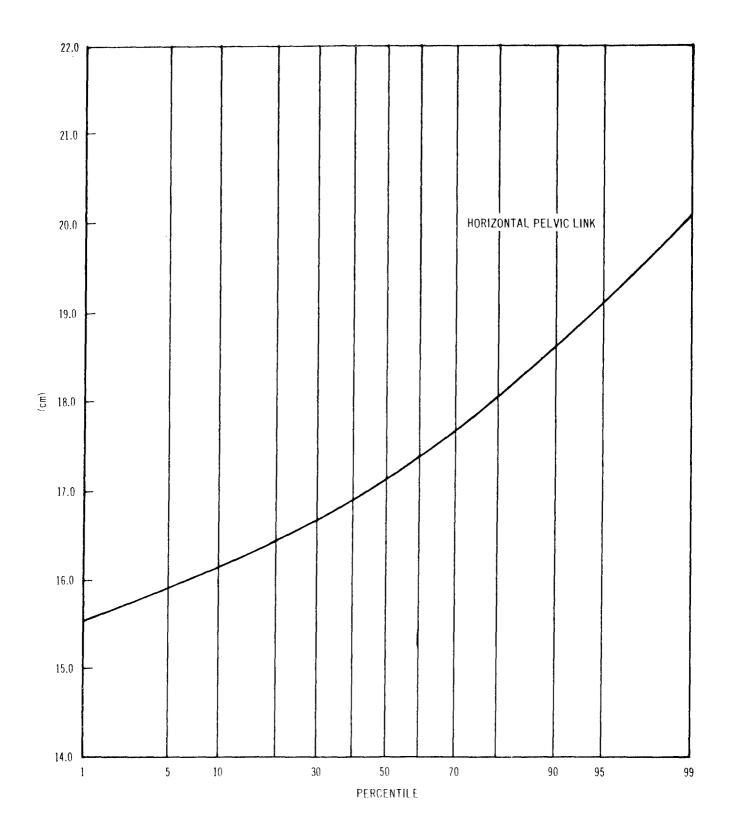


Figure 17. CUMULATIVE DISTRIBUTION OF HORIZONTAL PELVIC LINK LENGTHS

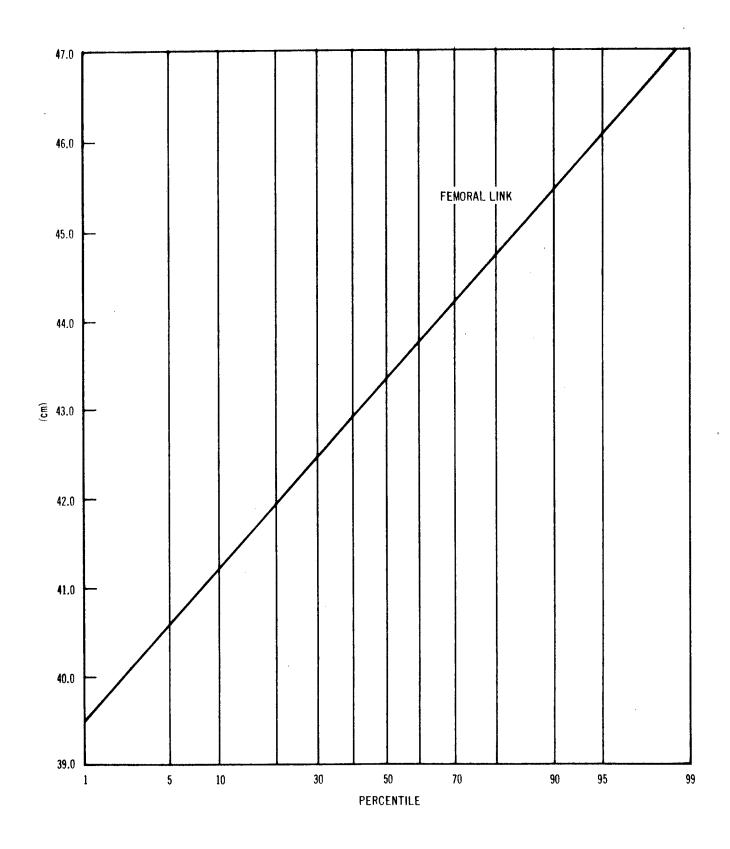


Figure 18. CUMULATIVE DISTRIBUTION OF FEMORAL LINK LENGTHS

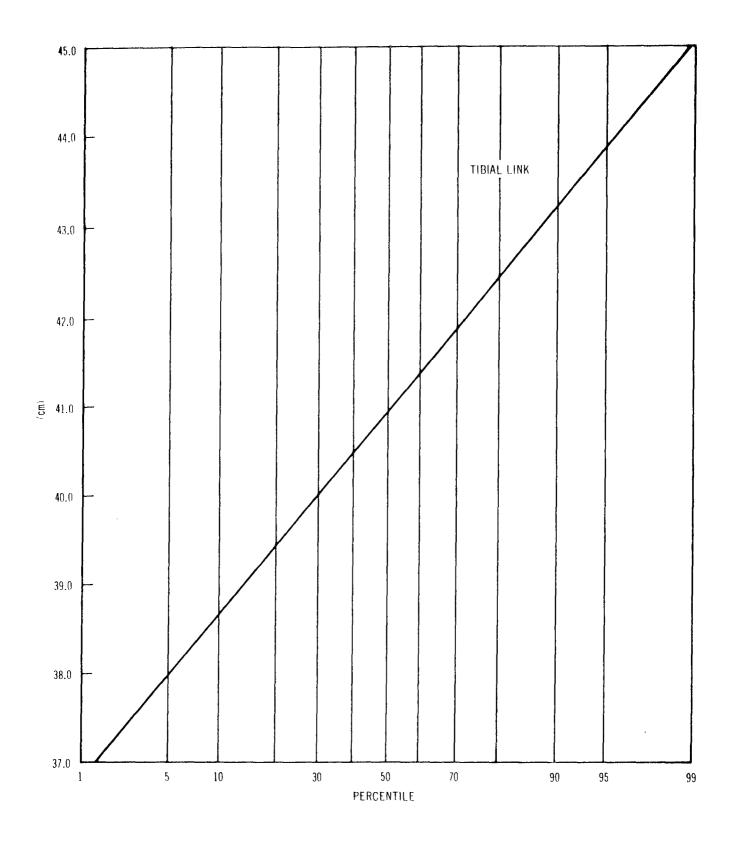


Figure 19. CUMULATIVE DISTRIBUTION OF TIBIAL LINK LENGTHS

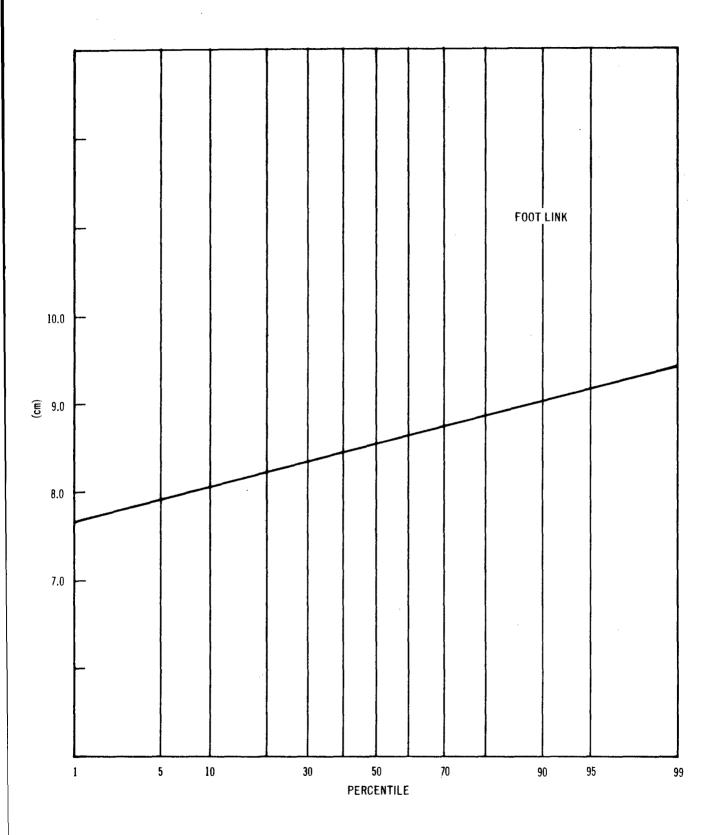


Figure 20. CUMULATIVE DISTRIBUTION OF FOOT LINK LENGTHS

beginning the interest was in the length relationships of the various body segments. The first modules were established by the Egyptians as far back as the third millenium before Christ. New standards were developed by Greek and Roman artists and architects and some such standards were attempted as late as the beginning of this century.

The determination of segment volumes or masses, however, was not attempted until the middle of the nineteenth century. The first of such studies was undertaken by Harless (Ref. 13) in Germany. He started his studies with the determination of the absolute and relative lengths of the body and its segments. From this he proceeded to the determination of the volume of body segments. He assumed for his studies that in any one segment its density or specific gravity is homogenous along its entire length. On this basis he was able to determine the absolute and relative masses of body segments.

For his investigations, Harless dissected five male cadavers and three female cadavers. His final report, in 1860, a treatise on "The Static Moments of the Human Body", used only the data gathered on two subjects. The results obtained by Harless were compared with those of others and those of the recent study by Drillis and Contini (Ref. 14).

In 1884, C. Meeh (Ref. 17) investigated body segment volumes of ten living subjects (8 males and 2 females).

In 1889, Braune and Fischer (Refs. 18, 19 and 20) made a very careful study of several cadavers. In the final report, the weight and height of the three male cadavers used were close to the average data of the German soldier of that period. Braune and Fischer (Ref. 19) introduced

for body parameter determinants the use of coefficients. They determined the masses of the various segments and measured their lengths from which they established three useful coefficients, ${\bf C_1}$, ${\bf C_2}$ and ${\bf C_3}$ which will be referred to several times later. The work of Braune and Fischer was so thorough that it has been used uncritically as a standard up until now, despite the fact that there exist pronounced differences in populations.

The most recent studies are those of Bernstein (Ref. 21) in Russia and Dempster (Ref. 11) and Drillis and Contini (Ref. 14) in the United States. With his co-workers at the Russian All-Union Institute of Experimental Medicine in Moscow, Bernstein in the 1930's carried out an extensive investigation of body segment parameters of living subjects. Excerpts of this investigation were published by him in his chapters on movement in the book "Physiology of Work", by Konradi, Slonim and Farfel.

Dempster (Ref. 11) conducted his studies at the University of Michigan from 1952 to 1954. His investigations were based on eight cadavers. Volume, mass, density, location of mass center and mass moments of inertia were reported. During the 1960's, Drillis and Contini (Ref. 14) performed studies at New York University.

3.1.3.2 Total Body Parameters

The studies of Braune and Fischer (Ref. 19), Fischer (Ref. 21), Harless (Ref. 13), Bernstein (Ref. 21), Dempster (Ref. 11), Weinbach (Ref. 32), etc., while technically well received, have been used sparingly in BOFMAN-I for the reasons given above. Thus, the small amount of data which is available has been reduced even further. For BOEMAN-I, the majority of the body parameter data have been obtained from Drillis and Contini (Ref.

14), Santschi, et al. (Ref. 23) and DyBois, et al. (Ref. 24). The latter two computed moments of inertia and centers of gravity of the whole living human body.

In the studies by Santschi, et al. (Ref. 23), and DuBois, et al. (Ref. 24), a compound pendulum technique was used to determine total body centers of gravity and moments of inertia. The only assumption was mean body density to compute a small second-order buoyancy correction factor. Figure 21 shows the reference landmarks for the location of the whole body center of gravity. Table 5 and Fig. 22 give a description of the body positions used in the investigation. The Santschi, et al. (Ref. 23) study gives total body centers of gravity and moments of inertia for eight body positions for 66 semi-nude subjects. Figure 23 shows a scattergram of statures and weights of the subjects used. Table 6 gives the mean and standard deviations of the center of gravity and moments of inertia of the semi-nude subjects and Table 7 gives correlation equations of moments of inertia with stature and weight. Figure 24 is a pictorial representation of the center of gravity data from Table 6.

DuBois, et al. (Ref. 24) conducted a similar study with 19 subjects dressed in both pressurized and unpressurized flying suits in a seated body position. Figure 25 is a scatter diagram of statures and weights of the subjects used. Table 8 gives the mean and standard deviations of the centers of gravity and moments of inertia. Table 9 gives correlation equations of moments of inertia with stature and weight.

Figure 26 is a pictorial representation of the center of gravity data from Table 8. Table 10 provides results of the statistical analysis of

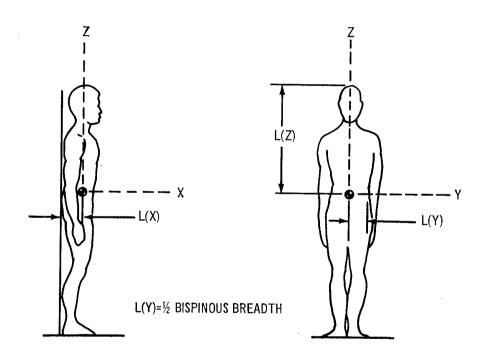


Figure 21. REFERENCE LANDMARKS FOR LOCATION OF TOTAL BODY CENTERS OF GRAVITY

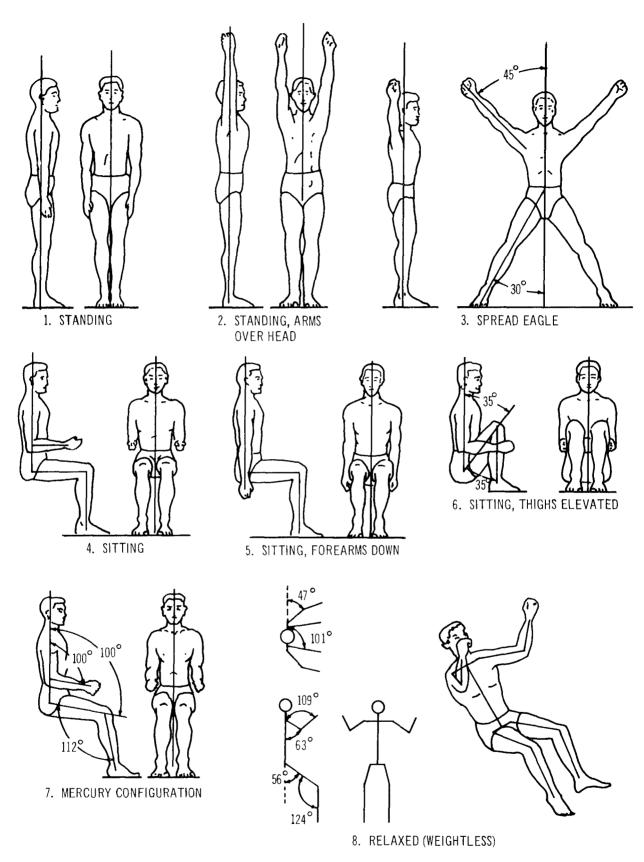


Figure 22. ILLUSTRATIONS OF THE BODY POSITIONS FOR CENTER OF GRAVITY AND MOMENT OF INERTIA MEASUREMENTS

SELECTION OF SUBJECTS (NUDE)

The sample of 66 male subjects was selected on the basis of stature and weight from North American Aviation employees to represent the Air Force population stature and weight characteristics described in Reference 1. For this total sample whose stature-weight scattergram is shown in Figure 7, 60 subjects are contained within the bounds of 1st and 99th percentile values of stature and weight and 50 within the area bounded by the 5th and 95th percentile values. The stature-weight correlation coefficient value for the total sample is approximately 0.6, in comparison with the Air Force population value of approximately 0.5 reported in Reference 6.

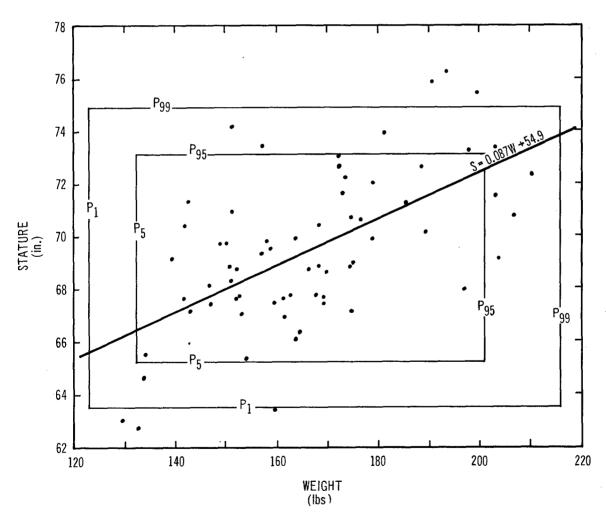
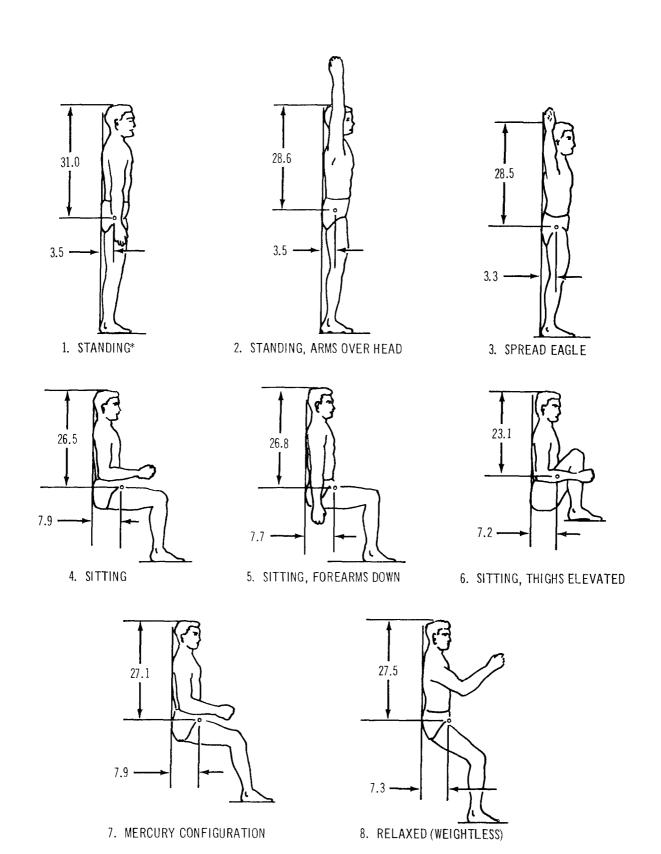


Figure 23. SCATTERGRAM OF STATURES AND WEIGHTS OF 66 MALE SUBJECTS USED TO DETERMINE CENTERS OF GRAVITY AND MOMENTS OF INERTIA



*DIMENSIONS ARE IN INCHES.

BODY SYMMETRY WITH RESPECT TO THE SAGITTAL PLANE IS ASSUMED.

Figure 24. ILLUSTRATIONS OF MEAN CENTERS OF GRAVITY OF SEMI-NUDE MALES IN EIGHT BODY POSITIONS

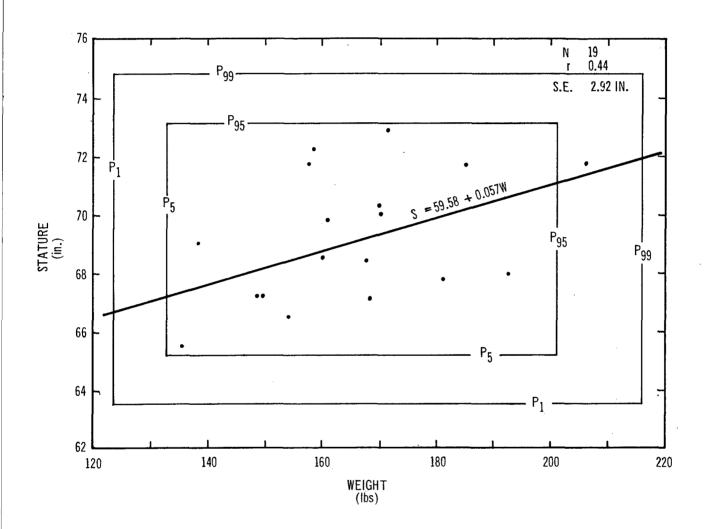
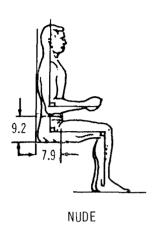
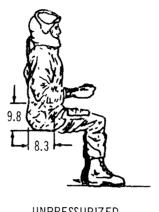
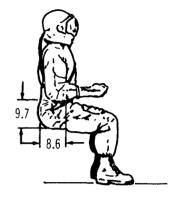


Figure 25. SUBJECT STATURE-WEIGHT SCATTERGRAM OF 19 PRESSURE SUITED MALES USED TO DETERMINE CENTERS OF GRAVITY AND MOMENTS OF INERTIA

From DuBois, et al. (Ref. 24)



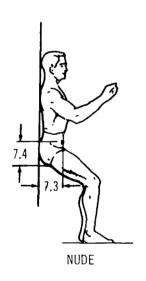


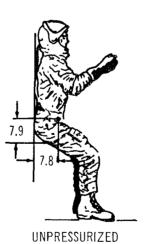


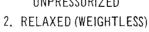
UNPRESSURIZED

1. SITTING









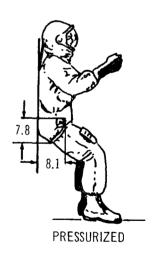


Figure 26. ILLUSTRATION OF MEAN CENTERS OF GRAVITY OF SEMI-NUDE AND PRESSURE SUITED MALES IN A SEATED POSITION

From DuBois, et al. (Ref. 24)

differences in moments of inertia between semi-nude, unpressurized, and pressurized subjects in a seated position.

While the thoroughness and attention to detail are apparent in the Santschi, et al. (Ref. 23) and DuBois, et al. (Ref. 24) reports, there remain unanswered questions. Duggar (Ref. 25) has suggested that there is a possibly significant damping effect of the muscles and joints. Also, assignment of coordinates of the center of gravity to one posture which were derived from measurements in another position (standing versus supine) must detract from the overall accuracy.

The method used by Drillis and Contini (Ref. 14) to determine the mass center of the whole body is one which employs a second class lever. In order to determine the X and Y coordinates (in a horizontal plane) of the whole body mass center, the subject is placed erect with his hands by his side on a board supported by a weighing scale at one end. Knowing the weight of the subject and the distance between supports, the scale reading establishes the line of action of the subject's weight, hence that of his center of mass.

Anthropometric data on the sample (Drillis and Contini (Ref. 14)) are given in Table 11. From these data a comparison between the sample and the population of Air Force personnel is obtained. Figure 27 illustrates the height and weight of the test sample along with those of previous investigators. The mean values differ significantly from that of the test sample. It would appear that the use of these other data would not be appropriate in studies concerned with United States adult males within the given age range and may not be appropriate even for other living populations.

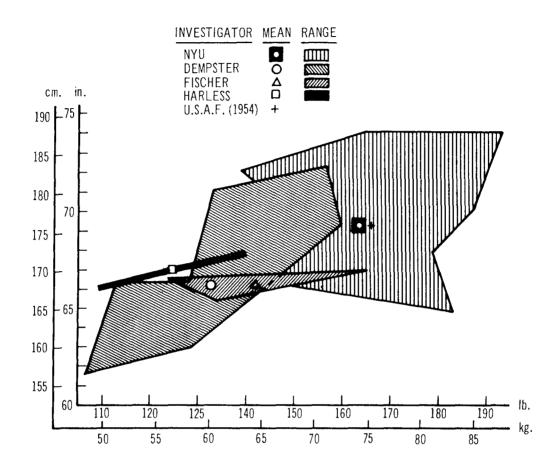


Figure 27. COMPARISON OF STATURE AND WEIGHT DATA OF VARIOUS INVESTIGATORS
From Drillis and Contini (Ref. 14)

Table 5

Description of Body Attitude Positions Investigated in Total Body Center of Gravity and Moment of Inertia Studies

1. Standing Subject stands erect with head oriented in the Frankfort plane and with arms hanging naturally at the sides as described in WADC TR 52-321 stature measurement (Ref. 1).

2. Standing, Arms Over Head Legs, torso and head same as position 1; upper extremities raised over head, parallel to Z-axis; wrist axes parallel to X-axis; hands slightly clenched.

3. Spread Eagle

Torso and head same as position 1; subject against plane parallel to YZ plane; arms at 45° with Z-axis, legs at 30° with Z-axis; wrist axes parallel to YZ plane; hands slightly clenched.

4. Sitting

Upper legs and forearms parallel to X-axis; upper arms, lower legs and spine parallel to Z-axis; soles parallel to XY plane; wrist axes parallel to Z-axis; head in Frankfort plane.

5. Sitting, Forearms Down Same as position 4, except forearms parallel to Z-axis, wrist axes parallel to X-axis.

6. Sitting, Thighs Elevated Same as position 4, except upper leg angle approximately 35° with YZ plane.

7. Mercury Configuration Same as position 4, except 100° back-thigh angle, thigh-leg angle 112°, forearm parallel to thigh.

8. Relaxes (Weightless) Position predicted to be assumed*by a human, relaxed in the weightless state.

(See Fig. 27)

^{*} Unpublished study by K. W. Kennedy, Anthropology Branch, Behavioral Sciences Laboratory, 6570th Aerospace Medical Research Laboratories, Wright-Patterson Air Force Base, Ohio.

Table 6

Centers of Gravity and Moments of Inertia of Semi-Nude

Males in Fight Positions

		Axis	Center of Gravity (in.)		Moment of Inertia (lb.in.sec. ²)		
			Mean	S.D.	Mean	S.D.	
1.	Standing	х У 7.	3.5 4.8 31.0	0.20 0.39 1.45	115.0 103.0 11.3	19.3 17.9 2.2	
2.	Standing, Arms Over Head	x y z	3.5 4.8 28.6	0.22 0.39 1.33	152.0 137.0 11.1	26.1 25.3 1.9	
3.	Spread Eagle	x y z	3.3 4.8 28.5	0.19 0.39 1.90	151.0 114.0 36.6	27.1 21.3 7.9	
¥.	Sitting	x y z	7.9 4.8 26.5	0.36 0.39 1.14	61.1 66.6 33.5	10.3 11.6 5.8	
5.	Sitting, Forearms Down	x ,y z	7.7 4.8 26.8	0.34 0.39 1.16	62.4 68.1 33.8	9.7 12.0 5.9	
6.	Sitting, Thighs Elevated	x y z	7.2 4.8 23.1	0.37 0.39 0.78	39.1 38.0 26.3	6.0 5.8 5.1	
7.	Mercury Configuration	x ,y z	7.9 4.8 27.1	0.34 0.39 1.14	65.8 75.2 34.2	10.3 14.0 5.6	
8.	Relaxed (Weightless)	x y z	7.3 4.8 27.5	0.33 0.39 1.44	90.2 88.2 35.9	13.3 13.3 5.4	

Sample Size 66

Mean Age 33.2 yrs. S.D. Age 7.2 yrs.

Mean Weight 166.4 lbs. S.D. Weight 19.8 lbs.

Mean Stature 69.4 in. S.D. Stature 2.9 in.

Table 7

Correlation of Moment of Inertia with Stature and Weight of Semi-nude Males in Fight Body Positions

		Axis	R i.sw	S.E.	Io Regression Equations *
1.	Standing	x ÿ z	0.98 0.96 0.93	4.18 5.27 0.84	-232.0 + 3.778 + 0.512W -212.0 + 3.438 + 0.460W -0.604 - 0.6988 + 0.112W
2.	Standing, Arms Over Head	х У z	0.98 0.96 0.89	5.63 6.89 0.87	-328.0 + 5.36S + 0.652W -332.0 + 5.34S + 0.589W 1.4 - 0.085S + 0.094W
3.	Spread Fagle	х У z	0.98 0.96 0.93	4.90 6.24 2.82	-353.0 + 5.638 + 0.677W -270.0 + 4.308 + 0.516W -101.0 + 1.528 + 0.191W
14.	Sitting	х У z	0.92 0.92 0.97	4.01 4.51 1.45	- 91.6 + 1.43s + 0.322W -135.0 + 2.26s + 0.268W - 52.8 + 0.76s + 0.201W
5.	Sitting, Forearms Down	х У z	0.91 0.92 0.97	3.98 4.67 1.36	- 78.7 + 1.29S + 0.309W -127.0 + 2.05S + 0.321W - 53.7 + 0.765S + 0.206W
6.	Sitting, Thighs Elevated	x y z	0.89 0.77 0.92	2.79 3.66 2.00	- 33.8 + 0.5438 + 0.212W - 22.2 + 0.4348 + 0.180W - 30.4 + 0.3288 + 0.204W
7.	Mercury Configuration	x y z	0.93 0.94 0.96	3.75 4.96 1.64	- 9h.3 + 1.578 + 0.308w -175.0 + 2.858 + 0.318w - 45.0 + 0.668s + 0.197w
8.	Relaxed (Weightless)	x y z	0.96 0.94 0.96	3.71 4.54 1.54	-106.0 + 1.778 + 0.452W -139.0 + 2.438 + 0.352W - 47.2 + 0.7768 + 0.176W

Sample Size 66

$$r_{sw} = 0.60$$
 S.E. = 2.33 in. S = 54.9 + 0.087W

S in in.

W in 1b.

^{*} Io and S.E. in lb.in.sec.²

Table 8

Centers of Gravity and Moments of Inertia of Semi-Nude and Pressure Suited Males in a Seated Position

		Axis	Center of Gravity (in.)		Moment of Inertia (lb.in.sec ²)	
			Mean	S.D.	Mean	S.D.
1.	Sitting					
	Nude	x	7.89	0.41	56.3	8.22
		y z	4.79 9.16	0.27 0.29	66.5 28.3	9.98 5.10
	Unpressurized	x	8.33	0.39	67.5	9.16
		y z	4.79 9.76	0.27 0.30	82.8 33.6	11.30 5.72
	Pressurized	x y z	8.62 4.79 9.70	0.38 0.27 0.28	68.8 82.4 34.0	8.70 11.30 5.72
2.	Relaxed (Weightless)					
	Nude	x y z	7.34 4.79 7.39	0.38 0.27 0.42	99.2 89.8 31.2	14.20 15.20 5.04
	Unpressurized	x y z	7.81 4.79 7.86	0.30 0.27 0.45	118.0 114.0 36.2	15.30 15.0 5.03
	Pressurized	x y z	8.08 4.79 7.81	0.29 0.27 0.48	118.0 114.0 36.1	15.20 15.70 4.85

Mean Age 27.4 yrs. S.D. Age 5.3 yrs.

Mean Weight 164.6 lbs. S.D. Weight 17.4 lbs.

Mean Stature 69.0 in. S.D. Stature 2.3 in.

Mean Clothing Weight 23.2 lbs. S.D. Clothing Weight 0.5 lb.

From DuBois, et al. (Ref. 24)

Table 9

Correlation of Moment of Inertia with Stature and Weight of Semi-nude and Pressure Suited Males in a Seated Position

		Axis	R i.sw	S.E.	Io Regression Equation
1.	Sitting				
	Nude ϵ	x y z	0.95 0.91 0.97	2.67 4.07 1.17	-105.0 + 1.598 + 0.317W -135.0 + 2.108 + 0.344W - 70.4 + 0.9238 + 0.212W
	Unpressurized	x y z	0.93 0.97 0.97	3.42 2.77 1.47	-114.0 + 1.825 + 0.337W -181.0 + 2.965 + 0.362W - 79.5 + 1.095 + 0.229W
	Pressurized	х у z	0.93 0.94 0.96	3.24 3.79 1.53	-120.0 + 2.06s + 0.281W -157.0 + 2.54s + 0.389W - 78.1 + 1.07s + 0.230W
2.	Relaxed (Weightless)				
	Nude	x y z	0.97 0.95 0.94	3.30 4.60 1.75	-191.0 + 2.88s + 0.556w -265.0 + 4.04s + 0.461w - 46.0 + 0.567s + 0.231w
	Unpressurized	x y z	0.95 0.96 0.96	4.62 4.38 1.33	-197.0 + 3.198 + 0.574W -217.0 + 3.598 + 0.506W - 54.8 + 0.8018 + 0.217W
	Pressurized	x y z	0.97 0.96 0.96	3.93 4.44 1.36	-208.0 + 3.425 + 0.550W -254.0 + 4.185 + 0.482W - 48.7 + 0.7205 + 0.214W
rsw		02 in.	S = 59	.58 + 0.	057 w

^{*}Io and S.E. in lb.in.sec.²

S in in.

W in 1bs.

From DuBois, et al. (Ref. 24)

Table 10

Tests for Significant Differences Among Moments of Inertia of Semi-Nude, Unpressurized, and Pressurized Males in a Seated Position

			t - Value	5
		I _x	$\mathtt{I}_{\mathbf{y}}$	$I_{\mathbf{z}}$
1.	Sitting			
	Nude - Unpressurized	3 . 863 *	4.583*	2,967*
	Nude - Pressurized	4.424*	4.512*	3.161*
	Unpressurized - Pressurized	0.428	0.083	0.184
2.	Relaxed (Weightless)			
	Nude - Unpressurized	3 . 750 *	4.736*	2.982*
	Nude - Pressurized	3.873*	4.639*	2.941*
	Unpressurized - Pressurized	0.098	0.022	0.094

*Significant (t 0.01 = 2.720, t 0.05 = 2.028)

From DuBois, et al. (Ref. 24)

Anthropometric Data on the Test Sample of Drillis and Contini

Subject	Age (yrs.)	Height (H	(H) (cm.)	Weight (W) (1bs.)	(W) (kg.)	Body Index C = H W-1/3	Somatotype Classifications
1. M.B.	22	74.00	188.0	193.5	87.77	12.78	4.5 - 4.5 - 4.0
2. T.A.	20	70.00	177.8	187.5	85.05	12.24	5.0 - 4.5 - 2.5
3. K.B.	28	68.25	173.4	179.0	81.19	12,10	5.0 - 4.0 - 2.0
4. F.A.	37	74.0	138.0	165.0	74.84	13.50	2.0 - 4.0 - 6.0
5. R.C.	23	64.75	164.5	162.0	73.48	11.40	5.0 - 5.0 - 1.0
6. D.W.	39	68.75	174.6	160.0	72.57	12.66	4.5 - 4.0 - 2.5
7. H.G.	25	69.75	177.2	153.0	04.69	13.04	4.0 - 4.0 - 3.0
8. А.Н.	23	68.00	172.7	152.5	69.17	12.71	4.5 - 3.5 - 2.5
9. A.M.	59	0.99	167.6	152.0	68.95	12.36	3.5 - 5.5 - 1.0
10. C.H.	22	69.50	176.5	151.5	68.72	13.04	4.0 - 4.0 - 3.0
11. R.B.	35	66.25	168.3	147.5	06.99	12.52	3.0 - 5.5 - 1.5
12. N.S.	23	72.00	182.9	139.0	63.05	13.93	2.5 - 3.5 - 5.0
Range	20	64.75	164.5	139.0	63.05	11.40	
	39	74.00	188.0	193.5	87.77	13.93	
Mean	07.0	76 09	30 321	88 ואר	5	97 04	
7545	C. • C.	7.50	٠٠٠٠١٦	00.101	13,42	44.09	
Standard Deviation	6.5	2.83	7.19	16.693	7.572	.661	

Figures 28 and 29 show the cumulative frequency curve for the body height and weight measurements of the selected population based on Hertzberg's data (Ref. 1). It is readily apparent that the height limit of this population varies approximately between 63 and 77 inches. The median is just over 69 inches. The cumulative frequency curve for the weight data for the same population show the weight limits vary approximately between 120 and 230 pounds with the median value of about 160 pounds.

To find the Z coordinate of the center of mass, the subject is placed supine on the board and the scale reading is taken. The principle of moments then gives the coordinates of the center of mass of the system. Since the weight and mass centers of the supporting structures are shown, the subject's mass center can be found by resolution of the loading forces.

Again, however, assignment of coordinates of the center of gravity to one posture which were derived from measurements in another position (standing versus supine) must detract from the overall accuracy.

This method has been used by New York University since 1950 (Ref. 26).

The torsional table can also serve as a tool for mass center distribution of the whole body. The data obtained by each method are presented in Table 12 and they indicate close agreement.

There are indications that body density displays some temporal changes during the seasons and depends on training progress or regress. The data collected by Boyd (Ref. 27), Brozek (Ref. 28), and others suggest that, in general, the body density tends to increase from birth up to the age of 20 to 27 years. The increase of body density is probably due to growth of the muscular tissues. According to Brozek (Ref. 28), the average density

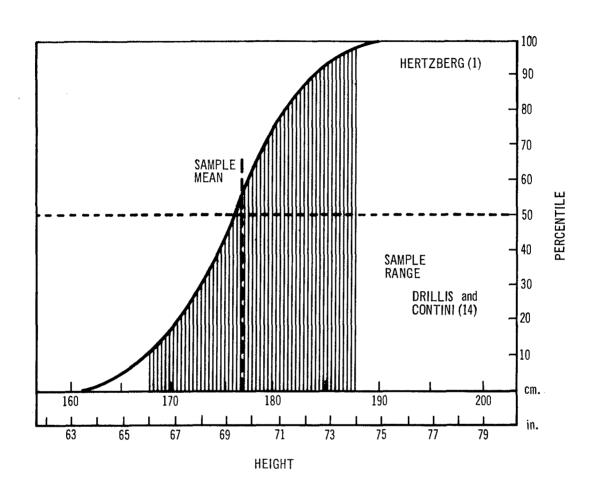


Figure 28. CUMULATIVE DISTRIBUTION OF BODY HEIGHT OF FLYING PERSONNEL COMPARED TO THE TEST SAMPLE OF DRILLIS AND CONTINI

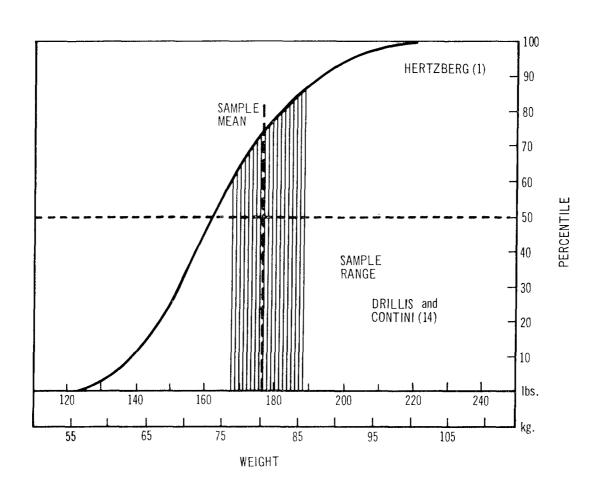


Figure 29. CUMULATIVE DISTRIBUTION OF BODY WEIGHT OF FLYING PERSONNEL COMPARED TO THE TEST SAMPLE OF DRILLIS AND CONTINI

Table 12

Location of the Mass Center of the Whole Body

(In Percentage of Body Height)

Subject		Reaction Board		Torsional Table		Average
т.А.		55.0	-	55.7		55.35
F.A.		55.8		56.8		56.30
K.B.		57.0		57.9		57.45
M.B.		56.8		55.8		56.30
R.B.		55.1		56.3		55.70
R.C.		56.4		54.7		55.55
H.G.		55.7		55.9		55.80
A.H.		61.9		58.9		60.40
C.Y.H.		59.1		56.1		57.60
A.M.		57.2		57.2		57.20
N.S.		55.9		55.9		55.90
D.W.		55.8		57.5		56.64
ange	from	55.0	from	54.7	from	55.35
	to	61.9	to	58.9	to	60.40
lean		56.81	a digendi en dirección de adecesión el Pr	56.56		56.68
tandard eviation	- avvey, gardin His His Him Him His His His	1.95	er staat villet in 1860 er 1860 - en 1860 er 1	1.15		1.39

on 153 male subjects shows that there is a decrease from 1.072 at age twenty years to 1.0% at age fifty-five years. The average body density of 62 female subjects indicated a decrease from 1.0% at twenty years to 1.016 at fifty-six. The density decrease, it seems, is due to the increase of the relative mass of body fat tissues.

The density formula developed by the Biomechanics Group of the School of Fingineering and Science, New York University, is based on data obtained by A. R. Behnke, et al. (Ref. 29) in 1942. The values of specific gravity were obtained by weighing 99 healthy Naval men under water. The men were in the 20 to 40 year age group and the data were corrected by determination of the residual air volume. The corresponding body indexes of the 99 subjects were determined by the N.Y.U. team from the relationship

$$C = HW^{-1/3}$$

where: C = the body build index

H = the body height in inches

W = the body weight in pounds

The relationship then between the body density and body build can be represented by the linear equation:

$$d = 0.6905 + 0.02970$$

To save computation time, Fig. 30 presents a nomogram for determination of C. By connecting the subject's height and weight values, there is obtained on the C scale the corresponding body index value. When these are substituted in the density formula, it is possible to determine the subject's approximate body density.

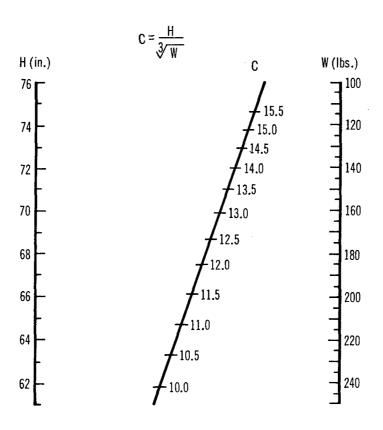


Figure 30. MONOGRAM FOR BODY INDEX (C) DETERMINATION

Table 13 presents the body densities of the test sample of the N.Y.U. study as determined by both the N.Y.U. equation and the Dupertuis equation. The Dupertuis (Ref. 30) equation developed in 1950 expresses body density as a function of Sheldon's (Ref. 31) somatotyping system:

$$d = 1.094 - 0.0119x$$

where x = rate of the first component in Sheldon's somatotyping system.

From the density data and the known body weight, it is possible to determine the volume of the total body. The results also are presented in Table 13. The mean value found by Drillis and Contini (Ref. 14) does not differ significantly from the mean value determined with the Dupertuis Formula but the values of particular subjects do. The maximum difference is 1.73 liters, the minimum 0 liters, the average difference is 0.878 liters or 1.27 percent.

The determination of the whole body density from the known weight and estimated body volume has been suggested by several investigators. The body volume estimation was used by Harless (Ref. 13) a hundred years ago. Formulas based on certain body lengths and circumferences have been developed by Weinbach, et al. (Ref. 32), Bashkirew (Ref. 33), and Skerlj (Ref. 34). However, they are tedious to use and their accuracies are no greater than the Drillis and Contini (Ref. 14) method.

3.1.3.3 Body Segment Parameters

Body segment parameters have been investigated by various investigators including Braune and Fischer (Refs. 18 and 19), Bernstein (Ref. 21), Dempster (Ref. 11), and Brillis and Contini (Ref. 14). Whenver possible, the mass and volume data of Drillis and Contini (Ref. 14) should be used as

Table 13
Total Body Density

Subject	Weight	Densi	ity	Volume in	Liters
•	(kg.)	Drillis and Contini	Dupertuis	Drillis and Contini	Dupertuis
1. M.B.	87.770	1.067	1.055	82.26	83.19
2. T.A.	85.050	1.049	1.049	81.08	81.08
3. K.B.	81.190	1.043	1.049	77.84	77.40
4. F.A.	74.840	1.096	1.085	68.28	68.98
5. R.C.	73.480	1.029	1.049	71.41	70.00
6. D.W.	72.570	1.064	1.055	68.20	68.79
7. H.G.	69.400	1.078	1.062	64.38	65.35
8. A.H.	69.170	1.066	1.055	64.89	65.56
9. A.M.	68.950	1.053	1.067	65.48	64.62
10. C.H.	68.720	1.078	1.062	63.75	64.71
11. R.B.	66.900	1.059	1.074	63.17	62.29
12. N.S.	63.050	1.112	1.079	56.70	58.43
Range	63.05	1.029	1.049	56.70	58.43
	87.77	1.112	1.085	82.26	83.19
Mean Value	73.42	1.066	1.062	69.02	69.20
Standard Deviation	7.572	.02475	0.01221	7.83	7.62

the physical characteristics of their subjects are compatible with those of modern day flying personnel (See Table 11). The other studies, while experimentally sound, were performed on cadavers with significantly smaller physical characteristics. In addition, there are questions as to the general applicability of the data due to time lapses, fluid loss, etc., and hence the data may not be entirely comparable to that obtained with living subjects.

There are also the factors of body build, percentile grouping, ethnic origin, and sex which influence the values of these parameters and hence affect their application to other populations. The determination of body segment parameters by Drillis and Contini (Ref. 14) was performed on the same sample used for the whole body parameter determination selected from the N.Y.U. student body and co-workers in the Biomechanics Group. Even so, the conclusions reached by Drillis and Contini (Ref. 14) were that there is no universal agreement on the planes of separation used between adjacent segments. Variations in the major biomechanical parameters will occur depending on the particular determination, for example, as to where the foot ends and shank begins. Even if such a unified and universally accepted subdivision of the human body into its segments could be achieved, it is unobtainable on the living subject.

Rody segment volume and mass for any subject depend upon build, occupational activity and his physical (health or pathological) condition. In most cases, some noticeable asymmetry exists between the left and right limbs; however, it is relatively small and practically speaking, it can be neglected. Drillis and Contini (Ref. 14) used a reaction change method to determine masses and mass centers of body segments. Segment volumes

were determined by a combination of immersion and segment zone techniques.

Their results of the segment volume determination are presented in Tables

14 through 16.

From Table 1^{l_4} , it is evident that for the upper extremity, the volume of the hand shows the greatest percent variability of the arm due to either muscle or bone formation differences (Ref. 1^{l_4} , p. 51).

In the lower extremity, the thigh shows the greatest variability, which is treat also for the foot. The shank has the least variability. The lower extremity as a whole shows a volume variability 2.5 times greater than the upper extremity. This indicates that the body build differences are more evident in the leg volume data.

To permit comparison of the segment volumes of subjects with different body build, it is customary to express the volume of the segment not in absolute values but as a percent of the total body volume. The data on this test sample are presented in Table 15.

For those subjects whose characteristics tend to be endotype (3 subjects) and those who tend to be ectotype (2 subjects), the segment mass volume data represented as a percentage of the total body volume are shown in Table 16.

The mean values of the body segment mass of the test sample of live subjects are given in Table 17. For comparison the data obtained by Dempster on cadavers are also presented. To enable a comparison of results obtained on different subjects or by various investigators, it is again customary to express the segment mass as a percentage of the total body mass. These

Table 14

Volume of Body Segments in Liters

Segment	Range	Mean	Standard Deviation	C.V. (in Percent)*
Hand	.328428	.384	.035	9.5
Forearm	1.055 - 1.296	1.175	.084	6.5
Upper Arm	2.094 - 3.047	2.412	.334	7.8
Whole Arm	3.512 - 4.583	3.971	.376	6.8
Foot	.670 - 1.105	.895	.175	19.6
Shank	2.263 - 3.272	2.818	.399	14.2
Thigh	4.750 - 8.456	6.378	1.464	22.9
Whole Leg	8.338 - 12.788	10.091	1.758	17.4

*C.V. is the Coefficient of Variability;

100 x Standard Deviation Mean

Table 15

Volume of Body Segments Expressed in Percent of the Whole Body

Segment	Range	Mean	Standard Deviation	C.V. in Percent
Hand	.4762	.566	.052	9.60
Forearm	1.47 - 1.72	1.702	.112	6.96
Upper Arm	2.98 - 3.53	3.495	.192	5.87
Whole Arm	4.93 - 5.79	5.73	.299	5.54
Foot	1.04 - 1.35	1.297	0.155	12.53
Shank	3.59 - 4.30	4.083	0.276	7.02
Thigh	6.92 - 10.77	9.241	1.486	16.79
Whole Leg	13.17 - 16.86	14.620	1.599	11.40

Table 16

Mean Body Segment Volume of Endotype and Ectotype Subjects in Percent of Body Volume

Segment	Endotypes $(n = 3)$	Ectotypes $(n = 2)$
Hand	0.517	0.623
Forearm	1.538	1.776
Upper Arm	3.426	3.120
Whole Arm	5.481	5.519
Foot	1.184	1.410
Shank	4.100	3.825
Thigh	8.949	6.925
Whole Leg	14.233	12.160

Table 17

Body Segment Masses (in kg.) (Mean Value of the Test Sample)

Investigators

Segments A	Dempster 8 Cadavers ge 52 - 83 Years	Drillis and Contini 12 Live Subjects Age 20 - 39 Years
Entire Body	59.790	73.420
Entire Upper Extremit	y 2.976	4.384
Upper Arm	1.575	2.619
Forearm and Hand	1.320	1.765
Forearm	.934	1.324
Hand	.385	.441
Entire Lower Extremit	y 9.611	11.023
Thigh	5.784	6.946
Shank and Foot	3.609	4.077
Shank	2.737	3.086
Foot	.853	.991

data are in Table 18, which presents the mean values of results obtained by each of the six investigators. To provide further reference information, Drillis and Contini (Ref. 14) presented the grand mean of all investigators; however, this is a straight average of the mean values of all investigators and it ignores the number of subjects each used, and, more important, the sample characteristics. These "mean" values are presented in Tables 19 and 20.

The coefficient method of establishing segment masses is based on the assumption that the ratio of segment mass to whole body mass as established using cadaver measurements can be transferred to live subject segment mass determination. From Table 18 it is evident that these ratios vary from one investigator to another. The ratios obtained by Harless (Ref. 13), Braune and Fischer (Ref. 18), and Dempster (Ref. 11) are based on cadaver measurements. The live subject factors are presented by Meeh (Ref. 17), Bernstein (Ref. 21) and Drillis and Contini (Ref. 14).

In the Drillis and Contini (Ref. 14) tests, the density determination was based on the segment volume determined by combining the immersion and segment zone methods and the mass determined by the reaction change method. Repeated volume determinations showed some variation caused by flow of blood and breathing.

The results of segment density determinations by Harless (Ref. 13),

Dempster (Ref. 11), and Drillis and Contini (Ref. 14) are shown in Table

21. Harless has found that:

1. The segment density increases in direction from proximal to distal parts, and

Table 18

	Body Segment Weights as Percent of Total Weight (Mean Values)	ts as Percent of (Mean Values)	Total Weigh	t)			
Investigator		Ř.	Body Segment				
	Head, Neck and Trunk	Upper Arms	Lower Arms	Hands	Upper Legs	Lower Legs	Feet
Harless	53.42	6.48	3.62	1.68	22.36	8.78	3.66
Meeh	59.08	6.19	3.38	1.46	17.36	9.35	3.18
Braune and Fisher	89.64	6.72	95.4	1.68	23.16	10.54	3.66
Bernstein	52.98	5.31	3.64	1,41	24.43	9.31	2.92
Dempster	56.50	5.30	3.10	1.20	19.30	9.00	2.80
Drillis and Contini	58.04	7.14	3.60	1.20	18.92	8.40	2.70

Table 19

Average Segment Masses in Percent of the Total Body Mass (Based on the Mean Value Data of Six Investigators)

Mass In Percent of the Total Body Mass	c,*
55.4	
44.6	
11.3	
6.2	0.062
3.6	0.036
1.5	0.015
33.3	
20.9	0.209
9.2	0.092
3.2	0.032
	of the Total Body Mass 55.4 44.6 11.3 6.2 3.6 1.5

^{*}Ratio of Segment Mass to Whole Body Mass (coefficient).

Table 20

Average Segment Masses of Live Subjects in Percent of the Total Body Mass

(Compared with the Average of Six Investigators)

Investigator:	(R	rnstein ussian) 76 Females	N.Y.U. (U.S.A.) 12 Males	Average of Six Investigators
Segment				
Upper Arms	5.31	5.20	7.14	6.20
Forearms	3.64	3.64	3.60	3.60
Hands	1.41	1.10	1.20	1.50
Thighs	24.43	25.78	18.92	20.90
Shanks	9.31	9.68	8.40	9.20
Feet	2.92	2.58	2.70	3.20

Table 21

Density of Body Segments (in kg/ltr)

Investigator:	Harless	Dempster	Drillis & Contin	i
Segment				Average
Hand	1.113	1.170	1.148	1.144
Forearm	1.109	1.130	1.127	1.122
Upper Arm	1.088	1.070	1.086	1.081
Foot	1.089	1.090	1.107	1.100
Chank	1.100	1.090	1.095	1.095
"high	1.069	1.050	1.089	1.069
Head and Neck	1.111	1.110		1.111
Trunk		1.030		1.030

Adapted from Drillis and Contini (Ref. 14)

2. there are density differences between the right and left side segments.

On the basis of the N.Y.U. segment density measurements, a third conclusion may be added that the segment density increases with the whole body density.

The segment density change with the body density increase is shown in Figs. 31 and 32. For the upper extremity more measurements were taken and as a result the curves approach more closely the actual densities. For the lower extremity fewer measurements were available and the curves shown are only approximations. Since the techniques for segment density determination of live subjects are in the early stages of development and the total number of measurements is not sufficient for any final statements, the use of the above density data is recommended for approximate segment mass calculations.

For correct determination of segment mass, density and volume of a specific individual direct measurements are a necessity.

The location of the segment mass centers is presented in Tables 22 through 25. Table 24 lists the data of 7 reports; however, the first two reports (Siedell and Guadagnolis (Ref. 55) and Gansler) appear to be reiterations and modifications of Dempster's (Ref. 11) work and hence are omitted from the average values. The last column in Table 24 shows the average value of the last five investigators independent of the number of subjects examined by each investigator.

3.1.3.4 Mass Moments of Inertia

Segment mass moments of inertia can be determined in several ways. A rough estimate can be obtained by the method described by Weinbach (Ref. 32) in

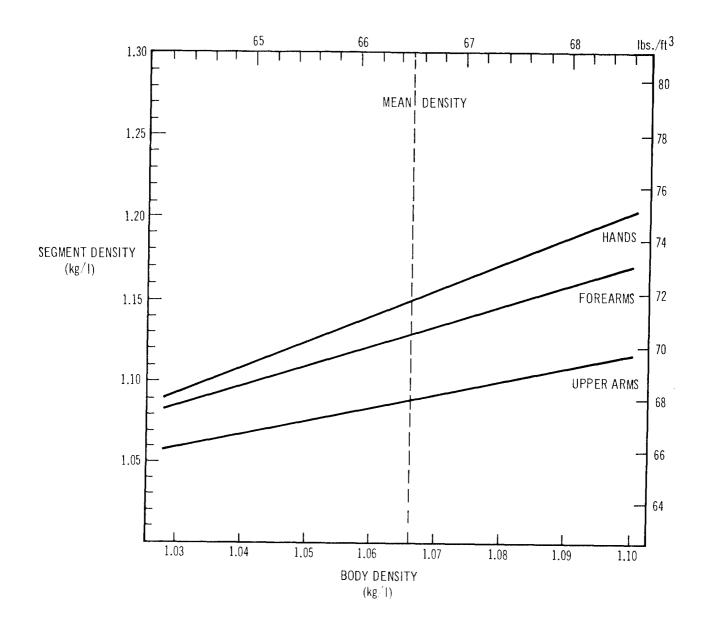


Figure 31. UPPER SEGMENT DENSITY AS A FUNCTION OF TOTAL BODY DENSITY

From Drillis and Contini (Ref. 14)

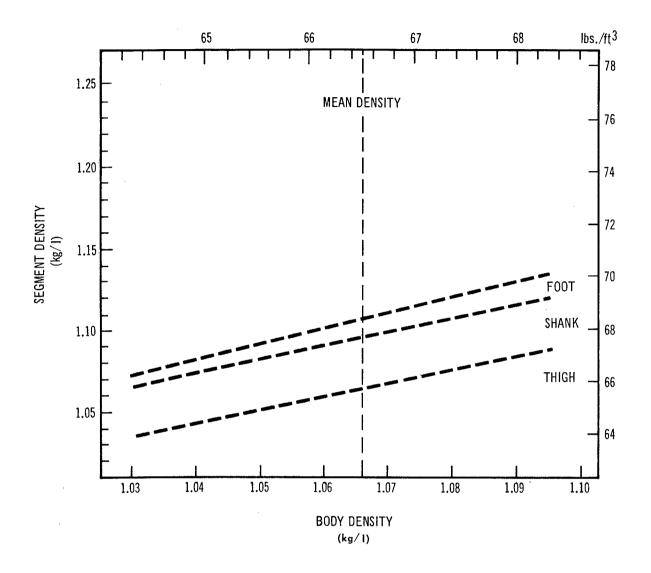


Figure 32. LOWER SEGMENT DENSITY AS A FUNCTION OF TOTAL BODY DENSITY From Drillis and Contini (Ref. 14)

Table 22.

Location of Segment Mass Centers from Proximal Joints (in meters)

(Mean values of the Drillis and Contini (Ref. 14) Test Samples)

Segments	Determine Immersion	d from Castings
Entire Upper Extremity	0.253	0.250
Upper Arm	0.119	0.113
Forearm and Hand	0.177	0.167
Forearm	0.115	0.110
Hand	*** *** ***	0.070
Entire Lower Extremity	0.298	0.319
Thigh	0.146	0.148
Shank and Foot	0.237	0.230
Shank	0.166	0.167
Foot (from heel)		0.118

Table 23

Relative Distances Between Center of Gravity and Joint
Axes or Other Handmarks

	Segment or Part and Reference Landmarks	No. Observed	Distance from Center of Gravity Reference Dimension Stated as %
1.	<pre>Hand (position of rest) wrist axis to knuckle III</pre>	16	50.6% to wrist axis 49.4% to knuckle III
2.	Forearm, elbow axis to axis	16	43.0% to elbow axis $57.0%$ to wrist axis
3.	Upper arm, gleno-humeral axis to elbow axis	16	43.6% to gleno-humeral axis 56.4% to elbow axis
4.	Forearm plus hand, elbow axis to ulnar styloid	16	67.7% to elbow axis 32.3% to ulnar styloid
5.	Whole upper limb, gleno- humeral axis to ulnar styloid	16	51.2% to gleno-humeral axis 48.8% to ulnar styloid
6.	Shoulder mass, sternal end of clavicle to gleno-humeral axis	14	84.0% of clavicular link dimension to sternal end of clavicle (oblique) 71.2% of clavicular link dimension to gleno-humeral axis (oblique)
7.	Foot, heel to toe II	16	*24.9% of foot link dimension to ankle axis (oblique) *43.8% of foot link dimension to heel (oblique) *59.4% of foot link dimension to toe II (oblique)
8.**	Lower Leg, knee axis to ankle axis	16	43.3% to knee axis 56.7% to ankle axis
9 .	Thigh, hip axis to knee axis	16	43.3% to hip axis 56.7% to knee axis
LO.**	Leg plus foot, knee axis to medial malleolus	16	43.4% to knee axis 56.6% to medial malleolus
11.	Whole lower limb, hip axis to medial malleolus	16	43.4% to hip axis 56.6% to medial malleolus

^{*}Alternately, a ratio of 42.9 to 57.1 along the heel to toe distance establishes a point above which the center of gravity lies; the latter lies on a line between ankle axis and ball of foot.

From Dempster (Ref. 11)

^{**}Questioned, sources verified but inspection indicates the same values for all are unlikely.

Table 23 (Continued)

	Segment or Part and Reference Landmarks	No. Obs erve d	Distance from Center of Gravity Reference Dimension Stated as %		
12.	Head and trunk minus limbs, vertex to transverse line through hip axes	7	60.4% to vertex 39.6% to hip axes		
13.	Head and trunk minus limb and shoulders, vertex to line through hip axes	7	64.3% to vertex 35.7% to hip axes		
14.	Head and neck, vertex to seventh cervical centrum	6	43.3% to vertex 56.7% to centrum		
15.	Thorax, first thoracic to twelfth thoracic centrum	6	62.7% to first thoracic centrum 37.3% to twelfth thoracic centrum		
16.	Abdomino-pelvic mass, centrum first lumbar to hip axes	5	59.9% to centrum first lumbar 40.1% to hip axes		

Table 24

Location of Mass Centers from Proximal
Joints in Percent of Segment Length

		Siedell Stiles	Sangle Control of the	To the state of th	(£) 200 (£)	(87) 84 84 84 84 84 84 84 84 84 84 84 84 84	200 Sept. (22)	The Island	(A)	Are Pala Continu
A	Head and Neck	51.6								
В	Trunk	42.0								A A
А, В	Trunk, Head and Neck		60.4							B B
C, D	Entire Arm							43.1	43.1	
С	Upper Arm	43.6	43.6	48.5	47.0	46. 6	43.6	孙.9	46.1	
D	Forearm Arm	43.0	43.0	祌.0	42.0	µ1.2	43.0	42.3	42.5	F
E	Hand	57.0	50.7	47.4					43.3	E
D, E	Forearm and Hand			45.8			67.7*	38.2	42.0	l AA
F	Thigh	3 8.5	43.3	46.7	44.0	38.6	43.3	中.0	42.7	(1\) \- 9
G	Shank	43.3	43.3	3 6.0	42.0	µ1.3	43.3	39.3	40.4	\Y\¾
Н	Foot (from Heel)	58.1		46. 0	43.4		43.3	44.5	14.3	
F, G	Entire Leg				41.5		43.4	39.7	41.5	au .
G, H	Shank and				51.9		43.3	45.0	46.7	

*Distance from elbow to ulnar styloid is assumed to be 100 percent.

Table 25

Distance of Forearm Mass Center from the Proximal Joint. Forearm Length = 1.000

Age	76 M	ales	76 Females		
	Mean M	Range $+\sigma$	Mean M	Range $\pm \sigma$	
12-15	0.383	0.359 - 0.407	0.415	0.392 - 0.1411	
16 -2 5	0.419	0.388 - 0.450	0.417	0.383 - 0.451	
26-3 5	0.409	0.383 - 0.435	0.425	0.388 - 0.462	
36-45	0.1403	0.384 - 0.422	0.405	0.370 - 0.440	
46-75	0.428	0.402 - 0.454	0.411	0.381 - 0.441	

Data of Bernstein (Ref. 21) from Drillis and Contini (Ref. 14)

which the coefficients developed by Braune and Fischer (Ref. 18) are used. An approximate estimate of the mass moment of inertia may also be made by determining the segment's volume and using the mean value of the density of the young adult male body. For more accurate determination of the mass moment of inertia of body segments, the compound pendulum method using castings of the appropriate segment under study is recommended as the best (Ref. 14).

The results of tests conducted by Drillis and Contini (Ref. 14) are shown in Table 26 along with similar data obtained by Dempster (Ref. 11). It should be noted that all of the methods discussed assume that the center of mass and the center of volume are coincident. The effect of this assumption is unknown.

By knowing the segment length, segment mass, location of mass center, and segment radius of gyration, it is possible to determine the segment's mass moment of inertia. To obtain the radius of gyration, Braune and Fischer (Ref. 18) suggested the use of a coefficient (C_3). They found that the radius of gyration for rotation about the axis through the mass center and perpendicular to the longitudinal axis of the segment can be established by multiplying the segment's length (ℓ) by the coefficient C_3 (to which they assigned a value 0.3). Hence the mass moment of inertia (I_{C_3}) with respect to the mass center would be:

$$I_{cg} = me^2 = m (0.3.1)^2 = 0.09 ml^2$$

= $m(0.3e)^2 = 0.09 ml^2$

For the rotation of the segment about its longitudinal axis, Fischer established a coefficient $C_{ij} = 0.35$, so that the radius of gyration

Table 26

Mass Moments of Inertia about the Center of Mass (I_{cg}) of Body Segments

(Mean Values of the Test Samples in gm.n²)

Segment	Dempster	Drillis and Contini
Entire Upper Extremith	1.05 × 10 ⁶	1.33 × 10 ⁶
Upper Arm	0.139 x 10 ⁶	0.138 x 10 ⁶
Forearm and Hand	0.187 x 10 ⁶	0.247×10^6
Forearm	0.055 x 10 ⁶	0.073 × 10 ⁶
Hand	0.0045 x 10 ⁶	0.0059 x 10 ⁶
Entire Lower Extremity	6.97 x 10 ⁶	7.49 x 10 ⁶
Thigh	1.08×10^6	0.895 × 10 ⁶
Shank and Foot	1.04 x 10 ⁶	1.120 x 10 ⁶
Shank	0.416 x 10 ⁶	0.495 x 10 ⁶
Foot	0.031 x 10 ⁶	0.020 x 10 ⁶

e = 0.35 D, where D is the diameter of the segment. The approximate
values of the segment length expressed as ratios of body height are
shown in Fig. 33, as reported by Drillis and Contini (Ref. 14). These
values or those values given in Table 2 for BOEMAN-I may be used for
approximations for determining the necessary parameters.

Since for a living subject the segment rotates about the proximal or distal joint, and not the mass center, the mass moment of inertia about the joint is greater than I by the term me², where e is the distance of mass center from the joint. It follows that the mass moment of inertia for segment rotation about the joint is equal to

$$I_1 = me^2 + me^2 = m(e^2 + e^2)$$

The data obtained experimentally tend not to be in agreement with values obtained by Fischer. The coefficient $C_3 = 0.3$ is generally too high. The apparent error in Fischer's (Ref. 20) value is probably due to the methods used in his second series of tests on which the value is based. In this series of tests two pivots were used at the opposite ends of the segment. This altered the mass configuration of the segment. Furthermore, the added pivot, which in any test would be at a maximum distance from the actual point of rotation (in a pendulum test) would obviously tend to increase the moment of inertia of the combination, and perhaps even have a major influence (Ref. 14). That this probably is a correct inference is shown in Table 28 in which the results of the first series of tests by Braune and Fischer (Ref. 18) vary from the second, and are in keeping with the results obtained by Drillis and Contini (Ref. 14). It is assumed that the Drillis and Contini (Ref. 14) tests based on

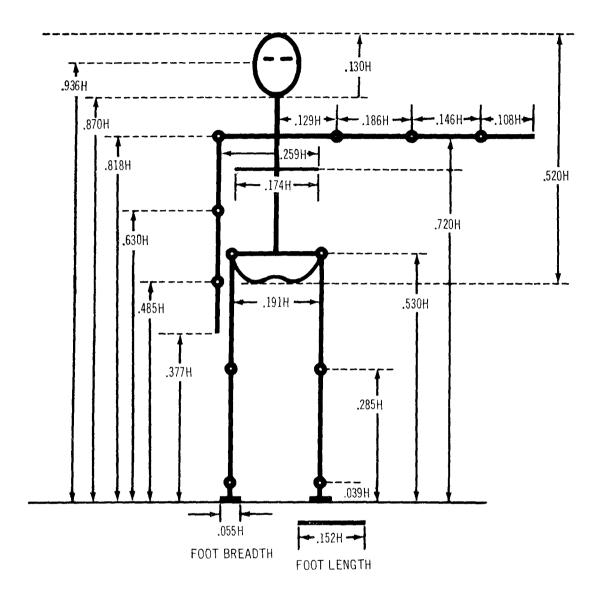


Figure 33. SEGMENT LENGTH EXPRESSED AS A FUNCTION OF BODY HEIGHT

eight subjects provide better coefficients for the different segments.

3.1.3.5 Sample Computation from Drillis and Contini (Ref. 14)

Assume it is desired to determine the mass, center of mass and mass moment of inertia of the upper arm and forearm and hand (in combination) for a male in this age category.

The following data are required:

- (1) The height of the subject
- (2) The weight of the subject

The following data are desirable, if obtainable:

(1) Length of the upper arm, and the forearm and hand.

(Measure as indicated in Ref. 1).

The following graphs, equations, and tables are used:

- (1) Nomogram, Fig. 30 (Body index C)
- (2) Graph, Fig. 34 (Whole body density)
- (3) Graph, Fig. 31 (Upper extremity density determination)
- (4) Table 15 (Volume of the body segments)
- (5) Fig. 33 (Segment length, mean)
- (6) Table 24 (Location of mass center)
- (7) Table 27 (Ratio C₃, radius of gyration)

Procedure

For a subject who weighs 172 pounds and measures 5 feet 11 inches (71 inches) in height, the computations are as follows:

Segment		Braune 1 Cadaver Test I		cher Sadaver est II	Drillis and Contini 8 Live Subjects	Weighted Average
	R	L	R	L		
Entire Upper Extremity			0.30	0.31	0.24	0.252
Upper Arm	0.27	0.27	0.29	0.31	0.26	0.268
Forearm and Hand	0.26	0.28	0.29	0.32	0.25	0.263
Entire Lower Extremity			0.32	0.32	0.24	0.256
Thigh	0.26	0.27	0.31	0.31	0.23	0.250
Shank and Foot	0.32	0.32	0.33	0.35	0.29	0.303
Shank	0.25	0,26	0.24	0.26	0.27	0.264
Average	0.27	0.28	0.30	0.31	0.25	0.265

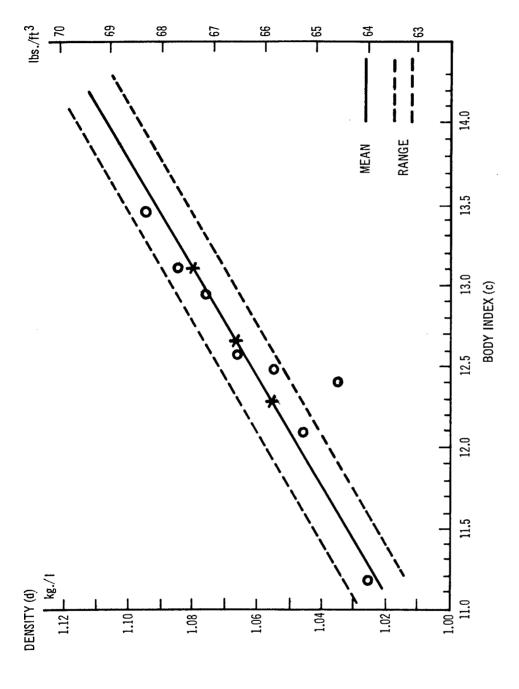


Figure 34. Body density as a function of Body index (c)

From Drillis and Contini (Ref. 14)

(1) On nomogram, Fig. 30, join the weight in pounds (172) by a line to height in inches (71) and at the intercept with the line for C, obtain a value for C.

C = 12.9 approximately

(2) On Graph, Fig. 34, locate C = 12.9, proceed vertically upward to intersect solid black line, then proceed horizontally to determine value of the whole body density.

 $d = 7.2 \text{ lbs/ft}^3$

(3) On Graph, Fig. 31, proceed as in (2). From d = 67.2 vertically upward to intersect lines of segment densities.

d, upper arm = 68.2 lbs/ft^3

d, forearm = 71.2 lbs/ft^3

d, hand = 72.5 lbs/ft^3

(4) Given the weight 172 pounds, whole body density of 67.2 pounds per cubic foot, we can now obtain the whole body volume by dividing the weight by the density:

 $172/67.2 = 2.56 \text{ ft}^3 \text{ whole body volume}$

(5) Table 15 gives the values of the volume of body segments expressed as percentages of the whole body volume:

v, upper arm = $3.495 \times 10^{-2} \times 2.56 = 0.0895 \text{ ft}^3$

v, forearm = 1.70 $\times 10^{-2} \times 2.56 = 0.0435 \text{ ft}^3$

v, hand = $0.566 \times 10^{-2} \times 2.56 = 0.0145 \text{ ft}^3$

(6) Multiplying the volumes of the segments by their respective densities, the masses (or weights) of the segments are obtained.

m (w) upper arm =
$$0.0895 \text{ ft}^3 \times 68.2 \text{ lbs/ft}^3 = 6.10 \text{ lbs}$$

m (w) forearm =
$$0.0435 \text{ ft}^3 \times 71.2 \text{ lbs/ft}^3 = 3.09 \text{ lbs}$$

m (w) hand =
$$0.0145 \text{ ft}^3 \times 72.5 \text{ lbs/ft}^3 = 1.05 \text{ lbs}$$

(7) To obtain the approximate lengths of the body segments when they have not been measured, Fig. 33 may be used. From this figure, the mean lengths, expressed in terms of the body height are:

$$e$$
 upper arm (.818 - .630) = .188 H

$$g \text{ forearm} \quad (.630 - .485) = .145 \text{ H}$$

$$e \text{ hand}$$
 (.485 - .377) = .108 H

and since H = 71 inches

$$u = .188 \times 71 = 13.35$$
 inches

$$f = .145 \times 71 = 10.30$$
 inches

$$h = .108 \times 71 = 7.68$$
 inches

(8) Having obtained the lengths of the segments, the locations of the center of mass (e) can now be determined by using values given in Table 25.

e upper arm = .461 x 13.35 inches =
$$6.15$$
 in

e forearm and hand = .420
$$(10.30 + 7.68) = 7.55$$
 in

(9) Having the segment lengths, the radius of gyration (ρ) can be determined using values given in Table 27.

$$\rho$$
 upper arm = 0.268 x 13.35 inches - 3.58 inches

$$\rho$$
 forearm and hand = 0.263 x (10.30 + 7.68) = 4.73 in.

(10) Since the moment of inertia of any segment about its proximal axis of rotation is expressed by the equation:

$$I_1 = m (\rho^2 + e^2),$$

we can substitute the values obtained in steps 6, 8, and 9

in the equation. Then,

I, (upper arm about the shoulder joint) =

(6.10 lbs) x
$$\left(\frac{2}{3.58} + \frac{2}{6.15}\right)$$
 inches² = 308 lb.in.²

I, (lower arm and hand about the elbow) =

$$(3.09 + 1.05)$$
lbs. $\left(\frac{2}{4.73} + \frac{2}{7.55}\right)$ inches² = 328 lb.in.²

To facilitate computations, Fig. 35 provides a graphic solution for body density (d) based on height and weight. Fig. 36 provides conversion from metric to British systems of measurement, and Figs. 37, 38, and 39 are for determining moments of inertia.

3.1.4 Joint Parameters

3.1.4.1 Joint Characteristics

Joints are formed wherever two or more bones are in juxtaposition. Immovable fibrous joints, like those between the bones of the skull are not interest here. The bones of the movable joints are bound together and sometimes encapsulated by ligaments which are tough, fibrous bands. The types of joints in the limbs include ball and socket in shoulder and hip, hinge for elbow and knee bending, pivot for elbow rotation (hand pronation and supination), and gliding (in part) for the wrist. Spinal joints important to BOEMAN include pivot and gliding for head turning. Joints which secure the shoulder to the sternum are of the gliding type.

The human body is, in the foregoing terminology, an open chain system of links rotating around joint centers. The end members of these open chain links, the hands and feet, can occupy a wide variety of positions in space

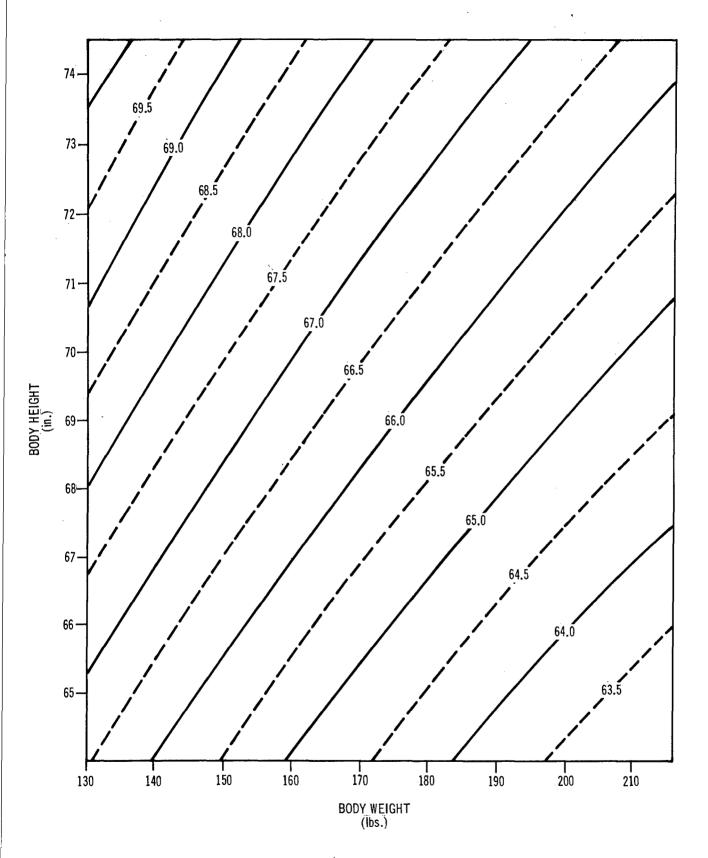


Figure 35. BODY DENSITY AS A FUNCTION OF BODY HEIGHT AND WEIGHT

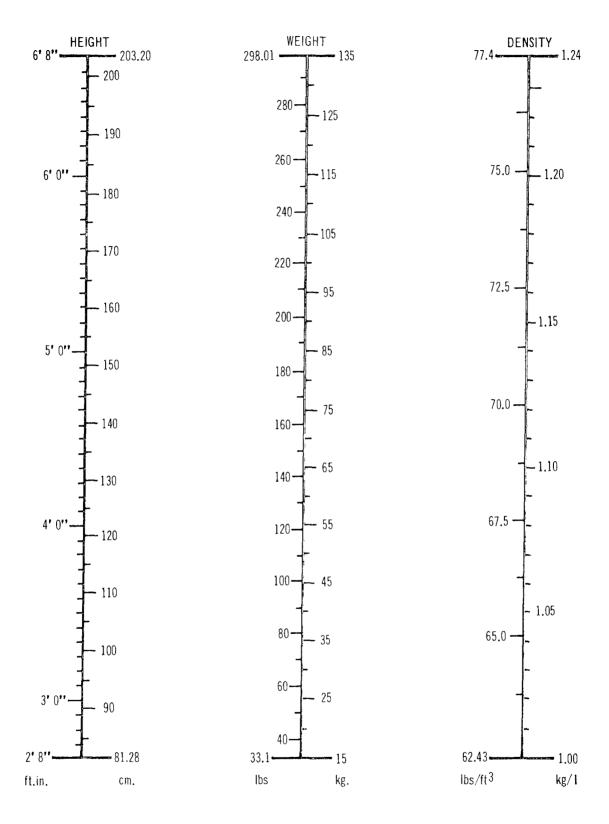


Figure 36. HEIGHT, WEIGHT, DENSITY CONVERSION SCALES

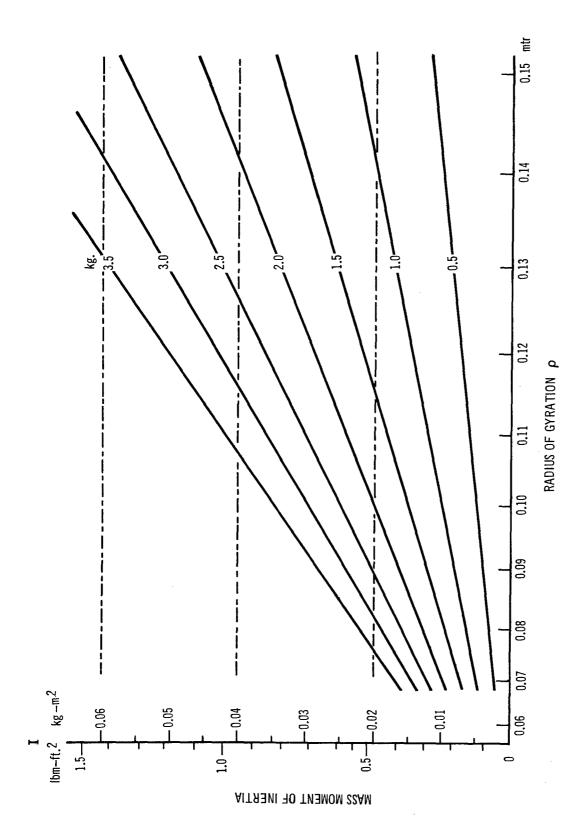


Figure 37. MASS MOMENT OF INERTIA AS A FUNCTION OF SEGMENT WEIGHT AND RADIUS OF GYRATION (LOW RANGE).

From Drillis and Contini (Ref. 14)

MASS MOMENT OF INERTIA AS A FUNCTION OF SEGMENT WEIGHT AND THE RADIUS OF GYRATION (MEDIUM RANGE) Figure 38.

From Drillis and Contini (Ref. 14)

MASS MOMENT OF INERTIA

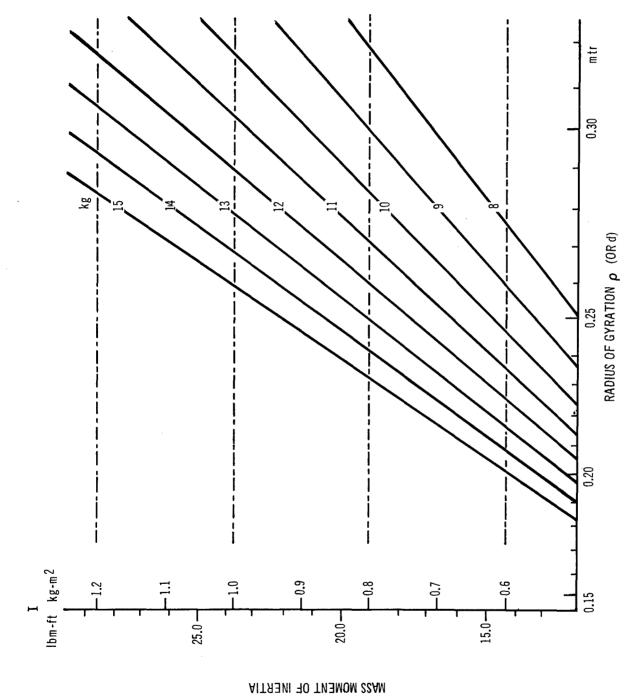


Figure 39. MASS MOMENT OF INERTIA AS A FUNCTION OF SEGMENT WEIGHT AND THE RADIUS OF GYRATION (HIGH RANGE)

From Drillis and Contini (Ref. 14)

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as a result of the cumulative ranges of the intervening joints (Dempster, Ref. 11).

3.1.4.2 Joint Angular Limits

The range of joint motion is determined by the bony configuration, constraints imposed by elastic limits of the attached muscles, tendons and ligaments, and the impedance of surrounding tissue, all of which vary somewhat from person to person and joint to joint. Also of importance is the difference between the angular range achieved by voluntary effort and that produced by other forces. Examples of forced limits are: augmented knee flexion when "sitting on one's heels" or twisting one's forearm when the hand is gripping a fixed handle. Factors which are believed to influence the range of joint movement are discussed below.

AGE: Joint mobility decreases only slightly between age 20 and age 60, barring injury, arthritis or other disease. Between the 1st and 7th decades, joint mobility declines about 10 percent, but no significant differences between youth and normal middle age have been found (Ref. 25).

SEX: Women exceed men in the range of movement at all joints but the knee. Differences vary from minor increases to as much as 14 degrees at the wrist (Ref. 25).

RACE: There may be racial differences in joint mobility, but no data are currently available (Ref. 25).

BODY BUILD: Slender men and women have the widest range of joint movements, fat ones the smallest. Average and muscular body builds, in that descending order, are intermediate. These differences

may reach practical significance, especially those between the thin and the fat groups, where variations of more than 10 degrees in a given movement are not uncommon (Ref. 25), although it should be noted that Laubach and McConville (Ref. 53) reported that: "There is a general lack of relationship between flexibility and somatotype components."

EXERCISE: Any joint of the body tends to become restricted in movement if it is not used regularly within the limits of its normal range. Physical exercise may increase the range of motion of a joint. However, excessive exercise can result in the so-called "muscle-bound" condition, which increases bulk and limits joint excursion (Ref. 25).

OCCUPATION: Some specialized tasks involve the repetition of certain body movements. As a result, the range of movement at the affected joints will tend to increase (Ref. 25).

FATIGUE: Severe fatigue will restrict the effective range of joint motion by decreasing not only motivation but muscle strength as well (Ref. 25).

DISEASE: Arthritis, poliomyelitis, and other diseases or injuries affecting the joints, muscles, or nervous system can severely restrict body movements or completely immobilize a joint.

MOTIVATION: Motivation influences the limits of joint motion by determining the effort exerted to attain the maximum amount of movement (Ref. 25).

RIGHT VERSUS LEFT SIDE: There is normally so little variation that the two sides can be considered identical. In arm rotation, for example, group differences between left and right ranged from 0 to 5 degrees (Ref. 25).

BODY POSITION: The range of movement of one part of the body is affected by the position or movement of neighboring parts; thus, hand rotation can be considerably increased if shoulder movements are added to those at the elbow. Wrist flexion is greater with the hand pronated than supinated. In addition, the range of movements in a prone position is not the same as in an erect position.

cLOTHING AND PERSONAL EQUIPMENT: Light clothing has little effect on joint movement, but bulky clothing such as cold-weather or flying gear considerably reduces the range of motion. The Army arctic uniform markedly restricts movements at the neck, shoulder, arm, and waist: crotch-shoulder flexion, for example, is reduced by over 20 degrees (Ref. 25). Joint motion values presented below are for nude or lightly clothed subjects.

Table 28 presents a summary of angular limits to be used for the baseline man-model (BOFMAN-I). Where data were not available, estimations were made (e.g., clavicle). The subsequent tables present more detail on individual movements as reported by various investigators.

Figures 40 and 41 illustrate the terminology and the null reference locations for each of the measurements. The types of body movement are:

FLEXION: Bending, or decreasing the angle of the joint.

EXTENSION: Straightening, or increasing the angle of the joint.

HYPEREXTENSION: The continuation of extension beyond the starting position.

ADDUCTION: Moving toward the midline of the body.

ABDUCTION: Moving away from the midline of the body.

MEDIAL ROTATION: Turning toward the midline of the body.

LATERAL ROTATION: Turning away from the midline of the body.

PRONATION: Rotating the forearm so that the palm faces downward.

SUPINATION: Rotating the forearm so that the palm faces upward.

FVERSION: Turning outward.

INVERSION: Turning inward.

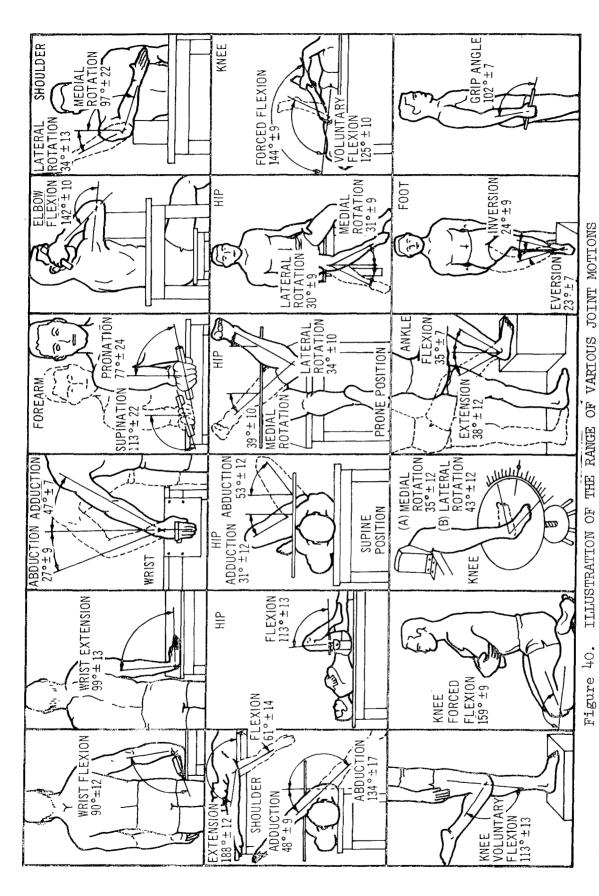
Table 28

Joint Movement Limits (Degrees)

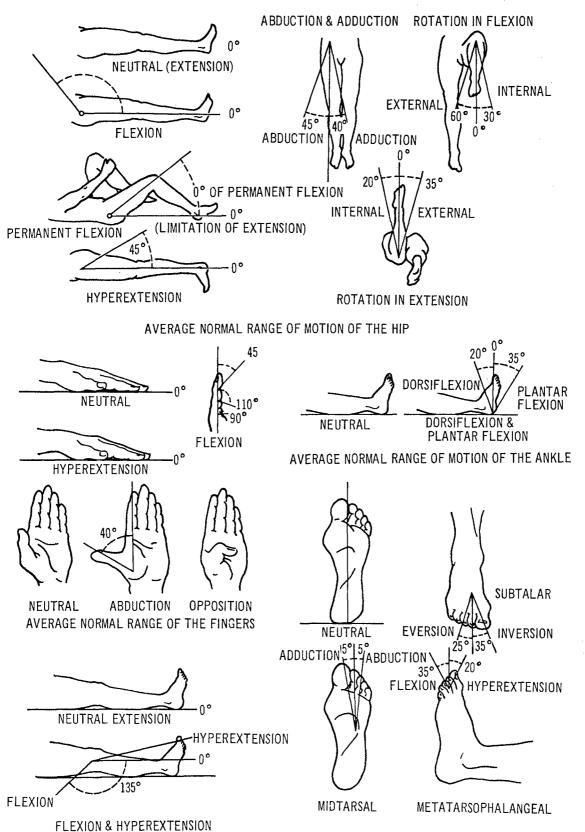
		Mean	S.D.	+2 S.D.	<u>-2 S.D.</u>
1.	Wrist, forced flexion (palmar flexion)	90	12	114	66
2.	Wrist, forced extension (dorsiflexion)	99	13	125	73
3.	Wrist, abduction (ulnar flexion)	47	7	61	33
4.	Wrist, adduction (radial flexion)	27	9	45	9
5.	Wrist, total flexion - extension angle	189	21	231	147
6.	Forearm, supination	113	22	157	69
7.	Forearm, pronation	77	5#	125	29
8.	Forearm, total supination - pronation angle	190	30	250	130
9.	Elbow flexion	142	10	162	122
10.	Shoulder, extension	61	14	89	33
11.	Shoulder, flexion	188	12	212	164
12.	Shoulder, total flexion - extension angle	249	19	287	211
13.	Shoulder, adduction	48	9	66	3 0
14.	Shoulder, abduction	134	17	168	100
15.	Shoulder, total adduction - abduction angle	182	20	222	142
16.	Shoulder, medial rotation	97	22	141	53
17.	Shoulder, lateral rotation	34	13	60	8
18.	Shoulder, total medial - lateral rotation angle	131	24	179	83
19.	Hip, flexion	113	13	139	87
20.	Hip, adduction	31	12	55	7
21.	Hip, abduction	53	12	77	29
2 2.	Hip, total adduction - abduction angle	84	14	112	56
23.	Hip, medial rotation, prone	39	10	59	19
24.	Hip, lateral rotation, prone	34	10	54	14
25.	Hip, total medial-lateral rotation, prone	73	16	105	41
26.	Hip, medial rotation, sitting	31	9	49	13
27.	Hip, lateral rotation, sitting	30	9	48	12
28.	Hip, total medial-lateral rotation, sitting	61	14	89	33
29.	Knee, voluntary flexion, prone	125	10	145	105
30.	Knee, forced flexion, prone	144	9	162	126

Table 28 (Contd). Joint Movement Limits (Degrees)

	·	Mean	S.D.	+2 S.D.	_2 S.D.
31.	Knee, voluntary flexion, standing	113	13	139	87
32.	Knee, forced flexion, kneeling	15 9	9	177	141
33.	Knee, medial rotation	35	12	59	11
34.	Knee, lateral rotation	43	12	67	19
35.	Knee, total medial-lateral rotation angle	78	16	110	46
36.	Ankle, flexion	35	7	49	21
37.	Ankle, extension	38	12	62	14
38.	Ankle, total flexion-extension angle	73	14	101	45
39.	Foot, inversion	24	9	42	. 6
40.	Foot, eversion	23	7	37	9
41.	Foot, total inversion-eversion angle	47	13	73	21
42.	Grip angle	102	7	116	88
43.	Neck, ventral flexion	67	9	8 5	49
44.	Neck, dorsal flexion	77	10	97	57
45.	Neck, right or left flexion	41	7	55	27
46.	Neck, rotation - right	73	5	83	63
47.	Neck, rotation - left	74	-14	82	66
48.	Lumbar Joint				
	Ventral and dorsal flexion Right and/or left lateral flexion	10 0			
49.	Thoracic Joint				
	Ventral flexion Dorsal flexion Right or left lateral flexion Rotation (about thoracic link) CW or CCW	60 20 40			
50	Eye Deflection (fixational angle)	35			
<i>7</i> 0.	Lateral movement (in transverse plane)				
	Temporal	74			
	Nasal	55			
	Up and down in sagittal plane)				
	Up Down	48 66			
51.	* Clavicle				
	Elevation	10			
	Depression	10			
	Abduction Adduction	10 10			



Ranges of joint motion in 39 young men, showing **the** median value in degrees, + 1 standard deviation. If + 2 SD are taken, 95% of the sample of 39 is included. Compared with the 1950 Air Force survey 6.0 lbs heavier, and 1.4 inches taller). Adapted from analysis by Barter et al. (56) of data from Dempster (11) of over 4000 flying men, this sample is 6.8 years younger, Source:



AVERAGE NORMAL RANGE OF MOTION OF THE KNEE A

AVERAGE NORMAL RANGE OF MOTION OF THE FOOT

Figure 41. RANGES OF JOINT MOTION

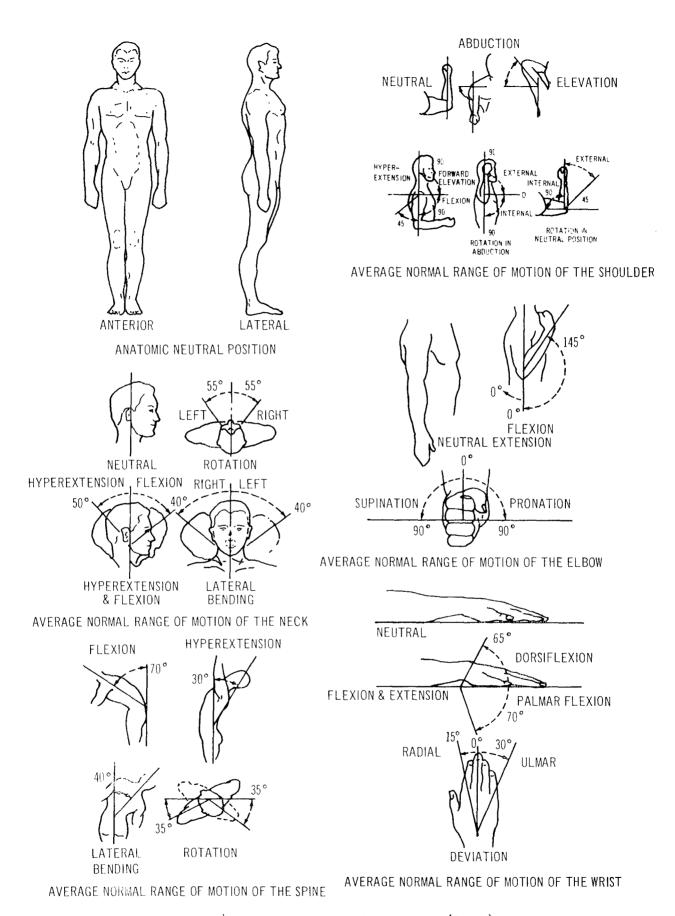


Figure 41. RANGES OF JOINT MOTION (Cont)

Table 29. Range of Movement at the Joints of the Arm and Hand^a

and the section of th		The second of th	Ra	nge of Movement (
Joint	Type of Movement	Mean	S.D.	5th Percentile ^c	95th Pe rc entile
Wrist	Flexiond	90	12	70	110
MITPO	Extension ^d	•		-	
	extensiond	<u>99</u>	13	78	120
	Total ^d	189	21	15h	224
	Adductiond	27	9	12	42
	Abduction ^d	47	7	3 5	59
	Total ^d	74	13	53	95
Forearm	Supination e	113	22	7 7	149
	Pronation ^e	_77	21;	3 8	116
	Total ^e	190	30	IJp	239
Elbow	Flexion	J] [†] 5	10	12 6	158
Shoulder	Flexion	188	12	168	20 8
	Extension	61	14	3 8	84
	Total	249	19	218	280
	Adduction	48	9	33	63
	Abduction	134	17	106	162
	Total	182	20	11,9	21.5
	Rotation: medial	97	22	61.	133
	Rotation: lateral	_34	13	13	55
	Total	131	24	92	170

a Barter, Emanuel and Truett (Ref. 56), 39 male subjects representing varied types of body build.

b See Figure 40.

Computed from the standard deviation.

These are "forced" movements in that the hand is physically restrained and the forearm then rotated about the wrist joint. Normal movements, in which the hand is rotated about the wrist, would have less excursion.

e Elbou at 90 degree angle.

Table 30. Range of Wrist Flexion and Extension While Grasping a Control

Subjects and Test Conditions:

79 male subjects, average age 28 years, representing varied body builds grasped a vertical handgrip located approximately 19 inches forward and 13-1/2 inches above the Seat Reference Point. Sixty-six subjects were used to determine the extreme limits. Flexion and extension of the right wrist were measured from the "neutral" or resting position of the handgrip selected as most comfortable by each subject. This position averaged 19 to the left of a midsagittal (fore-and-aft) plane.

	es-verlengings-garage directives cam		Range of Movement Percentile	Percentile ^a
Type of Movement	Mean	S.D.	5th	95th
Flexion - to left of neutral position				
Comfortable, usable limits	46.0	15.7	20	72
Extreme possible limits	91.0	16.6	64	118
Extension - to right of neutral position				
Comfortable, usable limits	33.6	13.7	11	56
Extreme possible limits	71.8	16.0	46	98
Total movement, extension - flexion				
Comfortable, upable limits	76.6	23.3	3 8	115
Extreme possible limits	164.2	22.6	127	201

Computed from standard deviation From Daniels and Hertzberg (Ref. 37)

Table 31. Range of Movement at the Joints of the Leg and Foot^a

(1721-17-17-17-17-17-17-17-17-17-17-17-17-17			ingan barana - alaman - ra	Range of Movement	
Joint	Type of Movementb	Mean	S.D.	5th Percentile ^c	95th Percentile ^c
Ankle	Flexion Extension	35 <u>38</u>	7 12	23 18	47 58
	Total	73	14	50	96
	Adduction (or inversion) Abduction (or	2կ	9	9	3 9
	eversion)	23	7	זב	3 5
	Total	47	13	26	68
Knee	Flexion (standing) Flexion (kneeling) Flexion (prone)	113 159 125	13 9 10	92 1111 109	134 174 141
	Rotation: Medial Rotation: Lateral	35 <u>43</u>	12 12	15 23	55 63
	Total	78	16	52	104
Hip	Flexion Adduction Abduction	113 31 53	13 12 12	92 11 33	134 51 73
	Total	84	14	61.	107
	Rotation: Medial (seated) Rotation: Lateral (seated)	31 <u>30</u>	9	16 15	4 6 145
	Total	61	11،	3 8	814
	Rotation: Medial (prone) Rotation: Lateral	3 9	10	23	55
	(prone)	34	10	18	50
derdoor various annual various	Total	73	16	47	99

^{*}Barter, Emanuel and Truett (Ref. 56), 1957: 39 male subjects representing varied types of body build.

b_{See Figure 40.}

^cComputed from standard deviation

Table 32. Range of Movement at the Neck

	Range of Move	ment (Degrees)
Type of Movement ^a	Mean	S.D.
Flexion (ventral)b	60	12
Flexion (ventral) ^c	67	9
Flexion (dorsal) ^b	61	27
Flexion (dorsal) ^c	77	10
Flexion (right or left) ^b	42	7
Rotation (right or left)b	79	114
Rotation (right) ^c	73	5
Rotation (left) ^c	74	4

^aSee Figure 41

^bGlanville and Kreezer (Ref. 38), 10 male subjects.

^cBuck et al., (Ref. 39), 100 subjects, 47 males, 53 females.

Table 33. Difference in Range of Joint Motion in Men and Women

Joint	Type of Movement	Mean Difference (Degrees)
Wrist	Flexion - extension	+3)4
	Adduction-abduction	+11
Elbow	Flexion-extension	+ 8
Sh o ulder	Abduction (rearward)	+ 2
lnk le	Flexion-extension	+ 4
nee	Flexion-extension	0
lip	Flexion	+ 3

^aSinelnikoff and Grigorowitsch (Ref. 40), 100 male and 100 female subjects.

b"Plus" (+) denotes greater range in women.

3.1.5 Visual Characteristics

The subject of vision has received a great deal of attention from researchers for a number of years and the literature is abundant with data. It is the task of this report to determine that data which are applicable and necessary for the computerized man-model without complicating the subject any more than necessary. Therefore, it was felt that a description of the field of vision in mathematical data terms which have considered the more important limitations and influences would be a practical approach.

The eye is a complex entity in itself; however, with regard to the computerized man-model, the retina, fovea, rods, and cones are most important. The retina is the immermost layer of the eyeball which is the receiving apparatus for a light stimulus. The fovea is a small pit at the center of the retina where photopic vision is best. The rods and cones are light sensitive neural receptors in the retina named for their general shape. The cones are concentrated in the region of the fovea and are highly sensitive to color and form. They function best at high levels of illumination and are relatively insensitive to low levels. The rods starting at the outer edges of the fovea increase in concentration through the region surrounding the fovea and completely predominate over the cones toward the extreme periphery of the retina. The rods are much more sensitive to light than cones and are relatively insensitive to form and color. Figures 42 and 43 help to illustrate these points.

The ability to observe and identify an object then depends in part on what part of the retina the image falls. In practical problems, therefore, it is

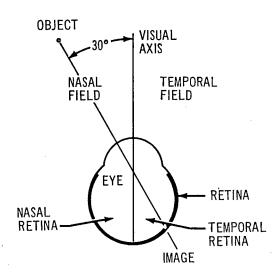
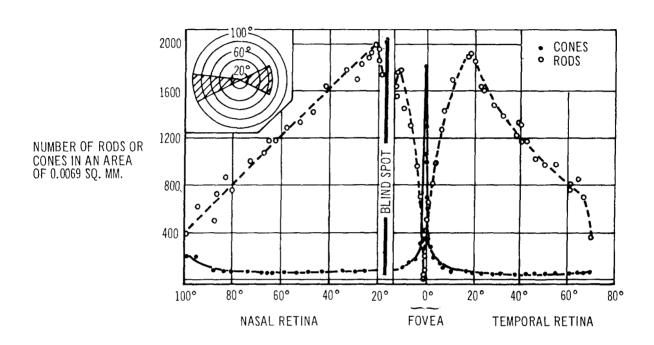


Figure 42. EYE IMAGES

Diagram Showing How Object on One Side of Visual Field Produces Image on the Other Side of the Retira (Right Eye is Shown).

From Wulfeck et al. (Ref. 41)



The density of cones and rods on or near the horizontal meridian through a human retina. The inset is a schematic map of the retina showing F, the fovia, and B, the blind spot. The striped area represents the regions of the retina which were sampled in obtaining the counts plotted here (from Ref. 42).

Figure 43. DISTRIBUTION OF THE RODS AND CONES IN THE HUMAN RETINA

From Wulfeck et al. (Ref. 41) data of Osterberg (Ref. 42)

essential to consider where the object will fall on the retina (see Fig. 42). It is true that vision is also a function of illumination, color, brightness contrast, size, visual angle, display time and others, but these factors are presently considered in cockpit designs and should not be critical to the computerized man-model. Some assumptions are necessary, however. For example, we have assumed that all things observed are black, gray or white, thereby eliminating the color restrictions as shown in Fig. 44.

The visual field is defined as the spatial area, in degrees, which can be seen by the fixated eye. The combined horizontal field extends through an arc of approximately 188 degrees and the monocular field is approximately 156 degrees. The binocular or overlapping field is approximately 124 degrees. The vertical field is 46 degrees up from the line of fixation and 67 degrees down (Ref. 41). Figures 45 and 46 help to illustrate these points.

Brightness contrast is a measure of how much target brightness (B_t) differs from the background brightness (B_b). The equation for obtaining brightness contrast is:

Percent contrast =
$$\frac{B_b - B_t}{B_b}$$
 x 100

Contrasts can vary from 100% to zero for targets darker than their back-grounds and from zero to infinity for targets brighter than their back-grounds. With less contrast, there is lower acuity. For example, it is harder to see black on gray than it is to see black on white.

COLOR ZONES: The color of a stimulus varies with its position in the visual field and with its intensity. Various color zones for the right eye are shown on the map as seen with indirect vision in different parts of the retina. Red and green colors have relatively small fields in the central region of the retina, while blue and yellow have the largest fields. Beyond these only gray can be seen. The crosshatched area indicates the area where nothing is seen. (Kennedy, Ref. 43, and Morgan and Stellar, Ref. 44: data from Boring, Langfeld and Weld, Ref. 45).

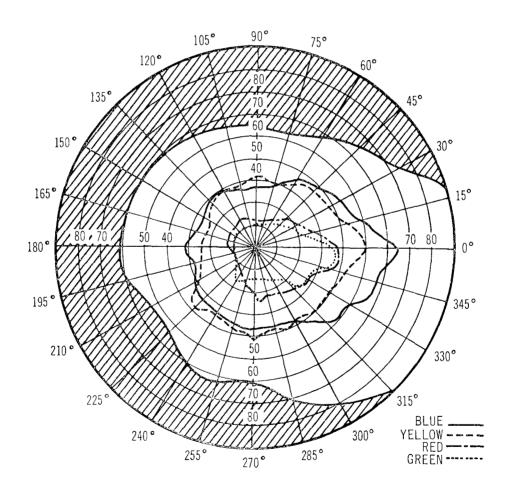
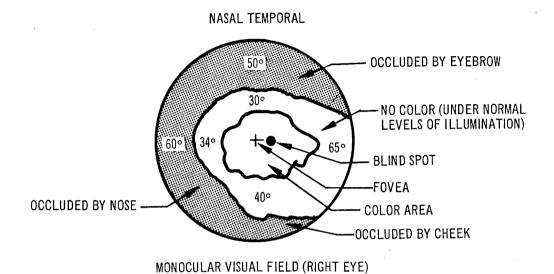


Figure 44. COLOR ZONES OF THE HUMAN EYE



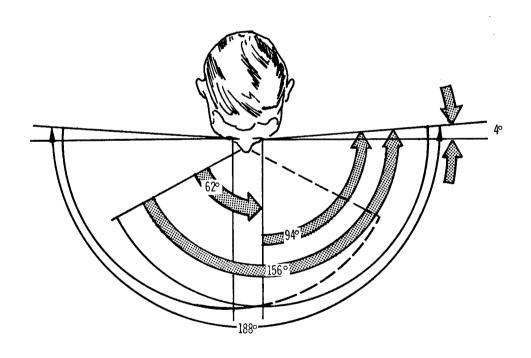


Figure 45. APPROXIMATE HORIZONTAL VISUAL FIELD From Allen (Ref. 57)

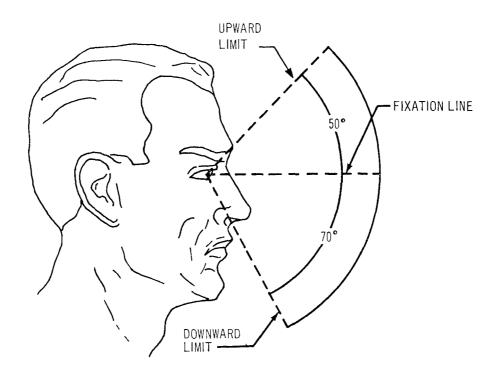


Figure 46. APPROXIMATE VERTICAL VISUAL FIELD

When a person is looking directly at a point, he is using his foveal, or central, vision. He is said to be fixating the point, and the point may be considered a fixation point. The fixation point lies on the visual axis, or line of sight; this point and any other object on the visual axis appears at the exact center of the visual field. The position of any other point in the visual field can then be given as an angle between the visual axis and a line between that point and the eye. This angle is the eccentricity angle - the angle by which the point is off-center in the visual field.

The eccentricity angle, then, indicates the distance of any point in the visual field from the center. On charts of the visual field, circles of equal eccentricity are generally drawn about the fixation point as guides (see Fig. 47).

For precisely specifying the direction of a point from the center of the visual field, a reference radius is arbitrarily designated as zero degrees. The direction of a point in the visual field can then be given as the angle between the reference radius and a line connecting the point and the center of the visual field. It is customary to provide equally spaced radial reference lines on charts of the visual field (see Fig. 47). The line selected as the zero-degree reference radius varies with different charts.

To locate a point in the visual field, then, we specify its eccentricity and its direction in degrees. For example, point A in Fig. 47 lies 20 degrees out in the field and 300 degrees from the reference radius. Point B lies 40 degrees out and 150 degrees from the reference radius (or 30 degrees above the horizontal in the upper left quadrant of the field).

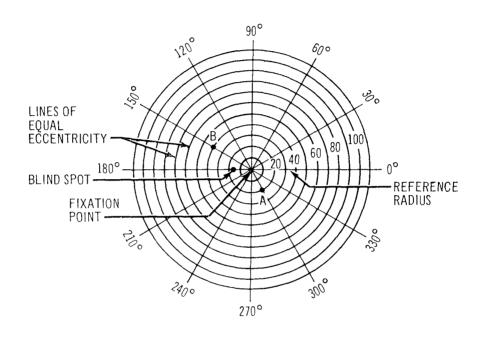


Figure 47. LOCATING POINTS ON A CHART OF THE VISUAL FIELD OF THE LEFT EYE

The direction from the center of a visual field is also often given as up, down, nasal, or temporal. Nasal refers to the half of the visual field toward the viewer's nose and temporal to the half toward his temple. The terms are limited to a monocular field. Obviously, the nasal half of the field is to the right in the left eye and to the left in the right eye, and the temporal half is to the left in the left eye and to the right in the right eye. Since the field in Fig. 47 is for the left eye (as shown by the location of the blind spot), point B could be located generally as "40 degrees on the temporal side" or precisely as "40 degrees out and 30 degrees above the horizontal in the upper temporal quadrant".

The terms nasal and temporal are also used to describe positions on the retina of the eye; the temporal retina is the side toward the temple, and the nasal retina is the side toward the nose. Note, however, that an object in the nasal field will be imaged on the temporal retina, and an object in the temporal field will be imaged on the nasal retina, because light rays cross the visual axis. In Fig. 42, for example, the object lies 30 degrees from the visual axis on the temporal retina. Similarly, an object that is up in the visual field will be down on the retina.

The angle subtended at the cornea of the eye by the viewed object is the visual angle. It is determined by the following equation in which "L" represents the size of the object measured perpendicular to the line of sight and "D" is the distance from the eye to the object:

Visual Angle = 2 arctan
$$\frac{L}{2D}$$
 (See Fig. 48)

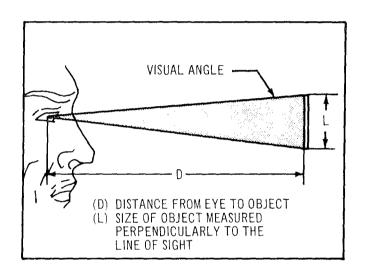


Figure 48. VISUAL ANGLE

The central portion of the visual area of the retina has a capability of fine definition. The function or capability is called central or foveal vision, and is essential for reading instruments and assessing displays such as the VSD and HSD. The centermost and best visual area, about 1° solid angle, is the fovea. Excellent detail vision extends over a larger area, perhaps 3 to 5 degrees, which is populated most heavily with cones.

Figure 49 shows the relationships between the probability of detection and the visual angle. Table 34 gives the horizontal and vertical angular limits of the human visual field as given in Wulfeck, et al. (Ref. 41) who also reported that the eyes can be turned approximately 50 degrees to either side of the resting position, 40 degrees above, 60 degrees below, and 10 degrees in torsion about the optical axis.

It should be noted, however, that with a full range of head, eye, and torso movement, the field of vision is 360 degrees in all planes (Ref. 41). However, the most important data for the computerized man-model in evaluating cockpit designs are the eyeball rotations, the narrow 3 to 5 degrees of detailed vision, and especially the 1 degree of foveal vision.

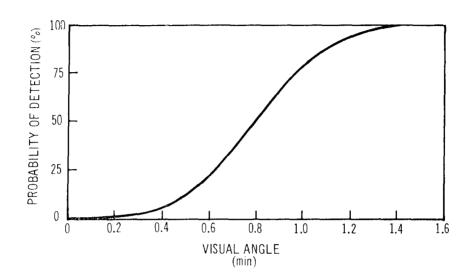


Figure 49. PROBABILITY OF DETECTION AS A FUNCTION OF VISUAL ANGLE

From White (Ref. 58)

Table 34 (Contd). Horizontal and Vertical Angular Limits of the Human Visual Field

ł			HORIZONTA	I LIMITS	VERTICAL LIMITS	LIMITS
			Temporal Nasa	Nasal	Field	Field
			Ambinocular		Angle	Angle
		TYPE OF FIELD AND	Field	Field	ďn	Down
	MOVIMENT PERMITTED	FACTORS LIMITING FIELD	(each side)			
0		Limits of head motion	720	720	800*	*oo6
		Maximum eye deviation	o 71/	250	084	299
		Range of fixation (from	्र ⁹ रा	127°	128°	156°
		central body line)		ģ	C	0
		Peripheral field (from	91,0	Approx (5)	180	16
		point of itxation)				
		Total peripheral field (from	237°	132°	°941	$172^{0\%}$
		central body line)				

* Estimated on the basis of tests on a single subject.

Ignoring obstruction of body (and knees if seated). This obstruction would probably impose a maximum field of 90° (or less, seated) directly downward; however, this would not apply downward to either side. ***

This is the maximum possible peripheral field; rotating the eye in the nasal direction will not extend it, The figures in parentheses on the line above are calculated values, chosen to give the maximum limit thus because it is limited by the nose and other facial structures rather than the optical limits of the eye. indicated.

1. All data except as noted are from Hall and Greenbaum (Ref. 59).

That is, at the sides, it The ambinocular field is defined here as the total area that can be seen by either eye; it is not limited to the binocular field, which can be seen by both eyes at once. That is, at the sides, it includes monocular regions visible to the right eye but not to the left, and vice versa. The term binocular is here restricted to the central region that can be seen by both eyes simultaneously stereoscopic vision). It is bounded by the nasal field-limits of the eyes. m i

From Wulfeck, J. W., et al. (Ref. 41)

Table 34. Horizontal and Vertical Angular Limits of the Human Visual Field

		1 HORIZONTAL	LIMITS	VERTICAL	LIMITS
		Temporal	-	Field	Field
MOVEMENT PERMITTED	TYPE OF FIELD AND FACTORS LIMITING FIELD	Ambinocular Field (each side)	ar Sinocular Field 9) (each side)	Angle Up	Angle Down
a. Moderate movements of head	Range of Fixation		009	37	1150
Eyes: 15° right or left 15° up or down	Eye deviation (assumed)	950	150	150	150
Head: 45° right or left		0011	*** 0 9	61 °	820
30° un or down	central ilxation Head rotation (assumed)	0511	1150	30.**	**************************************
	Total peripheral field (from body line	1550	105°	910	1120**
b. Head fixed Eyes fixed (central position to head)	Field of peripheral vision (central fixation)	950	0 09	941	670
c. Head fixed		۰،712	550	8 ¹	999
Eyes maximum deviation	<pre>(= range of ilxation) Peripheral field (from point of fixation)</pre>	910	Approx (5°)	180	160
	Total peripheral field (from central head line)	1650	***°09	°59	85 °
d. Head maximum movement	Limits of head motion (= range	720	720	80%	*o06
Eyes fixed (central with respect to head)	Peripheral field (from point of fixation)	950	009	797	670
	Total peripheral field (from central body line)	167°	1320	126°	1570**

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APPENDIX A

MAN-MODEL SPECIFICATIONS

1.0 SCOPE

The following specifications and requirements outline the items to be provided and the constraints within which the Baseline Man-Model (BOEMAN I) is to be developed during Phase I of the Cockpit Geometry Evaluation Program (Contract No. NOCOLL-68-C-0289). This is a program being conducted under the auspices of the Joint Army Navy Aircraft Instrumentation Research (JANAIR) Program Working Group (Committee).

The requirements detailed for the Baseline Man-Model are specific to Phase I and may or may not be applicable to later phases of the program. The requirements for the related section of the Computer Program will, in general, be applicable to the later phases of the Evaluation Program.

2.0 REFERENCE DOCUMENTS

The following documents include specifications and requirements for the Baseline Man-Model:

- 1. "Proposal for Cockpit Geometry Evaluation Method(s).

 Development", Boeing Document No. D6-15944, dated

 17 April 1967.
- 2. Clarification of Boeing Document D6-15944, Attachment to Boeing letter 6-1100-22-2300, dated 13 September 1967.
- 3. Addendum to Boeing Document No. D6-15944, dated 30 October 1967.
- 4. Boeing Document No. D6-53521, "Cockpit Geometry Evaluation Program" (a brochure to provide additional clarification of the program).
- 5. "Human Data for A Computerized Dynamic Man-Model BOEMAN", Boeing Document No. D6-53552, dated 1 March 1968.

3.0 EXPLANATION OF TERMS

Computer Program - The entire package of instructions to evaluate by digital computer the physical arrangement of a workspace, using a 21-pin-joint man-model.

Routines/Subprograms/Sections - Synonymous terms describing subsets of the computer program.

<u>Man-Model</u> - The abstraction of a given human pilot as a three-dimensional 21 pin-joint stick figure.

Math Model (Section) - That part of the computer program which calculates the joint locations and orientations during a movement.

Conventional (Standard) Anthropometric Dimensions - Measurements taken on live humans to define external dimensional characteristics.

Link - Ordinarily a connector between adjacent joint centers; otherwise, the segment beyond a terminal joint; a member of an immovable pair (neck and thoracic links); the distance between eyeball centers and the head link.

Task - A discrete physical movement or set of movements.

Movement - A specification of a fully defined initial position of all joints and a final position of all terminal joints (hands, feet, and head).

Geometry - The physical dimensions, volumes, shapes, locations, and orientations of all components and crewmembers in a workspace.

Computer Graphics Program - A separate computer program to draw pictures by computer controlled drafting machines or display pictures on a cathode ray tube (CRT).

Pre-Analysis (Section) - That part of the computer program which is to decide, a priori, if a given task is physically feasible.

Interference (Section) - That part of the computer program which is to discover if or how much interference (physical and visual) has occurred and how to eliminate it.

Input (Section) - That part of the computer program which describes the anthropometric characteristics and capabilities of any sized human, the sequence of tasks and the workspace geometry or physical restrictions.

Output (Section) - That part of the computer program which yields the numerical performance indicators and the task oriented history of the simulation using the man-model.

4.0 REQUIREMENTS

4.1 GENERAL

The Cockpit Geometry Evaluation Method(s) Program was instituted to establish an evaluation technique which is less costly in manhours, time, materials, and money than those presently used. The present techniques have been streamlined through the years and are not suited for additional reductions in flow-time or money costs. The three present methods employed (analysis, mockup, and flight test) are capable of accommodating only a limited number of geometric configurations with a limited number of operator sizes within time and economic constraints allowed.

The development of an improved evaluation method necessitates use of an efficient, rapid and accurate process or technique. The speed and accuracy available from a computer can provide the means to reduce evaluation time. In addition, the computer program is written to cover the large range of anthropometric sizes currently represented by the military pilot population. The tool, thus developed, will be especially useful and important during conceptual design studies. Large variations in operator size as well as many variations in the geometry of the crewstation can be examined before hardware must be designed and constructed.

The development of a computer program to provide the automated evaluation is a major undertaking. Models to synthesize three-dimensional human movements are not presently available. It is necessary, therefore, to develop this computerized articulated man-model in order that rapid evaluations can be successfully completed.

The general descriptions contained herein are to serve as guidelines in the development of the man-model and related sections of the computer program. The desired goals, functions and requirements, outlined in the following pages, are to be used in conjunction with the proposal on Cockpit Geometry Evaluation Method(s) (Boeing Document D6-15944).

4.2 SPECIFICATIONS AND CONSTRAINTS

The computer program to be developed will use input data consisting of: specified geometry, operator size, task sequences and physical restrictions to movement. These data are to be used to determine the adequacy of a given geometry. Assessments of reach capability and visual interferences, as well as summations of joint, mass and eye travels will be made. Body joint locations will be predicted. Discrepancies between control locations and human reach capability will be identified and noted. The results will be provided in tables, graphs and pictures as desired.

The initial man-model is to consist of a 21 pin-joint, stick-man, and the geometry will be lines and/or plane surfaces. Refinements will be made in a succession of steps to improve the configuration definition of both the human form and the geometry. An illustration of a proposed six-year (six-phase) program is shown in Figure 1.

The computer program for Phase I is to consist of six separate sections:

- (1) input data; (2) mathematical model to predict body joint locations;
- (3) visual assessment; (4) pre-analysis; (5) summation; and (6) output displays.

The input data will include those items necessary to specific crewstation geometry (the cockpit in this case), the operator (pilot) anthropometric

PHASE VI	FLEXIBLE SHAPE MAN-MODEL	FLEXIBLE SKIN INTERFERENCE ANALYSIS GEOMETRY DESCRIPTOR ROUTINES VALIDATION
PHASE V	ERGONOMIC MAN-MODEL	FORCE CAPABILITIES ENERGY EXPENDITURE GEOMETRY DESCRIPTOR ROUTINES VALIDATION
PHASE IV	ARTICULATED DIGIT MAN-MODEL	DIGIT ARTICULATION GEOMETRY DESCRIPTOR ROUTINES VALIDATION IEW
PHASE III	FLEXIBLE JOINT MAN-MODEL	JOINT INTERACTION JOINT CENTER EXCURSION REFINE MOVEMENT PATHS GEOMETRY DESCRIPTOR ROUTINES VALIDATION PROGRAM PLAN REVIEW
PHASE =	3-D MAN-MODEL	 THREE-DIMENSIONAL MAN-MODEL PHYSICAL INTERFERENCE GEOMETRY DESCRIPTOR ROUTINES VALIDATION
- 4	BASELINE MAN-MODEL	BASELINE MAN-MODEL DEVELOPMENT & VALIDATION VISUAL INTERFERENCE REACH ASSESSMENT HAND, HEAD, EYE, TORSO TRAVEL MASS DISPLACEMENT GEOMETRY DESCRIPTOR ROUTINES VALIDATION

Figure 50. RESEARCH PLAN SUMMARY

characteristics, the tasks to be performed, and the restrictions of movement of the operator. In addition, instructions will detail the amount, type, and quantity of evaluations to be performed and the manner in which results are to be displayed.

The mathematical model (man-model) is that mathematical description of the human form and its movement characteristics. The man-model is to identify the spetial locations of the body joints for specified movements or tasks required in the specified geometry.

Visual assessment capabilities are included in the first phase to (1) identify items which are not in view from the position synthesized for the operator, and (2) require simulation of that position the operator must assume in order to view the desired object.

The pre-analysis section of the computer program does an initial check on the feasibility of reaching and operating the specified control. In the event the specified operator is capable of the physical operation desired, a complete body joint location is specified, summations made, etc. If this operator cannot perform the required movements, the discrepancy is noted and amount of deviation from possible movement or reach capability is determined and recorded.

The results of the evaluation, body joint locations, joint, link, and mass movements are recorded. The output will be tables, graphs, and pictures drawn by computer graphics programs. The man-model defines joint spatial locations for each specified task. The joint location and link orientation will be used in computer graphic routines to depict the operator in the crewstation under investigation. The graphs will provide instantaneous

and/or cumulative travel for each link. This includes such items as eye or head deflection, wrist or palm movement, mass center displacement, and mass times distance totals.

L.3 INPUT DATA

The input data will include (1) cockpit configuration, (2) link dimensions, (3) task sequence, (4) standard position of the operator, and (5) joint angular limitations for unencumbered operators.

The following outline lists those presently identified items which must be considered. Additional items will be included when identified.

4.3.1 Cockpit Geometry

4.3.1.1 Raw Data

- a. Cockpit (eye) reference point for defining initial position of the man-model.
- b. Cockpit geometry x, y, z coordinates
 (controls, panels, displays, windscreen, seats, restraints, etc.).
- c. Cockpit control movements (path, movement, etc.).
- d. Surface description (fixed location) of additional crew member(s).

4.3.1.2 Transformation Adjustments and Subprograms

a. Transform all control and cockpit geometry locations from eye reference point to seat reference point (calculation based on link dimensions and standard position of 23-joint man-model).

- b. Allow for program calculation and storage of new positions that movable controls can assume.
- c. Data storage and retrieval subprogram to allow efficient program storage (i.e., cockpit control codes to reference the locations and dimensions of the controls).

4.3.2 Link Characteristics

4.3.2.1 Data Stored

- a. Operator link dimensions by mean and standard deviation.
- b. Mass quantity and location for the links and body segments by mean and standard deviation.
- c. Means of cross-referencing between the Hertzberg, et al., (AMRL-TR-52-321) Air Force pilot sample and other anthropometric surveys.
- d. Subprogram to calculate link dimension by specifying the percentile value of a given link, and then selecting the corresponding mass quantity and location.

4.3.3 Task Sequence

4.3.3.1 Data

a. Definition of the task (terminal point locations, orientation of links, time for performance, joint velocities and angular acceleration allowed, time to maintain position, sentence descriptors, etc.).

- b. Task sequence and/or frequency.
- 4.3.3.2 Transformation, Adjustments, and Subprograms
 - a. Transform the location of terminal points into cockpit codes.
 - b. Check for task feasibility with respect to the cockpit envelope, time compatibility, additional crewmember envelope, pilot's link dimensions or angular limitation of joints.

4.3.4 Initial Position

4.3.4.1 Data

- a. Eye reference point
- b. Starting position of hands
- c. Location of all other joints for specified operator
- 4.3.4.2 Transformations, Adjustments, and Subprograms
 - a. Subprogram to identify the joint and link locations of the specified operator.
 - b. Specification of standard position via coordinate system which is compatible with the computer graphics program.

4.3.5 Joint Angular Limits

4.3.5.1 Standard Position

- a. Head, Thoracic, Lumbar, Pelvic, Humeral,
 Tibial, and Foot Links Vertical
- Badial, Hand, Femoral Links Horizontal in Sagittal Planes

4.3.5.2 Data

- a. Absolute physical angular limitations of joints expressed as \pm deviations from the standard angle $(0^{\circ}, 0^{\circ}, 0^{\circ})$ of each joint.
- b. Modified limitations based on encumbrances (seat, harness, lap belt, clothing, etc.).
- c. A definition of preferred or "comfortable" joint angular positions.

4.3.5.3 Transformations, Adjustments, and Subprograms

- a. Define priorities to be used for deviating from the preferred "cone-of-operation".
- b. Define rules for determining the amount of individual joint movement outside the "preferred cones" before requiring angular changes in the adjacent joints.

4.4 OUTPUT DATA

4.4.1 Printed Output

- 4.4.1.1 Cockpit Geometry (from input).
- 4.4.1.2 Link Dimensions (from input).
- 4.4.1.3 Starting (Standard) Position.
- 4.4.1.4 Joint Angular Jimits (from input).
- h.h.l.5 Time Specified for Deginning and Execution of a Task, or Maintaining a Location (from input).
- 4.4.1.6 Beasons for Mon-feasibility of a Specified mask and the Amount of Deviation (determined in pre-analysis section).

- 4.4.1.7 Path of Motion of Terminal Point(s) (Straight Line Equation or Other Curve from Model).
- 4.4.1.8 Joint Locations for a Specified Number of Positions
 Along the Movement Path (depending upon the path
 length) Including Initial and Final Positions.
- 4.4.1.9 Results of Visual Interference Assessment
 - a. Portion of the viewed object which is obstructed in the initial position of the head.
 - b. Position to which the head is moved to eliminate interference.
 - c. Distance the head is moved to alleviate interference.
 - d. Percent of the central cone obstured in the initial and redefined head positions.

4.4.1.10 Summation Quantities

- a. Joint center of travel
- b. Mass displacement (each link and total body).
- c. Head angular deflection to observe all terminal hand positions plus other specified sighting points.
- d. Eye deflection (in addition to head movement).

The above quantities must be identified for each task specified, as well as the cumulative amounts for an entire mission. These data will be used to display instantaneous and cumulative results via graphs and/or tables.

APPENDIX B

Bivariant data on pertinent anthropometric measurements of the 1950 USAF pilot survey by Hertzberg, et al. (Ref. 1); the yet unpublished 1967 USAF pilot survey; the 1960-61 combined NATO survey of military personnel of Greece, Turkey, and Italy; and the 1964 Naval aviators survey (Ref. 47) are provided herein.

BIVARIANT DATA OF THE 1950 USAF PILOT SURVEY

Variables	Pages
Functional Reach and Seated Height	161-62
Functional Reach and Stature	163-64
Functional Reach and Seated Shoulder Height	165-66
Functional Reach and Buttock-Knee Length	167-68
Functional Reach and Seated Eye Height	169-70
Functional Reach and Seated Shoulder Breadth	171-72
Buttock-Knee Length and Seated Shoulder Height	173-74
Buttock-Knee Length and Scated Eye Height	175-76
Buttock-Knee Length and Scated Knee Height	177-78
Stature and Seated Height	179-80
Stature and Seated Eye Height	181-82
Stature and Seated Knee Height	183-84
Stature and Buttock-Knee Length	185-86
Stature and Seated Shoulder Breadth	187-88
Stature and Shoulder-Elbow Length	189-90
Seated Shoulder Height and Seated Knec Height	191-92
Seated Shoulder Height and Seated Eye Height	193-94
Seated Shoulder Height and Seated Shoulder Breadth	195-96
Seated Shoulder Height and Shoulder-Elbow Length	197-98

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BIVARIATE FREOUENCY TABLE FOR FORMARD ARM REACH AND AND BUTTOCK-KNEF LENGTH

BUTTOCK-KNEE LENGTH

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BUTTOCK-KNEE LENGTH

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RIVAZIATE FREQUENCY TABLE FOR FIGHT FOKWARD ARM REACH

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BIVAPIATE FREGUENCY TABLE FOR FORMARD ARM SEACH BIGHT

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BIVARIATE FREQUENCY TABLE FOR FORMAND ARM PEACH AND SEATED SHOULDER BREADTH

SEATED SHOULDER BPEADTH

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RIVARIATE FREQUENCY TABLE FOR PREADTH AND SFATED SHOULDER PREADTH

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SEATED SHOULDER HEIGHT

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SFATED SHOULDER HEIGHT

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BIVARIATE FREQUENCY TABLE FOR AUTTOCK-KNEE LENGTH AND AND

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BIVARIATE FREQUENCY TABLE FOR AND SEATED SHOULDER BREADTH STATURE

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TABLE FOR	LDER HT AND SHOULDER-ELBOW LENGTH
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BIVARIANT DATA OF THE 1967 USAF PILOT SURVEY

<u>Variables</u> <u>Pag</u>	es
Functional Reach and Seated Height	-201
Functional Reach and Stature	-203
Functional Reach and Seated Shoulder Height	-205
Functional Reach and Buttock-Knee Length 206	-207
Functional Reach and Seated Eye Height 208	-209
Functional Reach and Seated Shoulder Breadth210	-211
Buttock-Knee Length and Seated Shoulder Height 212	-213
Buttock-Knee Length and Seated Eye Height 214	-215
Buttock-Knee Length and Seated Knee Height	-217
Stature and Seated Height	-219
Stature and Seated Eye Height	-221
Stature and Seated Knee Height	-223
Stature and Buttock-Knee Length	-225
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Seated Shoulder Height and Seated Knee Height	-231
Seated Shoulder Height and Seated Eye Height	-233
Seated Shoulder Height and Seated Shoulder Breadth 234	-235
Seated Shoulder Height and Shoulder-Elbow Length 236	-237

BIVARIATE FREQUENCY TABLE FOR SEATED HEIGHT AND FORWARD ARM REACH

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BIVARIATE FREQUENCY TABLE FOR SEATED HEIGHT AND FORWARD ARM REACH

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BIVAPIATE FPEQUENCY TABLE FOR SEATED SHOULDER HEIGHT AND FORWAPD ARM REACH

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BIVARIATE FREQUENCY TABLE FOR SEATED EYE HEIGHT AND FORWARD ARM PEACH

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#EAN STD DEV REGRESSION EQUATIONS SITTING 809.50 30.16 (0.296)*Y + (571.626) EACH————————————————————————————————————	SUMMARY STATISTICS MEAN STD DEV REGRESSION EQUATIONS SITTING 809.50 30.16 (0.296)*Y + (571.626) EACH 803.08 39.80 (0.516)*X + (385.584) *** CIENT 0.391 (BASED ON ORIGINAL DATA) 0.391 (BASED ON *** *** *** *** *** *** ***				i				· }	}			-4	-	5			İ	2420
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BIVARIATE FREQUENCY TABLE FOR SEATO SHLDR BROTH AND FORWARD ARM PEACH

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SUMMARY STATISTICS	
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Y TABLE FOR	BUTTDCK-KNEE LENGTH
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RIVARIATE FREQUENCY TABLE FO? SEATED EYE HEIGHT AND BUTTOCK-KNEF LENGTH

BUTTOCK-KNEE LENGTH

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BIVARIATE FREQUENCY TABLE FOR SUTTOCK-KNEE LENGTH

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634	00.		0.0	0.1	0.3	•	0.5	0.3	8.0	6.0	1.1	6.0	0.9	0.3	0.2	0.1	0.0							0	•	CENT	SIZE 2420.		ON EQ	4		0.388		1.2	0.794
624	60.	0.0	0.1	0.1	0.2	0.5	0.1	0.8		1.7	2.0	1.0	0.8	0.5	0.5	0.2		0.1	0.0					5	1	40000	0F \$12	S	REGRESSION EQUATIONS	V*(357)	0.3501*X		;	4 C	95
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VALUES IN THE TABLE APE PERCENTAGES BASED ON A SAMPLE OF SIZE 2420.

SUMMARY STATISTICS

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	5.00	5.00	5.00	5.00	5,00	5.00	5.00	5.00	5.00	795.00	785.00	775.00	5.00	5.00	5.00	735.00	5.00	5.00	705.00	5.00	5.00	5.00	5.00	•				1					:	
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BIVARIATE FREQUENCY TABLE FOR FORMARD ARM REACH AND SEATED SHOULDER HEIGHT

SEATED SHOULDER THE SERVE

34 644 654 664 1	684 694	.00 .00 .00 TOTAL) e ^e	-	, , ,	77 7 7			7	130	000	757	5 2 2	77.	1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1	CKE	300	010	K 5 -	K. C.	6	26	`	36 11 -7 3324		; ;	SE-EST	31.78	SROUPED DATA!	1 2 2	
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		TOTAL	•		•	٠ د	0.7	1.0	1.7	2.0	4.1	4.5	6.9	9.5	7.6	11.3	12.3	10° C	.3	9.9	4. 8	3.4	1.6	6.0	•	100.0			! !			į				:
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	684					0			0	0	0					0.0		0								0.3			1		SE-EST	31.78	0.424 (BASED ON GROUPED DATA)	, R	1.82	-1.01
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	499	00							0.2	C•3	Ǖ3	0.3	0.5	0.2	0.2	0.0	0.3	0.2	0.1	0						2.2	BASED		•		Š.	397,536)	NO 0:	0 OF	15+3307	1+33
	654	00•	•	•	•	0	•	0.2	۳ د	0.1	0,3	0.3	4.0	9.0	0.5	4.0	0.2	0.2	0.1	0.1	0.1					3.9		•			ATION	397 379	(BASE			
	544	00•		•		1.0	0.1		0,3	0,3	0.5	9.0	1.0	6.0	9.0	1.0	9.0	0.4	0.3	1.0	0.2	0.0				7.0	CENTA	3324•			N EQU	++	•454		1.76	0.693
	634	609	0 0) ·	7.0		0.2	ر. 2	۳,	0.3	7.0	0.3	6.0	1.2	1.3	1,3	1.0	8.0	4.0	4.0	C•2	0.2	0.0			10.2	ARE PERCENTAGES	OF SIZE			REGRESSION EQUATIONS	0.582)*Y 0.310)*X		.≪	Ņ	60
HEIGHT	624	00.					2.0		0.2	0.2	8.0	0,3	1.1	1.4	1.5	1.7	2.2	1.2	1.0	0.7	0.3	0.3	0.1	0.1	0.0					SUMMARY STATISTICS	REGR	00	0.425 (BASED ON DRIGINAL DATA)	F.	X AS A FUNCTION OF Y 0.432	0.42
DER	614			•				٠, ن	6.2	0.4	C. 7	C* 2	1.1	1.7	1.7	2.3	2.1	1,3			**			0		15.0 1	E TAB	ON A SAMPLE		STATI	>		GINĀL	CHEC		
SEATED SHOULDER	604	00						٠. د	o.,	2.1	0.3	0.5	0.7	1.4	1.3	1.6	2.2	2.1	1.6	1.0	6.0	7.0	0,3	.0	0.1		VALUES IN THE TABLE	V N		MARY	STD DEV	35.11 25.63	N ORIG	SSION	>	×
ATED	594	8				o.		:	0.0	0.1	C• 2	9.0	6.5	8°0	1.5	1,2	1.7	1.6	1.5	6.0	6.0	9.0	0.2		0.0	12.4 1	LUES		•	SUF			SED C	REGRE	0N OF	P. O
SE	584	00.				,	0	ပ	0.0	0.1	C. 1	0.2	C. 4	8.0	ر• ي	٥. ٢	1.0	1•1	6.0	6.0	1.1	0.5	4.0	.0	0,1		>				MEAN	754.76	S (BA	¥ 0F	UNCTI	UNCTI
	574								0.0	0.0	0.1		0.1	0.3	0.3	7.0	٥٠ ٢	0,5	9.0	6 0	0.2	0.2	0.3			5.2							0.42	EARIT	SAF	SAF
	564	00.										ပ ိ ဂ	1.0	0.3	0.2	0.2	Ç.1	4.0	C.4	0. 4	0.2	0.4	0.2	C. 2		5.9						EACH HT/SI	IENT	2	×	∀
	554	00.									0.0	0.0	0.0		0.0	0.0	0.2	C•2	0.1	0.2	C •2		٠ ت	0		1.2						X-FUNCTIONAL REACH Y-MID-SH'LDER HT/SIT	EFFIC			
	544	00															0.1	0.1	0.0	0.0	0.1	0.1	ن	0		4.0						NCT IC D-SH	ON CO			
	534	8																		٥ . ٥		0.0			0.1	0.1						X-FU	CORRELATION COEFFICIENT			
		,	885.00	812.00	00.000	30.558	00	835,00	00.	815.00	805.00	195.00	785.00	00.	765.00	755.00	145.00	735.00	725.0C	715.00	705.00	695.00	685.00	675.00	665.00	•							CORR			
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BIVARIATE FREQUENCY TABLE FOR FURMARD ARM REACH AND BUITDCK-KNEE LENGTH

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BUTTOCK-KNEE LENGTH	274 584					_	•	•	, 4	0	7 23	12 24	23 51				106 65		39 22	31 8	13 8	٠	æ			184 664	SUMMARY STATISTICS	STD DEV	35.11 25.33	0.676 (BASED ON ORIGINAL DATA)	LINEARITY OF REGRESSION CHECK
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		00 000												•	~				4 23		12 2:	7		7	•	61 19			X-FUNCTIONAL REACH Y-BUTTOCK-KNEE L'GTH	CORRELATION COEFFICIENT	
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825,00							0.0		0.0	0.3	0.1	0.1	0.1	C•2			0.1
200									0.1	0.3	0.5	6.2	0.3	0.2	•		
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805.00						ပ ်	0.2	0.2	۰,	8	0.8	9.0	0.5		0.2		
195.00				0.0	0		0.5	9.	C.2	1.0	0.8	••	4.0	2.0	0.0		
785.00				0.0	0,2	0.2	Ç.5	0.0		1.6	7.0	9.0	0.3	0.2	0.1	0	
175.00				•	0.1	9.0	1.3	1.7	5. 0	1.7	1:1	9.0	0.2	0		0	•
765.00			0.0	0	•	6	1.2	2.1	2.1	1.8	8.0	4.0	0.2	0.0			
755.00				C.2	0.5	1.3	2.4	2.2	2.3	1.1	8.0	4.0	0.2			•	
745.00				0.2	0.1	1.5	2.8	3.2	2.0	6.0	4.0	0.2	0.1				
735.00		0.1	0	9.0	1.1	2.0	2.2	1.7	1.4	9.0	O.3	0.1	0		!	í	
725.00	0		3	0.7	1.3	2.1	1.6	1.2	6.7	0.2	0.2						
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685.00	0	0.0	4.0	0.2	.0	0	0.2	0.1			•						
675.00	0	.0	6.0	0	0.2	0.2	ů								į		
665.00		0	0.2		1	1	0.0		0.0	0							
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	¥. ₹.	JNCT I	ONAL K-KNE	X-FUNCTIONAL REACH Y-BUTTOCK-KNEE LYGTH	ا ج		92	35	33	• •	0.936)*Y +		215,	215.2491		25.89 18.67	
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					VEARI	TY OF	REGR	LINEARITY OF REGRESSION CHECK	N CHE	E.	: 1	!	u	0.05	ı	, P. P.	
				×	15 A 1	A FUNCTION OF	ION	FY		0.682	82	1.10		15+3307	. 20	0.39	
ì			ŗ	>	AS A I	FUNCTION	ION OF	×	•)	0.441		21+330		-2.21	

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SEATED EYE HEIGHT

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VALUES IN THE TABLE ARE PERCENTAGES BASED ON A SAMPLE OF SIZE 3324.

SUNHARY STATISTICS	MEAN STD DEV REGRESSION EQUATIONS SE-EST	X-HEIGHT (STATURE) 1762-18 59-87 (2.8531*Y + (692-807) 37-54 Y-SHOULDER-ELBOW LTH 353-82 16-35 (0.2131*X + (-8.274) 10-25	CORRELATION COEFFICIENT 0.779 (BASED ON DRIGINAL DATA) 0.776 (BASED ON GROUPED DATA)	LINEARITY OF REGRESSION CHECK ETA F D OF F C.R. X AS A FUNCTION OF Y 0.777 0.452 22+3300 -2.21
		X-HEIO	CORRELATIO	

	10101	, ,	17	36	13	131	234	339	461	664	498	411	301	174	97	*	12	•	3324
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	464	,									-	-	-	-	-	-		_	~
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SE-EST	22.21 22.12	GRCUPED DATA)	6 C.33
REGRESSION EQUATIONS	(C,501)*Y + (349,401) (C,496)*X + (223,089)	.496 (BASED ON	1.077 16+3306 C.33 1.402 15+3307 1.10
		GINAL DATA) 0.	
MEAN STD DEV	613.50 25.63 527.66 25.52	8 (BASED ON DRIG	LINEARITY OF REGRESSION CHECK ETA X AS A FUNCTION OF Y 0.5C0 Y AS A FUNCTION OF X 0.5CG
	X-MIC-SHILDER HT/SIT Y-KNEE HGT/SITTING	CCRRELATION CCEFFICIENT C.498 (BASED ON DRIGINAL DATA) 0.496 (BASED ON GROUPED DATA)	LINEARIT X AS A F V AS A F

SUMMARY STATISTICS

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	544	• 00	,	0	0.2	0.2	9.0	1.3	1.7	2.2	2.0	1.5	0.9	ۍ د	0.3	0.0				11.5		TABLE SAMPLE		SUMMARY STATISTICS			0.498 (BASED ON CRIGINAL DATA)	CHECK
	534	00•	•	0	٠.	0,2	0, 5	6,0	1,1	2.2	2,2	7,4	1,7	9.0	0.2	•	.0			11.2				Y ST	STO DEV	25.63	*** RIGI	M
	524	00		!	ļ	0.2	0.2	0.7	0.9	1.8	2.0	2. C	1.6	0. B	9.0	0.2	0.1			11.6		VALUES IN THE		UMMÄ	STO	2 2	8	LINEARITY OF REGRESSION X AS A FUNCTION OF Y
	514	00	0			0.2	9.0	6.0	2,1	2.5	3.2	3.8	2.9	2.2	1.2	0.7	C •2	0.1	•	20.6 11.0		VALUE			MEAN	613.50 527.66	BASEC	TY OF REGRES
	504	° 00	•	0			6.1	0.4	C. 7	1.1	1.9	2.4	1.7	1.9	1,3	Ǖ3	C•3	0.0	0.0					1	1	613 527	498 (TTY 0 FUNC
	464	٠ 00						0,1	2,0	7,0	0°2	1.3	1,1	1,3	9,6	9,0	0,2			6,8 1	,	,				SIT		INEAR AS A
	484	00•					0.0	0.0	0.1	4.0	0.3	9.0	1.1	8.0	0	0.5	0•3	0.1	0.1	5.1	;				•	R HT/	IC I EN	ű×.
	414	00.							0.0	0.0		0.3	0.1	0.2	0.1	0,2	0.1	0.1		1.2			:	;		HILDE HGI/S	COEFF	
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0.841 (BASED ON GROUPED DATA)

CCRRELATION COEFFICIENT C.844 (BASED ON CRIGINAL DATA)

613,50 778,89

X-MIC-SH'LDER HT/SIT Y-EYE HT/SITTING

13,74

25.63 (0.727)*Y + (46.913) 29.74 (0.980)*X + (177.899) 8.0°0 8.0°0 8.0°0

F D OF F 0.764 19+3303 0.990 15+3307

LINEARITY OF REGRESSION CHECK ETA X AS A FUNCTION OF Y 0.841 Y AS A FUNCTION OF X 0.841

SEATED EYE HEIGHT

	TOTAL	0.1	0.3	1:1	2.2	3.9	7.0	10.2	13.9	15.0	15.0	12.4	9.1	5.2	5.9	1.2	4.0	.0	100.0
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834	00		0.1	0.3	6.5	4.0	0.8	0.1	0.1	0.0				ĺ		-			2.3
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114						0,1	0.3	1.0	1.8	3.2	3.5	2.0	1.0	0,1	0.0				2.91
764						0.0	0.1	0.2	0.9	2.2	3.4	2.9	1.8	9.0	0.0				12.21
154								0.1	C• 3	1:1	2,3	2.9	2.2	0.7	C• 2	•			9.91
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VALUES IN THE TABLE ARE PERCENTAGES BASED ON A SAMPLE OF SIZE 3324.

SURFARY STATISTICS	MEAN STO DEV REGRESSION EQUATIONS SE-EST	613,50 25,63 (0,727)*Y + (46,913) 13,74 778,89 29,74 (0,980)*X + (177,899) 15,94	CCRRELATION COEFFICIENT C.844 (BASED ON CRIGINAL DATA) 0.841 (BASED ON GROUPED DATA)	LINEBRITY OF REGRESSION CHECK ETA F C OF F C.R.		0.841
	;	X-MIC-SHILDER HT/SIT Y-EYE HT/SITTING	CCRRELATION COEFFICIENT C.84	LINEBRIT	A SA X	J W SW A

	i 1	SEATD	SEATD SHOULER	H	BIVARIATE		ENCY	TABLE SEATED	FOR SHOULDER		BREADTH	~				
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	X-MIC-S Y-BICEL	X-MIC-SH'LDER HT/SIT Y-BICELTGIO(SHLCR)BR	HT/SIT L DR 18R	613 454	613,50 454,14	25.63	m 9	0,25	C.256)*X		472,363 297,006	£ 5	24.58	1	1	1
COR	CORRELAT ICN	COEFFICIENT		C, 282 ((BASED	ON CRIG	CRIGINAL	DATA)	0.28	•	(BASED ON		GROUPED DATA)	ATA)		
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BIVARIATE FREQUENCY TABLE FOR SEATO SHOULDER BREADTH ______

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645,00 \$ 635,00 # 625,00		0,0	ı	0.2	0.1	4.0	C. 4	9.0	9.0	0.0	0,5	C•3	0.2		0	0.1	m
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U 605,00		0,1	0.3	0.7	1.1	2.8	2.1	2.3	2.3	1.4	0.8	0.3	0.2	0.1	0.0		15.
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**	-MIC-S	X-MIC-SH'LDER HT/SIT Y-BICELTOID(SHLDR)BR	HT/S	IT BR	613.50 454.14	0 4	25.63	63	60	0.311)*Y C.256)*X	++ >×	472	472,363)	İ	24.58 22.32	• !	
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317	• 50							~			m	4	S	~	7	6	ď		54		
312	,50									~	7	7	~	m	4	~			15		
307	• 50								~			-	~		7	~			•		
305	• 50												-						7		
		695.00	685,00	615.00	665,00	655.00	645.00	635.00	625.00	615.00	605,00	595.00	585,00	575.00	565,00	555.00	545.00	535,00		,	

1

0.497 (BASEC ON GROUPED DATA)

CORRELATION COEFFICIENT C.496 (BASED ON CRIGINAL DATA)

C.R. -1.09

D DF F 22+3300 15+3307

0.681

X AS A FUNCTION OF Y
V AS A FUNCTION OF Y
0.500
V AS A FUNCTION OF X
0.500

SE-EST

22.25 14.19

REGRESSION EQUATIONS (C.778)*Y + (338.259) (C.317)*X + (159.587)

> 25°63 16°35 ***

613,50 353.82

X-MIC-SH*LDER HT/SIT Y-SHCULDER-ELBOW LTH

STD DEV

MEAN

417 .50 TCTAL

SHGULDER-ELBOW LENGTH

D162-10126-1 276 SHOULDER-ELBOW LENGTH

0.681

LINEARITY OF REGRESSION CHECK ETA X AS A FUNCTION OF Y 0.500 Y AS A FUNCTION OF X 0.500

BIVARIANT DATA OF THE 1964 NAVAL AVIATOR'S SURVEY

<u>Variables</u>	Page
Forward Arm Reach and Seated Height	280
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COMPELATION TABLE

FORMAND ARM REACH AND SIFT

AND SIFTING HEIGHT

ENTHIES REPHESENT PERCENTAGES OF 1549 SUBJECTS.

FORMAKD ARM REACH

32.0 TO 37.6	SITIING HEIGHT	E 10	27.7	6. a.c.	£ 6	39.5	30.6	30.6	31.2	31.8		33.0 33.6	33.6	34.7	35.3	35.3 5.3	35.9 36.5	101 AL
33.8 TG 34.4 34.4 TG 35.6 35.0 TG 34.4 35.0 TG 34.6 36.0 TG 34.6 36.0 TG 34.6 37.0 TG 34.6 37.0 TG 36.6 37	32.0 TO 32.6 32.6 TO 33.2	,	0000	965		129		000		1 Kg 0	0000	000	0 3 3 7 3 3		00000	100	0000	.363 .258
39.6 TO 37.0	200	000			.710	710	.775		.516		0 1 1 0 0 1 0 4 0	2 T				00	000.0	1.356 5.358
35.6 TG 34.2 36.8 TG 34.2 37.7 TG 34.2 37.7 TG 34.2 37.7 TG 34.2 37.7 TG 34.2 37.7 TG 34.2 37.7 TG 34.2 37.7 TG 34.2 37.7 TG 34.2 37.7	20	000°¢			. 008 000.	4 C	162.			• • • • • • • • • • • • • • • • • • •	969	. 487	* C C C		0.000	•	0.0001	4.461
36.8 TO 37.4	20	000000			591	m ~	148. 14 M		A IV	112.	972		186.	183	387	000000	0.00019	J. ~
38.0 TO 39.6 0.000 0.000 0.000 0.000 0.000 0.194 0.387 0.581 0.39 0.646 0.347 387 387 387 387 387 387 387 387 387 38	0 0	9.000		290	. 258 146	1.033	284		N2 -	986	988	16.69	01/		.258.		0.00016	
39.6 TO 39.2	10	00000		000-0	.065	0000.0			•		944	387	6 4 4 4 4 4 4 4 4 4 4 4 4 4 4 4 4 4 4 4		.258	•	. 0 66 0 65	4.325
39.4 TO 41.0 39.4 TO 41.0 39.4 TO 41.0 39.4 TO 41.0 39.4 TO 41.0 39.4 TO 41.0 39.6 TO 41.0 30.000 0.00	2 5	00000	0	000.0	000-0	00000	•129	.367	527	944.	53		. 323		00000	0	•	2,260
#0.0 TO 41.0 0.000	2 2	0000	9 0	00000	000000	90	000	000	\$ 3	60	000	# 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0	0.400 0.400) C	0000	CC	000	047
#1.0 TO 41.0 TOTAL O.65 .323 1.614 4.261 A.78012.07218.72214.65513.36310.200 7.811 3 MEASUREMENTS AND INCHES STANDARD MEAN DEVIATION RANGE HIGH LUW 1 5 50 9 ONWARD ARM CEACH ITTING MEIGHT TOTAL O.65 .323 1.614 4.261 A.78012.07218.72214.65513.36310.200 7.811 3 STANDARD STANDARD REASUREMENTS AND INCHES STANDARD BEHCENTILE LEVE SOUTH AND ARM CEACH I 1.246 9.0 41.3 32.3 33.4 34.2 36.2 COMMELATION R .377 SOUTH AND ARM CEACH SOUTH AN	10	00000	0	000.0	00000	000	000	0000.0	000	000.	000	0000		000	000	, C		
#EASUREMENTS AND INCHES #EASUREMENTS AND INCHES #EAN DEVIATION RANGE HIGH LUW 1 5 50 90 90 410 410 410 3 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.2 30.4 30.4 30.4 30.4 30.4 30.4 30.4 30.4	\$1.9 TO	0.000	0.000	000-0		000.	• 000	00000	000	00~	000	000-0	•	000.00	000*	0.00.0	•	• 0.65
FYPE MEAN DEVIATION RANGE HIGH LUW 1 5 50 9 31.51 1.421 8.8 36.2 27.4 28.6 29.3 31.4 36.28 1.246 9.0 41.3 32.3 33.4 34.2 30.2 COMMELATION R .377	101/L	2.0°	.323	1.614	.261	A.7801	2.0721	.7271	.65513	.2631	200	8 1 1	4 1	2,453	1,356	,323	. 258	100.0
### STANDARD #### DEVIATION RANGE HIGH LUW S 50 9 31-51	¥	INCHES			•	•								,				
31.51 1.421 8.8 36.2 27.4 28.6 29.3 31.4 36.28 1.246 9.0 41.3 32.3 33.4 34.2 30.2 COMMELATION R .377	dX1 (n∃ijdenS¤3m	لمٍ	MEAN	STAMD	180 1108	R N GE	1911	3	-	ម្ចា ស	CENTI	ור ורנעו פי	ELS 95	ው ን				
36.28 1,246 9.0 41.3 32.3 33.4 34.2 36.2 COMMELATION N 377	FORWAYD ARM DEACH		31.51	~	.421	5C 3D	36.2		28		m	31.4	34.0	35.0				
(VOY)	SITING MFIGMJ		36.26	Ď	.246 KRELAT	_	4 # (377	£ 33	4 0 K		2. eE	7) 10 (C)	♦ • 6€				

CORRELATION TABLE

FORMARD ARM REACH

ENTRIES REPRESENT PERCENTAGES OF 1549 SUBJECTS. AND STANDING HEIGHT

FORMARU ARM REACH

STANDING NEIGHT	27.1	27.7	24.3	29.5	10.0	30.0	30.6	31.2	3) 08	32.4	33.6	34.6	34.	36.7	35.3	36.9	70 F#L
63.0 TO 64.0	000		965 (0.000	065	0.000	0000	0000	00-0		000	9000		000	0.000	0000	.516
2 2	000	000	516	516	516							200	0000	000000		00000	2,250
	000-0		258	1.162	1,162	1.033	639	.581			000.0			• 0.65		0.000	5.249
2	0000	• 065	•159	968		1.614	1.291	÷83€	198	129			0.000	00000		00000	7.360
2	.065	•129	194	896	2,389	2.647	3.744		895	8228	***	6000		0000	0000	100000	٠, ۱
			000	129	707.1	7.130	3,551 3	776°	2.518	1.291	1.49	9 A	129	000		0.000	5.300
70-3 TO 71-2	0	000	000.0	.065	516				686.5	_	1.000	.343	A 58	129	0	0.0001	, m
	00000	00000	000-0	00000	194		1.420		094.	2,001	1,356	.775	.258	.258	.065	.0651	-
20	9-000	0.000	. 165	0.000	0.000		.581		1.479	1,162	1.485	. 713	.367	194		: 1165	•
70	00000	00000	00000	00000		• 000	• 065	.581	+00•	1,356	995	***	454	. 323	0	000.0	5.487
2	9.000	00000	0	00000	000.0	000.	•129	• 353	• 323	405		, U.	425	.129		• 065	3,551
2	00000	00000	_	00000					• ^ 65	.129		000.0	*67 •	.258		00000	\$08
75.8 TO 74.7	00000	00000	6	00000	00000		0		000.0	00000	5900	862	• 0.65	000.0	00000	• 065	452
2	00000		000.0	000.0	000.0	00000	0 000.0		00000	0000	000.0	00000	•065	000.0	00000	000.0	. 065
TOTAL	.065	.323	1.614	4.261	8.7801	.78012.07218.72214.65513.36310	B. 72214	,6551	3.3631	200	7.811	3,700	2,453	1,356	323	.258	100.0
MEASUREMENTS ARE IN INCHES	INCHES		•									•					,
MEASUREMENT TYPE	. ند	MEAN	STAND	NDARD	RANGE	HIGH	20		4 0	RCENTI S	PERCENTILE LEVELS 5 50 95	ELS 95	\$				
FORWARD ARM REACH		31.51		1.421	•	36.2	27.4	28.6		29.3	31.4	34.0	35.0				
STANDING HEIGHT		*6.6*		2.328 13 CORRELATION	13.6 ION R	77-1	673 35.201	•0	χ.	2.00	64.6	73.4	75.3				
						# *	2.197		1111								

CORNELATION TABLE

FORWARD ARM REACH AND SITTING SHOULNER HEIGHT

1549 SUBJECTS.

ENTRIES REPRESENT PERCENTAGES OF

FORWARD ARM REACH

SITTIMG SHOULDER MEIGHT	27.1	27.7	m •	29.9	39.00	30.0	30.6	31.2	M + 4 K	40	~	o v	. 4 H	34.7	35.3		101m
29.8 TO 20.8 22.2 22.7 TO 22.2 23.2 23.2 23.2 24.2 TO 23.2 25.2 25.2 25.2 25.2 25.2 25.2 25.2								0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0				PUBLICANT ACTOCCCCCCCCCCCCCCCCCCCCCCCCCCCCCCCCCC				00000000000000000000000000000000000000	
TOTAL	.065	,323	• i	261	8.7801	2.0721	. /8012.07218.72214	.65513	36310	7 00		*	2.453	1,356	,323	.258	0.001
MEASUMENTS AHE IN INCHES	A INCHES	Z X	STAND	PARD	RANGE	H9 I H	LOF	~	PERC	PERCENTILE LEVELS 5 50 95	. LEVE	ELS 95	*				
FORWARD ARM SEACH		31.51	-	124.	Q	36.2	27.4	28.6	29,3		31.4	34.0	35.0				
SITING SHOULDER HEIGHT	J. 10	23.80	0	1.063 7 ORRELATION	mα	\ \ \ \ \ \ \ \ \ \ \ \ \ \ \ \ \ \ \	.4 20.0 .285 17.084+ 22.454+	พี	.5 22.0 .213X) .3alY)		23 • 88	ن د	26.4				

COMPELATION TABLE

FORMARD ARM REACH

AND BUTTOCK TO KNEE LENGTH

ENTRIES REPRESENT PERCENTAGES OF 1549 SUBJECTS.

FORMAND ARM REACH

DUTTOCK TO KNEE LENGTH	O XX	EE LENGTH	27-1	1 27.7 7 28.3	28.3	29.5	30.05	30.0	30.6	31.2	37.4	32.4	3.66	33.6	7.00	74°4	35.3	35.9	ŦU! AL
N	1	2	000-0		.065												0.000	0.000	.065
ri in			0000	290.0	0.00		00000			00000	0000	0000	000.0	0000	0000	0000	000.0	0000	7
. Ñ	21.9 T	TO 22.4	990			186	452	1961	950									000	1.743
Ä			00000	0.055			1.485		1.227	581		999	.065		00000	00000	00000	00000	5.71
Ñ			000-2		•	1.591	1.743	_	3.228		.710	,323	.458		.065			0.00011.352	1.352
Ň	23.3.1	,	00.0		-		2.647	2,324			1.937	.775	.387		.129		0.000	0.00015.042	3+0+2
ni i			00.0		• 065		1.420				2.647		1.485	.75	159	•194		0.0001	9.561
Ň	24.2 .10	0 24.7	00.0		00000	0.000	.646			3.486 2	2.711		162.4	•51¢	+52	323	• 065	.06516.850	5.85¢
Ň			00.0	000-00	00000	00000	• 065				5.453		1.937	.046	. 323	194		.0651	1.165
Ñ			000.0	0.0.0.0	00000	00000	•065	.452	.581			1.679	1.162	.740	.516	1194	120	000.0	8.522
Ň			000.0	000-0 0	• 065	00000		•065					•646		. 367			129	***
Ñ			0000	000.00	000.0	00000							185		.065			000.0	1.808
Ñ		0 27.0	0000	000-0 0	00000	00000			_				184		.129			000.0	5/1
Ň		ď	0000	000000	000.0		000.0		0.000	0 00000	0000		000.0	• 065		D.000-	000.0	000.0	+ 25B
~	7.4 T	0 27.9	0.000	000-00	000.0	000-0		00000	0 000 0	00000 0000		00000	007.0	0.00.0	. 065	00000	00000	000.0	• 065
ĺ	TOTAL	4.	590.	5 .323	1.614	4.261	9.7801	2.0721	8.78012.07218.72214.65513.36310.200	1.65513	1,3631(1	7.811	3.7.4	2.453	1,356	.323	. 258	100.0
***		#			Ì														
Ŧ	SASUR	EMENTS AR	MEASUREMENTS ARE IN INCHES		•	1								; j					
	¥	MEASUREHENT	TYPE	HEAN	STANDARD		RANGE	HIGH	101	***	ğ vı	TCENT I	PERCENTILE LEVELS 5 50 95-	66.5 95.	6				
FOR	1ARD	FORWARD ARM REACH		31.51		1-4-1		36.2	27.4	9.82		29.3	31.+	34.0	35.0				
3	70CK	BUTTOCK TO KNEE LENGTH	ENGTH	24.09		666.	••	27.6	20.7	21.8		22.5	24.0	25.8	<6.5				
					B	CORRELATION R	4 1 C I	# # # >	586	_	.412X)								
								J	11.414.	•	(458)								

COMMELATION TABLE

FORWARD ARM REACH AND SITTING ETE HEIGHT

ENTHIES REPRESENT PERCENTAGES OF 1544 SUBJECTS.

FORWAHD ARM HEACH

3 F. 900 0.000 .365 0.00 .65 0.000 0.000 0.055 0.000 0	ME IG	27.1	27.7	28.9 9.85	28.9 29.5	30.00	30.0	30.6	31.2	31 • 8 3	32.4	33.0	33.6	34.2	36.7	35.3	35.9	TO I A i
29.3 TO 29.4 C.000 0.000 0.000 .25 4.52 4.52 4.52 4.65 4.65 0.005 0.000	10	000-	0.00	1	004.0	.045	00000		0	0	b	•)	000	0000	0000	00000	0
83.8 TO 29.8 0.000 0.000 129 134 1.97 1.72 1.97 1.94 0.000 0.000 0.100 0.000 0	2	0000	0.000		00000	25.7	. 25×											3
20.3 TO 29.8 0.000	10	00000	000.0		0	5,5	554			0								9 6
29.8 TO 31.3	2	00000	00000	00000	186	387	.710			'								A . A . A
30.3 TG 31.6 0.000 0.194 .065 1.079 1.356 3.099 1.872 1.220 775 .039 .347 .129 .129 .357 1.549 .347 .129 .129 .348 .349 2.318 2.71 1.549 .347 .129 .129 .348 .349 2.326 1.472 1.852 1.472 1.872	2	9.000		4 2 3	.77%	1,227		_			•	של איני על איני		45				
30.8 TG 31.3	0	0.000		0.65	1.033				~		1	3	707	.129	000	900	0.00013	,
31.3 TO 31.8	2	€90.		452	.516				: 14		_	240	100		2	00000	00000	4
31.8 To 32.4 0 0.000 0.129 .387 1.047 1.679 2.841 2.453 2.724 1.614 1.033 .347 .323 .129 3.429 3.729 1.029 1.029 1.029 1.023 1.429 .347 .323 .129 3.429 1.02	0	000-0		• 194	.546						_	167	**		129	00000	0.00015.133	
32.4 TO 32.9 0.000 0.000 0.005 .194 .710 .775 1.937 1.614 1.008 1 743 1.465 .839 .323 .337 .323 .323	2	000.0		129	.387					_	_	033	1880		2	00000	0.51	
32.9 TC 33.4	٠. و	00000	000.0	• 065	•194	.710	.775		_	-		584	3.0		387	129	0.653	6/11/
33.4 TO 33.9 0.000 0.000 0.000 0.000 0.005 0.129 0.452 323 0.139 710 516 387 323 0.055 3.055 3.059 0.129 0.129 0.129 0.129 0.129 0.129 0.129 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.129 0.059 0.129 0.000 0.000 0.000 0.000 0.000 0.129 0.129 0.129 0.000 0.0	٥	7.000	00000	000.0	.129	590	* 452		_	_	'	.64	100.		.323	3.4	00000	7
34.9 TO 34.9 0.000 0.000 0.000 0.000 0.129 .323 .387 .123 .129 .129 .129 .129 0.000 34.9 0.000 0.000 0.000 0.000 0.000 0.000 0.129 0.05 0.000 0.258 .129 0.05 0.000 35.4 TO 34.9 0.000 0.000 0.000 0.000 0.000 0.129 0.05 0.000 0.129 0.05 0.000 35.4 TO 35.9 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.129 0.05 0.000 35.4 TO 35.9 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 35.4 TO 35.9 0.000 0.0	ТО	00000	0000.0		000.0	.065	•129		•	•		516	337		0.00	290		2
34.4 TO 34.9 34.9 0.000 0.000 0.000 0.000 0.000 0.000 0.129 0.055 0.254 0.165 0.000 0.129 0.000 0.129 0.000 0.169	ě O	0000	0000		000.	00000	.129					129	**		00000	00000	9 6	100
35.4 TO 35.4 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.000 0.29 0.00 0.00	10 3	00000	0.00	000	006.0	.065	•065	•				2900	, V V					7
35.4 TO 35.9 0.000	10 3,	9.000	0.00	000		000		000	0	0		129	14	000		00000		7
TOTAL WEASUREMENTS ARE IN INCHES WEASUREMENT TYPE WEASUREMENT STANDARD AND 36.0 35.0 STANDARD WEASUREMENT WEASUREMENT TYPE CORRELATION R WEASUREMENT TYPE CORRELATION R WEASUREMENT TYPE CORRELATION R WEASUREMENT TYPE CORRELATION R WEASUREMENT TYPE T	35.4 TO 35	000	• 00			.000		0	0		0	000.			00000	000000	000000	.063
TTS AME IN INCHES STANDARD STANDAR	TOTAL	.065	! •	1.614		7. /801	2.0721/	1.72214	65513	16310		811		2,453	1.356	323	258	100.0
TTS ARE IN INCHES STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD STANDARD PENCENTILE LEVELS 95 95 95 94 PENCENTILE LEVELS 95 95 95 95 95 95 96 PENCENTILE LEVELS 95 95 95 95 96 PENCENTILE LEVELS 95 95 95 95 96 PENCENTILE LEVELS 95 95 95 96 96 96 96 96 96 96		8 - 1							8 8 8) () () () () (
STANDARD NEAN DEVIATION RANGE HIGH LOW 1 5 50 95 9 REACH 31.51 1.421 8.8 36.2 27.4 28.6 29.3 31.4 34.0 HEIGHT 31.57 1.185 7.6 35.6 28.1 28.8 29.7 31.5 33.6 CORRELATION R .358	MEASUREMENTS ARE IN	INCHES																
REACH 31.51 1.421 8.8 36.2 27.4 28.6 29.3 31.4 34.0 HEIGHT 31.57 1.185 7.6 35.6 28.1 28.8 29.7 31.5 33.6 35.6 28.1 28.8 29.7 31.5 33.6 35.6 28.1 28.8 29.7 31.5 33.6			MF A M	STAND		2	1	3	-	A S	ENTIL	LEVE	S 1	ć				
REACH 31.51 1.421 8.8 36.2 27.4 28.6 29.3 31.4 34.0 HEIGHT 31.57 1.185 7.6 35.6 28.1 28.8 29.7 31.5 33.6 35.6 28.1 28.8 29.7 31.5 33.6 35.6 28.1 28.8 29.7 31.5 33.6 35.6 35.8 35.8 35.8 35.8 35.8 35.8 35.8 35.8				01: 4 T M		1		<u>.</u>	•	^	2	<i>,</i>	ັບ	P.				
HEIGHT 31.57 1.185 7.6 35.6 28.1 28.8 29.7 31.5 33.0 CORRELATION R 22.160. (.299x)	FORWARD ARM REACH		31.51		144.	•	36.2	27.4				4.1	34.0	35.0				
ORRELATION R = .358 Y = 22,160+(.299X)	SITING EYE HELGHT		31.57		.185	7.6	35.6	28.1	(VI			3.5	33.6	34.5				
				S	RRELAT			358		Š				•				
_						- •		7.955		797								

AND SITTING SHOUL ER HEIGHT PUTTOCK TO KNFE LENGTH

ENTHIES REPHESENT PERCENTAGES OF 1549 SUBJECTS.

BUTTACK TO KNEE LENGTH

NG SHOULDER HE	50	21.0	21.4	21.9	20	22.8	23.3	23.7	24.2	* !	45.1	20.62	66.0 0.65 0.05	26.5	27.	27.4	TOFAL
######################################					00000000000000000000000000000000000000		00	0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0	00 00 00 00 00 00 00 00 00 00 00 00 00		1 = c c n d + + 0 0 + 4 0 0 0 0 0 0 0 0	O O C O O O O O O O O O O O O O O O O		220030 7 7 77		0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0 0	0 30 30 40 40 40 40 40 40 40 40 40 40 40 40 40
TOTAL	065		033		- i	m :	5.04219.	5611	, ¤501	168	. 522	0	1.808	775	,258	.065	100.0
MEASUREMENT MEASURE		HEAN		FANDARD	RANGE	H9 I H	LON	-	1	CENT		LEVELS 95	*				
BUTTOCK TO KNEE LENGTH	10	54.09	·	666.	6.9	27.6	20.7	21.8		22.5	24.0	25.8	46.5				
SITTING SHOULDER HEIGHT		23.80	100	1.063 7 CORRELATION	7.3 R NOI	N H H	20° 400 13°535 15°149	 	7 6 X	22.0	23.8	5 · c 2	69.				

AND KNEE HEIGHT BUTTOCK TO KNEE LENGTH

EMTHIFS REPRESENT PERCENTAGES OF 1549 SUBJECTS.

BUTTACK TO KNEE LENGTH

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		12	23.0 23.4	.12	• 52 6	22.	C)	23	24.2	2007	25.1	v.	25.0	Ð	27.0	27.4		TUTAL
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BUTTOCK	BUTTOCK TO KHEE LENGTH	FNISTA	24	54.09	666.	о £	9 27.6		20.7 21	Đ.	22.5	24.0	23.3	6.65				
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BUTTOCK TO KNEE LENGTH AND SITTING EYE MIGHT
ENTRIES REPRESENT PERCENTAGES OF 1549 SUBJECTS.

SUTTOCK TO KNEE LENGTH

SITTING EYE HEIGHT	€16HT	20.5	×12	21.4	21.9	22.4	22.8	23.3	23.7 2	24.2	24.7 6	65.5	20.6	26.0	26.5	27.4	27.4	TOTAL
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SITTING	SITTING EYE HEIGHT		31.57		1.195	7.6	35.6	28.1	26.8	1 29.7		31.5	33.6	34.5				
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COMPELATION 1ABLE

AND SITTING HEIGHT

STANDING HEIGHT

ENTRIES REPHESFNI PERCENTAGES OF 1549 SUBJECTS.

STANDING HEIGHT

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STANDING HEIGHT		69.94	2	.328	13.6	77.1	63.5	65.2	66.2	6.69	73.9	75.3				
SITTING HEIGHT		36.20	7	902.1	9.	61.3	32.3	(F)	34.8	36 02	36.3	39.4				
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COMMELATION TABLE

AND BUTTOCK TO KNEE LENGTH

STANDING HEIGHT

1549 SUBJECTS. ENTRIES HEPRESFNT PERCENTAGES OF

STANDING HEIGHT

PUTTOCK	TO KNE	BUTTOCK TO KNEE LENGTH	6.0 6.0 6.0	6.9	6.4.0 8.4.0	65.8	46.7	67.6 68.5	68.5	7 6.04	71.2 72.1	72.1	73.9	73.9	74.9	75.8	76.7	101AL
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COMPLIATION TABLE

STANDING HEIGHT AND KNEE HEIGHT

ENTAIRS REPHESENT PERCENTAGES OF 1549 5112 HELTS.

STAWING HEIGHT

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	AND HEIGHT			21.84	• (116.		25.1	19.0	19.7	20.3	31.8		2.4.5	24.2				
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STANDING HEIGHT

AND SITTING EYE MFIGHT

ENTAILS REPRESENT PERCENTAGES OF 1549 SUBJECTS.

STANDING HEIGHT

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\$111K	\$	SITTING EYE HEIGHT	-	31.57		1.185	7.6	35.6	20.1	28.4	7.62 8		31.5	33.6	34.5	_			
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COMPELATION TABLE

SITING SHOULDFH HEIGHT AND KNEE HEIGHT

ENTHIES REPRESENT PERCENTAGES OF 1549 SUBJECTS.

SITTING SHOULDER HEIGHT

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	SETTIM	Ø O	SITTING SHOULDER HEIGHT	EIGHT	23.80	-	.063	7.3	27.4	20.02	21.5	22.0	83.8	25.5	26.4				
	NAME OF THE POPE	Ę	<u>.</u>		23.84				25.1	19.0	19.7	20.3	8.15	23.5	24.2				
						8	CORRELAT	R MCIT		1.851+(.420K)	9 X 3							
								•				•							

COMMELATION TABLE

AND SITTING EYE MEIGHT SITTING SHOULDER HEIGHT ENTRIES REPRESENT PERCENTAGES OF 1544 SUBJECTS.

SITTING SHOULDER HEIGHT

sitting lye might	26.3		21.3	21.3	71.7	2 ~	22.7	23.2	23.7	24.2	25.2	25.2	25.7	26.1	26.6	27.1	10 FAL
47.8 TO 28.3	0000	000	129	323	000	7.000 (0.000	000	000	000	•	0000	00	0000	0000	000	. 194 . 839
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